# **Numerical Modeling** of COVID-19 Neurological Effects **ODE/PDE Analysis in R**

### **William E. Schiesser**

$$
\frac{\partial u_1}{\partial t} = -v_z \frac{\partial u_1}{\partial z} - (2/r_l) k_{m1} (u_1 - u_{2n})
$$

$$
u_1(z, t = 0) = u_{1n}
$$

$$
u_1(z = z_l, t) = u_{1e}(t)
$$



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### Contents





### Preface

Covid-19 is primarily a respiratory disease which results in impaired oxygenation of blood. The  $O_2$ -deficient blood then moves through the body, and for the study in this book, the focus is on the blood flowing to the brain. The dynamics of blood flow along the brain capillaries and tissue is modeled as systems of ordinary and partial differential equations (ODE/PDEs).

As further background (from [3]):

While fewer people who get COVID are dying, not all of them are recovering. We don't know how many people will remain hobbled, long-term. But it is plausible that tens of thousands in the United States may never be the same again.

Additional background is provided in [1, 2, 4, 5].

The ODE/PDE methodology is presented through a series of examples,

- 1. A basic one PDE model for  $O_2$  concentration in the brain capillary blood.
- 2. A two PDE model for  $O_2$  concentration in the brain capillary blood and in the brain tissue, with  $O_2$  transport across the blood brain barrier (BBB).
- 3. The two model extended to three PDEs to include the brain functional neuron cell density.

Cognitive impairment could result from reduced neuron cell density in time and space (in the brain) that follows from lowered  $O_2$  concentration (hypoxia).

The computer-based implementation of the example models is presented through routines coded (programmed) in R, a quality, open-source scientific computing system that is readily available from the Internet. Formal mathematics is minimized, e.g., no theorems and proofs. Rather, the presentation is given through detailed examples that the reader/researcher/analyst can execute on modest computers. The PDE analysis is based on the method of lines (MOL), an established general algorithm for PDEs, implemented with finite differences. Appendix A is a basic introduction to PDE modeling and computer-based analysis the reader can consult when starting on Chapters 1–6.

The routines are available from a download link so that the example models can be executed without having to first study numerical methods and computer coding. The routines can then be applied to variations and extensions of the blood/brain hypoxia models, such as changes in the ODE/PDE parameters (constants) and form of the model equations.

The author would welcome comments/suggestions concerning this approach to the analysis of brain hypoxia resulting from Covid-19.

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#### **REFERENCES**

- 1. Bridwell, R., B. Long and M. Gottlieb (2020), Neuorologic complications of COVID-19, American Journal of Emergency Medicine, 38, pp 1549.e3–1549.e7.
- 2. Collins, F. (2021), Taking a closer look at COVID-19's effects on the brain, NIH Director's Blog, January 14, 2021.
- 3. https://www.health.harvard.edu/diseases-and-conditions/what-are-the-longlasting-effects-of-covid-19.
- 4. Nuzzo, D., and P. Picone (2020), Potential neurological effects of severe COVID-19 infection, *Neuroscience Research*, 158, pp 1–5.
- 5. Wood, H. (2020), New insights into the neurological effects of COVID-19, *Nature Reviews Neurology*, June 26, 2020.

## **Source of Neurological** Effects One PDE Model

#### **1.1 INTRODUCTION**

COVID-19 neurological effects are generally described in the following introductory statement [2]:

While primarily a respiratory disease, COVID-19 can also lead to neurological problems. The first of these symptoms might be the loss of smell and taste, while some people also may later battle headaches, debilitating fatigue, and trouble thinking clearly, sometimes referred to as "brain fog". All of these symptoms have researchers wondering how exactly the coronavirus that causes COVID-19, SARS-CoV-2, affects the human brain.

This book focuses on a mathematical model describing a reduction in oxygen  $(O_2)$ to the brain resulting from impaired respiratory function of the lungs. The reduced brain  $O_2$  (hypoxia) decreases the population density of normal (healthy) neuron cells that then leads to brain cognitive impairment.

Patients who experience diminished  $O_2$  in the capillary blood to the brain resulting from respiratory impairment are sometimes termed "Covid long haulers", long haul Covids", or "long Covids".

Additional background concerning COVID-19 neurological effects is given in  $[1, 3, 4].$ 

#### **1.1.1 ONE PDE MODEL FORMULATION**

A mass balance on the  $O_2$  concentration in the capillary blood flowing in the brain follows (the balance is derived in chapter appendix A1):

$$
\frac{\partial u_1}{\partial t} = -v_z \frac{\partial u_1}{\partial z} - (2/r_l) k_{m1} (u_1 - u_{2n}) \tag{1.1-1}
$$

Equation  $(1.1-1)$  states that the time rate of change of the blood  $O_2$  concentration  $\left(\frac{\partial u_1}{\partial x}\right)$  equals the sum of the rate of convection of *O*  $\left(\frac{\partial u_1}{\partial t}\right)$  equals the sum of the rate of convection of  $O_2$  along the capillary  $\left(-v_z \frac{\partial u_1}{\partial z}\right)$  and the rate of transfer of  $O_2$  across the BBB (−(2/*r*  $\frac{\partial u_1}{\partial z}$  and the rate of transfer of  $O_2$  across the BBB  $(-(2/r_l)k_{m1}(u_1 - u_{2n}))$ .

#### **Table 1.1 PDE model variables, parameters**



Equation (1.1-1) is first order in *t* so that it requires oneinitial condition (IC).

$$
u_1(z, t = 0) = u_{1n} \tag{1.1-2}
$$

 $u_{1n}$  is the normalized blood  $O_2$  concentration used as an IC.

Equation (1.1-1) is first order in *z* and requires one boundary condition (BC).

$$
u_1(z = z_l, t) = u_{1e}(t)
$$
 (1.1-3)

Equations (1.1) constitute the one PDE model that is implemented in  $\mathbb{R}^1$  as explained in Chapter 2.

#### **1.1.2 SUMMARY AND CONCLUSIONS**

The one PDE model for  $O_2$  entering the brain through capillary blood flow consists of eqs.  $(1.1)$ . These equations are a test case with constant  $O_2$  concentration in the brain tissue adjacent to the BBB,  $u_{2n}$ . Equations (1.1) are implemented in R in Chapter 2. Variations in the brain tissue  $O_2$  concentration are considered in subsequent chapters through the addition of PDEs.

#### **APPENDIX A1: DERIVATION OF THE BLOOD** *O*<sup>2</sup> **BALANCE**

A mass balance on the blood with the incremental volume  $\pi r_l^2 \Delta z$  ( $r_l$  is the radius of the capillary) gives

$$
\pi r_l^2 \Delta z \frac{\partial u_1(z,t)}{\partial t} = \pi r_l^2 v_z(t) u_1(z,t) |_{z} - \pi r_l^2 v_z(t) u_1(z,t) |_{z + \Delta z} \n- 2\pi r_l \Delta z k_{m1}(u_1(z,t) - u_{n2})
$$
\n(A1-1)

The terms in eq. (A1-1) are

 ${}^{1}R$  is a quality, open source scientific programming system that is available for download through an Internet connection, http://www.r-project.org/, http://cran.fhcrc.org/.

- $\partial u_1($  $\pi r_1^2 \Delta z \stackrel{\partial u}{\longrightarrow}$  $\frac{2}{1} \Delta z \frac{\partial u_1(z,t)}{\partial t}$ •  $\pi r_1^2 \Delta z \frac{\partial u_1(z,t)}{\partial t}$ : accumulation of  $O_2$  in the incremental volume  $\pi r_1^2 \Delta z$ . If this term is negative (from the sum of the RHS terms), the  $O_2$  concentration decreases (is depleted) with time.
- $\pi r_1^2 v_z(z,t) u_1(z,t) \Big|_z$ : flow (convection) at velocity  $v_z^2$  of the  $O_2$  transported into the incremental volume at  $z (v_z > 0)$ .
- $-\pi r_1^2 v_z(t)u_1(z,t)|_{z+\Delta z}$ : flow (convection) at velocity  $v_z$  of the  $O_2$  transported out of the incremental volume at  $z + \Delta z$  ( $v_z > 0$ ).
- $-2\pi r_l \Delta z k_{m1}(u_1(z,t) u_{n2})$ : rate of mass transfer of  $O_2$  across the BBB. The transfer area is  $2\pi r_1\Delta z$  and the mass transfer coefficient (BBB permeability) is  $k_{m1}$ .

If this term is negative, the transfer is from the blood through the BBB into the brain tissue, which reduces  $\frac{\partial u_1(z,t)}{\partial x_i}$ reduces  $\frac{\partial u_1(x)}{\partial t}$ 

If eq. (A1-1) is divided by the incremental volume  $\pi r_1^2 \Delta z$  (the coefficient of  $\partial u_1(z,t)$  $\frac{\partial f(x, y)}{\partial t}$ , after minor rearrangement,

$$
\frac{\partial u_1(z,t)}{\partial t} = -\frac{v_z(t)u_1(z,t)|_{z+\Delta z} - v_z(t)u_1(z,t)|_z}{\Delta z} - \frac{2}{r_1}k_{m1}(u_1(z,t) - u_{n2})
$$
\n(A1-2)

For  $\Delta z \rightarrow 0$ , eq. (A1-2) becomes a PDE

$$
\frac{\partial u_1(z,t)}{\partial t} = -\frac{\partial v_z(t)u_1(z,t)}{\partial z} - \frac{2}{r_1}k_{m1}(u_1(z,t) - u_{n2})
$$
\n(A1-3)

Equation (A1-3) is eq. (1.1-1) with  $v_z(t) = v_z$  (a constant).

#### **REFERENCES**

- 1. Bridwell, R., B. Long and M. Gottlieb (2020), Neuorologic complications of COVID-19, *American Journal of Emergency Medicine*, 38, pp. 1549.e3–1549.e7.
- 2. Collins, F. (2021), Taking a closer look at COVID-19's effects on the brain, *NIH Director's Blog*, January 14, 2021.
- 3. Nuzzo, D. and P. Picone (2020), Potential neurological effects of severe COVID-19 infection, *Neuroscience Research*, 158, pp. 1–5.
- 4. Wood, H. (2020), New insights into the neurological effects of COVID-19, *Nature Reviews Neurology*, June 26, 2020.

 $^{2}v_{z}$  is assumed to be uniform (constant) across the capillary. This is an idealization since the velocity will have a radial profile with zero velocity at the capillary wall (the interface between the blood and the BBB inner surface) and a maximum velocity at the capillary centerline. *v<sup>z</sup>* is termed a *superficial velocity* with the property that multiplication by the capillary cross sectional area  $\pi r_1^2$  gives the blood volumetric flow rate in the capillary.



## 2 Implementation of the One PDE Model

#### **2.1 INTRODUCTION**

The one PDE model of Chapter 1 for the  $O_2$  in the capillary blood (eqs. (1.1)) is implemented in R routines discussed in this chapter.

#### **2.1.1 R ROUTINES FOR THE ONE PDE MODEL**

Equations  $(1.1)$  that constitute the PDE model for the  $O_2$  concentration in the capillary blood are implemented with the following R routines, starting with a main program.

#### **Main program for** *O*<sup>2</sup> **concentration**

The main program for eqs. (1.1) follows.

```
#
# One PDE model
#
# Delete previous workspaces
  rm(list=ls(all=TRUE))
#
# Access ODE integrator
  library("deSolve");
#
# Access functions for numerical solution
  setwd("f:/brain hypoxia/chap2");
  source("pde1a.R");
#
# Parameters
 nz=21;
  rl=1;
 km1=0;km1=1;
  vz=1;
  u1e=0.75;
  u1n=1;
  u2n=0;
#
# Spatial grid in z
```

```
zl=0;zu=1;dz=(zu-zl)/(nz-1);
  z=seq(from=zl,to=zu,by=dz);
#
# Independent variable for ODE integration
  t0=0; tf=1; nout=21;tout=seq(from=t0,to=tf,by=(tf-t0)/(nout-1));
#
# Initial condition (t=0)
  u0=rep(u1n,nz);
  ncall=0;
#
# ODE integration
  out=lsodes(y=u0,times=tout,func=pde1a,
      sparsetype="sparseint",rtol=1e-6,
      atol=1e-6,maxord=5);
  nrow(out)
  ncol(out)
#
# Arrays for plotting numerical solution
  u1=matrix(0,nrow=nz,ncol=nout);
  for(it in 1:nout){
    for(iz in 1:nz){
      u1[iz, it] = out[it, iz+1];}
  u1[1,it]=u1e;
  }
#
# Display numerical solution
  iv=seq(from=1,to=nout,by=4);
  for(it in iv){
    cat(sprintf("\n t z u1(z,t)\n\langle n");
    iv=seq(from=1,to=nz,by=2);
    for(iz in iv){
      cat(sprintf("%6.2f%6.2f%12.3e\n",
           tout[it],z[iz],u1[iz,it]));
    }
  }
#
# Calls to ODE routine
  cat(sprintf("\n\n ncall = \delta5d\n\n",ncall));
#
# Plot PDE solution
#
# u1
```

```
par(mfrow=c(1,1));matplot(x=z[2:nz],y=u1[2:nz,],type="l",xlab="z",ylab="u1(z,t)",
        xlim=c(zl,zu),lty=1,main="",lwd=2,col="black");
persp(z,tout,u1,theta=60,phi=45,
      xlim=c(z1,zu), ylim=c(t0,tf), zlim=c(0,1.1),
      xlab="z", ylabel="t",zlab="u1(z,t)");
```
Listing 2.1: Main program for eqs. (1.1)

We can note the following details about Listing 2.1.

• Previous workspaces are deleted.

```
#
# One PDE model
#
# Delete previous workspaces
 rm(list=ls(all=TRUE))
```
• The R ODE integrator library deSolve is accessed [2].

```
#
# Access ODE integrator
 library("deSolve");
#
# Access functions for numerical solution
 setwd("f:/brain hypoxia/chap2");
  source("pde1a.R");
```
Then the directory with the files for the solution of eqs. (1.1) is designated. Note that setwd (set working directory) uses  $/$  rather than the usual  $\backslash$ .

• The model parameters are specified numerically.

```
#
# Parameters
 nz=21;
  r = 1;
  km1=0;km1=1;vz=1;
  u1e=0.75;
  u1n=1;
  u2n=0;
```
where

- − nz: number of spatial grid points for eq. (1.1-1).
- − rl: radius of the blood capillary (and inner radius of the blood brain barrier (BBB))
- $-$  km1: mass transfer (permeability) coefficient for  $O_2$  across the BBB in eq. (1.1-1).  $k_m = 0$  was used initially during the development of the coding (programming). The mass transfer coefficient was then changed to  $k_m = 1$ .
- − vz: capillary blood flow superficial velocity in eq. (1.1-1).
- $-$  u1e: entering blood  $O_2$  concentration in BC (1.1-3).
- − u1n: normalized blood *O*<sup>2</sup> concentration in IC (1.1-2).
- − u2n: normalized brain tissue *O*<sup>2</sup> concentration in eq. (1.1-1).
- A spatial grid for eq.  $(1.1-1)$  is defined with 21 points so that  $z =$ 0,1/20=0.05,...,1. The BBB length is a normalized value,  $z = z_u = 1$ .

```
#
# Spatial grid in z
  z1=0;zu=1;dz=(zu-zl)/(nz-1);
  z=seq(from=zl,to=zu,by=dz);
```
• An interval in *t* is defined for 21 output points so that tout=0, 1/20=0.05,  $\dots$ , 1. The time scale is normalized with  $t_f = 1$  specified as the final time that is considered appropriate, e.g., day, week, and month.

```
#
# Independent variable for ODE integration
  t0=0; tf=1; nout=21;tout=seq(from=t0,to=tf,by=(tf-t0)/(nout-1));
```
• IC (1.1-2) is implemented, with  $u_{1n} = u1n$  defined previously as a parameter.

```
#
# Initial condition (t=0)
  u0=rep(u1n,nz);
  ncall=0;
```
Also, the counter for the calls to pde1a is initialized.

• The system of nz=21 ODEs is integrated by the library integrator 1 sodes (available in deSolve, [2]). As expected, the inputs to lsodes are the ODE function, pde1a, the IC vector u0, and the vector of output values of *t*, tout. The length of u0 (21) informs lsodes how many ODEs are to be integrated. func,y,times are reserved names.

```
#
# ODE integration
  out=lsodes(y=u0,times=tout,func=pde1a,
      sparsetype="sparseint",rtol=1e-6,
      atol=1e-6,maxord=5);
 nrow(out)
 ncol(out)
```
nrow,ncol confirm the dimensions of out.

•  $u_1(z,t)$  is placed in a matrix for subsequent plotting.

```
#
# Arrays for plotting numerical solution
  u1=matrix(0,nrow=nz,ncol=nout);
  for(it in 1:nout){
    for(iz in 1:nz){
      u1[iz, it] = out[it, iz+1];}
  u1[1, it] = u1e;}
```
The offset +1 is required because the first element of the solution vectors in out is the value of *t* and the 2 to 22 elements are the 21 values of *u*1. These dimensions from the preceding calls to nrow,ncol are confirmed in the subsequent output.

• The numerical values of  $u_1(z,t)$  returned by 1 sodes are displayed. Every fourth value in *t* and every second value in *z* appear from by=4,2.

```
#
# Display numerical solution
  iv=seq(from=1,to=nout,by=4);
  for(it in iv){
    cat(sprintf("\n t z u1(z,t)\n\langle n");
    iv=seq(from=1,to=nz,by=2);
    for(iz in iv){
       cat(sprintf("%6.2f%6.2f%12.3e\n",
             \text{tout}[\text{it}],\text{z}[\text{iz}],\text{u1}[\text{iz},\text{it}]),}
  }
```
• The number of calls to pde1a is displayed at the end of the solution.

```
#
# Calls to ODE routine
  cat(sprintf("\n\n ncall = %5d\n\n",ncall));
```
•  $u_1(z,t)$  is plotted in 2D against *z* and parametrically in *t* with the R utility matplot and in 3D with R utility persp. par  $(mfrow=c(1,1))$  specifies a  $1 \times 1$  matrix of plots, that is, one plot on a page.

```
#
# Plot PDE solution
#
# 111par(mfrow=c(1,1));
  matplot(x=z[2:nz],y=u1[2:nz,],type="l",xlab="z",
          ylab="u1(z,t)",xlim=c(zl,zu),lty=1,main="",lwd=2,
          col="black");
  persp(z,tout,u1,theta=60,phi=45,
        xlim=c(zl,zu),ylim=c(t0,tf),zlim=c(0,1.1),
        xlab="z", ylabel="t",zlab="u1(z,t)");
```
This completes the discussion of the main program for eqs. (1.1). The ODE/MOL routine pde1a called by lsodes from the main program for the numerical MOL integration of eqs. (1.1) is next.

#### **ODE/MOL routine**

pde1a called in the main program of Listing 2.1 follows.

```
pde1a=function(t,u,parm){
#
# Function pde1a computes the t derivative
# of u1(z,t)#
# One vector to one vector
 u1=rep(0,nz);for(iz in 1:nz){
    u1[iz]=u[iz];#
# BC, z=zl
 u1[1] = u1e;#
# PDE
 ut=rep(0,nz);for(iz in 1:nz){
    if(iz==1){u1t[iz]=0;}
    if(iz>1){
      u1t[iz] = -vz*(u1[iz]-u1[iz-1])/dz -(2/r1)*km1*(u1[iz]-u2n);}
```

```
#
# One vector to one vector
 ut=rep(0,nz);
 for(iz in 1:nz){
    ut[iz]=u1t[iz];#
# Increment calls to pde1a
 ncall <<- ncall+1;
#
# Return derivative vector
 return(list(c(ut)));
 }
```
Listing 2.2: ODE/MOL routine for eqs. (1.1)

We can note the following details about Listing 2.2.

The function is defined.

```
pde1a=function(t,u,parm){
#
# Function pde1a computes the t derivative
# of u1(z,t)
```
t is the current value of *t* in eqs. (1.1). u is the 21-vector of ODE/PDE dependent variables. parm is an argument to pass parameters to pde1a (unused, but required in the argument list). The arguments must be listed in the order stated to properly interface with lsodes called in the main program of Listing 2.1. The derivative vector of the LHS of eq. (1.1-1) is calculated and returned to lsodes as explained subsequently.

• BC  $(1.1-3)$  is programmed.

```
#
# BC, z=zl
  u1[1]=u1e;
```
• Equation  $(1.1-1)$  is programmed.

```
#
# PDE
  u1t=rep(0,nz);
  for(iz in 1:nz){
    if(iz==1){u1t[iz]=0;}
    if(iz>1){
      u1t[iz] = -vz*(u1[iz]-u1[iz-1])/dz -(2/rl)*km1*(u1[iz]-u2n);}
  }
```
The derivative  $\frac{\partial u_1}{\partial z}$  in eq. (1.1-1) is approximated with a two-point upwind finite difference (FD).

$$
\frac{\partial u_1(z,t)}{\partial z} \approx \frac{u_1(z,t) - u_1(z - \Delta z, t)}{\Delta z} + O(\Delta z)
$$

programmed as

(u1[iz]-u1[iz-1])/dz

 $O(\Delta z)$  indicates that the error in the FD approximation is first order in  $\Delta z$ . The variation in the numerical solution of eq.  $(1.1-1)$  can be studied as a function of the FD increment ∆*z* by varying nz in Listing 2.1. Alternate approximations for the axial derivative  $\frac{\partial u_1}{\partial z}$  are considered in Appendix A and [1].

For  $z = z_l$ , BC (1.1-3) sets the value of  $u_1(z = z_l, t)$  and therefore the derivative is set to zero (if(iz==1)u1t[iz]=0;) to ensure the boundary value is maintained.

The correspondence of the programming with eq.  $(1.1-1)$  is an important feature of the MOL.

• The 21 ODE derivatives are placed in the vector ut for return to 1 sodes to take the next in *t* along the solution.

```
#
# One vector to one vector
  ut=rep(0, nz);for(iz in 1:nz){
    ut[iz]=u1t[iz];
```
• The counter for the calls to pde1a is incremented and returned to the main program of Listing 2.1 by  $\lt\lt$ -.

```
#
# Increment calls to pde1a
  ncall <<- ncall+1;
```
• The vector ut is returned as a list as required by lsodes. c is the R vector utility. The final } concludes pde1a.

```
#
# Return derivative vector
  return(list(c(ut)));
  }
```
This completes the discussion of pde1a. The output from the main program of Listing 2.1 and ODE/MOL routine pde1a of Listing 2.2 is considered next.

#### **Numerical, graphical output**

The numerical output is given in Table 2.1.

[1] 21 [1] 22 t  $z$   $u1(z,t)$ 0.00 0.00 7.500e-01 0.00 0.10 1.000e+00 0.00 0.20 1.000e+00 0.00 0.30 1.000e+00 0.00 0.40 1.000e+00 0.00 0.50 1.000e+00 0.00 0.60 1.000e+00 0.00 0.70 1.000e+00 0.00 0.80 1.000e+00 0.00 0.90 1.000e+00 0.00 1.00 1.000e+00 t  $z$   $u1(z,t)$ 0.20 0.00 7.500e-01 0.20 0.10 6.401e-01 0.20 0.20 6.187e-01 0.20 0.30 6.449e-01 0.20 0.40 6.635e-01 0.20 0.50 6.692e-01 0.20 0.60 6.702e-01 0.20 0.70 6.703e-01 0.20 0.80 6.703e-01 0.20 0.90 6.703e-01 0.20 1.00 6.703e-01 . .  $\bullet$  . <br> <br> . <br> <br> . <br> <br> <br> <br> <br> <br><br><br> <br><br><br> . <br> <br> . <br> <br> <br> <br> <br> <br> <br> <br><br><br><br><br><br><br><br><br><br><br> Output for  $t = 0.4$ , 0.6, 0.8 removed . <br> <br> . <br> <br> <br> <br> <br> <br> <br> <br><br><br><br><br><br><br><br> . <br> <br> . <br> <br> <br> <br> <br> <br> <br> <br><br><br><br><br><br><br><br> . <br> <br> . <br> <br> <br> <br> <br> <br> <br> <br><br><br><br><br><br><br><br><br><br><br> t  $z$   $u1(z,t)$ 1.00 0.00 7.500e-01 1.00 0.10 6.198e-01 1.00 0.20 5.123e-01



```
ncall = 113
```
Table 2.1: Numerical output from Listings 2.1, 2.2

We can note the following details about this output.

- 21 *t* output points as the first dimension of the solution matrix out from lsodes as programmed in the main program of Listing 2.1 (with nout=21).
- The solution matrix out returned by 1 sodes has 22 elements as a second dimension. The first element is the value of *t*. Elements 2 to 22 are  $u_1(z,t)$ from eqs. (1.1) (for each of the 21 output points).
- The solution is displayed for  $t=0,1/20=0.05,...,1$  as programmed in Listing 2.1 (every fourth value of *t* is displayed as explained previously).
- The solution is displayed for  $z=0,1/20=0.05,...,1$  as programmed in Listing 2.1 (every second value of *z* is displayed as explained previously).
- IC (1.1-2) is confirmed  $(t = 0)$ .
- BC (1.1-3) is confirmed ( $t = 0, z = z_l = 0$ ). There is a discontinuous change from the IC  $(t = 0)$  to the BC  $(t > 0)$ , which is subsequently smoothed, e.g.,  $t = 0.2$ . To improve the appearance of the graphical output (Figure 2.1-1 considered next), the output does not include the solution at  $z = z_l = 0$  (matplot (x=z[2:nz], y=u1[2:nz,],... in Listing 2.1). Use of Listings 2.1, 2.2 with the solution at  $z = z_l = 0$  included is left as an exercise.
- The computational effort as indicated by  $ncall = 113$  is modest so that lsodes computed the solution to eqs. (1.1) efficiently.

The graphical output is in Figures 2.1.

The solution  $u_1(z,t)$  starts from IC (1.1-2), and confirms BC (1.1-3). In general,  $u_1(z,t)$  is a front moving left to right (as expected with  $v_z > 0$ ) in response to the reduced entering  $O_2$  concentration,  $u_1(z = z_l = 0, t) = u_{1e} = 0.75$ .

Figure 2.1-2 reflects the decreasing blood  $O_2$  concentration with *t*.

Two special cases can be considered to confirm the model and coding:

- $v_z = 0$ : With no blood flood,  $u_1(z,t)$  remains at IC (1.1-2).
- $k_{m1} = 0$ : With no  $O_2$  transfer through the BBB,  $u_1(z, t \to \infty) = u_{1e}$  ( $t_f = 2$ ) indicates the solution for large *t*.

These cases are left as exercises.



**Figure 2.1-1**  $u_1(z,t)$  from eqs. (1.1), 2D.

#### **2.1.2 SUMMARY AND CONCLUSIONS**

The one PDE model for blood  $O_2$  concentration,  $u_1(z,t)$  defined by eqs. (1.1), is implemented within the MOL. Parameters in this model are defined numerically in Listing 2.1 and can be used to investigate dynamic effects, e.g., the blood convection with  $v_z$ , mass transfer through the BBB with  $k_{m1}$ .



**Figure 2.1-2**  $u_1(z,t)$  from eqs. (1.1), 3D.

For this prototype code, which is intended to explain the computer implementation with the main program of Listing 2.1 and ODE/MOL routine of Listing 2.2, the brain tissue  $O_2$  concentration is constant ( $u_{2n} = 0$  in eq. (1.1-1)). The model is now extended to include a second PDE for the brain tissue  $O_2$  concentration,  $u_2(z,t)$ .

#### **REFERENCES**

- 1. Schiesser, W.E. (2019), *Numerical PDE Analysis of the Blood Brain Barrier*, World Scientific Publishing Co., Singapore.
- 2. Soetaert, K., J. Cash, and F. Mazzia (2012), *Solving Differential Equations in R*, Springer-Verlag, Heidelberg, Germany.

# 3 Two PDE Model

#### **3.1 INTRODUCTION**

The one PDE model of Chapter 1, eqs. (1.1), is extended in this chapter by adding a PDE for the brain tissue  $O_2$  concentration,  $u_2(z,t)$ . Equation (1.1-1) for  $u_1(z,t)$  is also modified to include  $u_2(z,t)$ .

#### **3.1.1 TWO PDE MODEL FORMULATION**

Equations (1.1) are restated with  $u_2(z,t)$  included.

$$
\frac{\partial u_1}{\partial t} = -v_z \frac{\partial u_1}{\partial z} - (2/r_l) k_{m1} (u_1 - u_2)
$$
\n(3.1-1)

$$
u_1(z, t = 0) = u_{1n} \tag{3.1-2}
$$

$$
u_1(z = z_l, t) = u_{1e}(t) \tag{3.1-3}
$$

A mass balance on the  $O_2$  concentration in the brain tissue follows (the balance is derived in chapter appendix A3):

$$
\frac{\partial u_2}{\partial t} = D_2 \frac{\partial^2 u_2}{\partial z^2} + \frac{2r_l}{(r_u^2 - r_l^2)} k_{m1}(u_1 - u_2)
$$
 (3.2-1)

Equation  $(3.2-1)$  states that the time rate of change of the brain tissue  $O_2$  concentration  $\left(\frac{\partial u_2}{\partial t}\right)$  equals the sum of the rate of axial diffusion of  $O_2$  along the brain tissue  $\left(\frac{\partial^2 u_2}{\partial x_1}, \frac{\partial^2 u_3}{\partial y_2}\right)$  and the rate of transform f  $\Omega$  corresponds **PPP**  $\begin{pmatrix} 2r_1 & 0 & \dots & 0 \\ 0 & 2r_1 & 0 & \dots & 0 \end{pmatrix}$  $D_2 \frac{\partial^2 u_2}{\partial z^2}$  and the rate of transfer of  $O_2$  across the BBB  $\left(\frac{2r_l}{\partial z^2}k_{m1}(u_1-u)\right)$  $\partial z$ and the rate of transfer of  $O_2$  across the BBB  $\left(\frac{2r_l}{(r_u^2 - r_l^2)} k_{m1}(u_1 - u_2)\right)$ .

 $D_2$  is the effective diffusivity (dispersion coefficient) for  $O_2$  in the axial (longitudinal *z*) direction. Radial (transverse to *z*) variation of  $O_2$  has been neglected, which implies a narrow radial dimension so that the  $O_2$  concentration is effectively uniform in the radial direction<sup>1</sup>.

Equation (3.2-1) is first order in *t* so that it requires one initial condition (IC).

$$
u_2(z, t = 0) = u_{2n} \tag{3.2-2}
$$

 $u_{2n}$  is the normalized brain tissue  $O_2$  concentration used as an IC.

Equation (3.2-1) is second order in *z* and requires two boundary conditions (BCs).

$$
\frac{\partial u_2(z=z_l,t)}{\partial z} = \frac{\partial u_2(z=z_u,t)}{\partial z} = 0
$$
\n(3.2-3,4)

<sup>&</sup>lt;sup>1</sup>Radial variation of  $O_2$  in the brain tissue can be analyzed by the methodology discussed in [1].

Equations (3.2-3,4) are homogeneous (zero) Neumann BCs for zero flux at the boundaries of the brain tissue.

Equations  $(3.1)$ ,  $(3.2)$  constitute the two PDE model that is implemented in R, as explained in Chapter 4.

#### **3.1.2 SUMMARY AND CONCLUSIONS**

Equations (3.1), (3.2) are the two PDE model for  $O_2$  in the capillary blood flow and brain tissue. The transfer of  $O_2$  across the BBB is represented with the terms  $\pm k_{m1}(u_1 - u_2)$  which can be used to study the effects of reduced  $O_2$  from the blood stream to the brain tissue resulting from pulmonary impairment (through variation of  $k_{m1}$ ).

The implementation of eqs. (3.1), (3.2) is considered in Chapter 4.

#### **APPENDIX A3: DERIVATION OF THE BRAIN TISSUE** *O*<sup>2</sup> **BALANCE**

A mass balance on the brain tissue with the incremental volume  $(\pi r_u^2 - \pi r_l^2) \Delta z$  ( $r_l$ ,  $r_u$ are the inner and outer radial boundaries of the brain tissue, respectively) gives

$$
(\pi r_u^2 - \pi r_l^2) \Delta z \frac{\partial u_2(z,t)}{\partial t} = (\pi r_u^2 - \pi r_l^2) \left( -D_2 \frac{\partial u_2(z,t)}{\partial z} \Big|_z + D_2 \frac{\partial u_2(z,t)}{\partial z} \Big|_{z+\Delta z} \right) + 2\pi r_l \Delta z k_{m1} (u_1(z,t) - u_2(z,t))
$$
 (A3.1)

The terms in eq. (A3.1) are

- $\frac{(\pi r_u^2 \pi r_l^2) \Delta z \frac{\partial u_2(z,t)}{\partial t}}{2}$ : accumulation of *O*<sub>2</sub> in the incremental volume  $(\pi r_u^2 - \pi r_l^2) \Delta z$ . If this term is negative (from the sum of the RHS terms), the  $O_2$  concentration decreases (is depleted) with time.
- $\sqrt{ }$  $\setminus$  $\bullet$   $(\pi r_u^2 - \pi r_l^2) \left(-D_2 \frac{\partial u}{\partial r_l}\right)$  $\int_{l}^{2} \left( -D_{2} \frac{\partial u_{2}(z,t)}{\partial z} | z \right)$ : rate of diffusion of *O*  $\frac{2(x, y)}{\partial z}|z$  is rate of diffusion of  $O_2$  in the brain tissue at *z*. This term is based on Fick's first law

$$
q = -D_2 \frac{\partial u_2(z, t)}{\partial z} \tag{A3.2}
$$

- $\int_{\mathbb{R}} \partial u_2(z,t)$ •  $(\pi r_u^2 - \pi r_l^2) \left(D_2 \frac{\partial u_2(z,t)}{\partial z}|_{z+\Delta z}\right)$ : rate of diffusion of  $O_2$  in the brain tissue at  $z + \Delta z$ .
- $2\pi r_l \Delta z k_{m1}(u_1(z,t) u_2(z,t))$ : rate of mass transfer of the  $O_2$  transported between the capillary and the inner surface of the BBB. The transfer area is  $2\pi r_1 \Delta z$  and the mass transfer coefficient is  $k_{m1}$ .

If eq. (A3.1) is divided by the incremental volume  $(\pi r_u^2 - \pi r_l^2) \Delta z$  (the coefficient of  $\partial u_2(z,t)$  $\frac{\partial \phi(x, y)}{\partial t}$ ), after minor rearrangement,

$$
\frac{\partial u_2(z,t)}{\partial t} = \frac{D_2 \frac{\partial u_2(z,t)}{\partial z}|_{z+\Delta z} - D_2 \frac{\partial u_2(z,t)}{\partial z}|_z}{\Delta z} + \frac{2r_l}{(r_u^2 - r_l^2)} k_{m1}(u_1(z,t) - u_2(z,t))
$$
(A3.3)

For  $\Delta z \rightarrow 0$ , eq. (A3.3) becomes

$$
\frac{\partial u_2(z,t)}{\partial t} = D_2 \frac{\partial^2 u_2(z,t)}{\partial z^2} + \frac{2r_l}{(r_u^2 - r_l^2)} k_{m1}(u_1(z,t) - u_2(z,t)) \tag{A3.4}
$$

Equation (A3.4) is eq. (3.2-1).

#### **REFERENCE**

1. Schiesser, W.E. (2019), *Numerical PDE Analysis of the Blood Brain Barrier*, World Scientific Publishing Co., Singapore.



## 4 Implementation of the Two PDE Model

#### **4.1 INTRODUCTION**

The two PDE model of Chapter 3 for  $O_2$  in the capillary blood (eqs.  $(3.1)$ ) and the brain tissue (eqs. (3.2)) is implemented in R routines as discussed in this chapter.

#### **4.1.1 R ROUTINES FOR THE TWO PDE MODEL**

Equations (3.1), (3.2) for the  $O_2$  concentration in the capillary blood and brain tissue are implemented with the following R routines, starting with a main program.

#### **Main program**

The main program for eqs. (3.1), (3.2) follows:

```
#
# Two PDE model
#
# Delete previous workspaces
  rm(list=ls(all=TRUE))
#
# Access ODE integrator
  library("deSolve");
#
# Access functions for numerical solution
  setwd("f:/brain hypoxia/chap4");
  source("pde2a.R");
#
# Parameters
 nz=21;
  r = 1;ru=2;
  D2=0.1;
 km1=0;
  km1=10;
  vz=1;u1e=0.75;
  u1n=1;
  u2n=1;
#
```

```
# Constants
  r1=2/rl;
  r2=(2*r1)/(ru^2-rl^2);#
# Spatial grid in z
  z1=0; zu=1; dz=(zu-z1)/(nz-1); dzs=dz^2;z=seq(from=zl,to=zu,by=dz);
#
# Independent variable for ODE integration
 t0=0; t f=1; nout=21;tout=seq(from=t0,to=tf,by=(tf-t0)/(nout-1));
#
# Initial condition (t=0)
 u0 = rep(0, 2*nz);for(iz in 1:nz){
   u0[iz] = u1n;u0[iz+nz]=u2n;
  }
 ncall=0;
#
# ODE integration
  out=lsodes(y=u0,times=tout,func=pde2a,
      sparsetype="sparseint",rtol=1e-6,
      atol=1e-6,maxord=5);
  nrow(out)
 ncol(out)
#
# Arrays for plotting numerical solution
  u1=matrix(0,nrow=nz,ncol=nout);
  u2=matrix(0,nrow=nz,ncol=nout);
  for(it in 1:nout){
    for(iz in 1:nz){
      u1[iz, it] = out[it, iz+1];u2[iz, it] = out[it, iz+1+nz];}
  u1[1, it] = u1e;}
#
# Display numerical solution
  iv=seq(from=1,to=nout,by=4);
  for(it in iv){
    cat(sprintf("\n t z u1(z,t) u2(z,t)\n\langle n''\rangle;
    iv=seq(from=1,to=nz,by=2);
    for(iz in iv){
```

```
cat(sprintf("%6.2f %6.2f %12.3e %12.3e\n",
          tout[it],z[iz],u1[iz,it],u2[iz,it]));
    }
  }
#
# Calls to ODE routine
  cat(sprintf("\n\n ncall = \delta5d\n\n",ncall));
#
# Plot PDE solution
#
# u1
  par(mfrow=c(1,1));matplot(x=z[2:nz],y=u1[2:nz,],type="l",xlab="z",ylab="u1(z,t)",
          xlim=c(zl,zu),lty=1,main="",lwd=2,col="black");
  persp(z,tout,u1,theta=60,phi=45,
        xlim=c(z1,zu), ylim=c(t0,tf), zlim=c(0,1.1),
        xlab="z", ylab="t", zlab="u1(z,t)");
#
# u2
  par(mfrow=c(1,1));
  matplot(x=z,y=u2,type="l",xlab="z",ylab="u2(z,t)",
          xlim=c(zl,zu),lty=1,main="",lwd=2,col="black");
  persp(z,tout,u2,theta=60,phi=45,
        xlim=c(zl,zu),ylim=c(t0,tf),zlim=c(0,1.1),
        xlab="z",ylab="t",zlab="u2(z,t)");
```
Listing 4.1: Main program for eqs. (3.1), (3.2)

We can note the following details about Listing 4.1 (with some repetition of the discussion of Listing 2.1 so that the explanation is self-contained).

• Previous workspaces are deleted.

```
#
# Two PDE model
#
# Delete previous workspaces
  rm(list=ls(all=TRUE))
```
• The R ODE integrator library deSolve is accessed [3].

```
#
# Access ODE integrator
 library("deSolve");
#
# Access functions for numerical solution
```

```
setwd("f:/brain hypoxia/chap4");
source("pde2a.R");
```
Then the directory with the files for the solution of eqs.  $(3.1)$ ,  $(3.2)$  is designated. Note that setwd (set working directory) uses / rather than the usual  $\backslash$ .

The model parameters are specified numerically.

```
#
# Parameters
  nz=21;
  r = 1;
  ru=2;
  D2=0.1;
  km1=0;km1=10;
  vz=1:
  u1e=0.75;
  u1n=1;
  u2n=1;
```
where

- − nz: number of spatial grid points for eqs. (3.1-1), (3.2-1).
- − rl: radius of the blood capillary and inner radius of the blood brain barrier (BBB). The wall thickness of the BBB is neglected so  $r_l = r_l$  also designates the inner boundary of the brain tissue.
- − ru: outer boundary of the brain tissue, *r<sup>u</sup>* = ru.
- − *D*2: *O*<sup>2</sup> diffusivity of the brain tissue in eq. (3.2-1).
- − km1: mass transfer (permeability) coefficient for *O*<sup>2</sup> across the BBB in eqs. (3.1-1), (3.2-1). For  $k_m = 0$ ,  $O_2$  is not transferred from the capillary blood to the brain tissue, so the latter remains at the IC of eq. (3.2-2),  $u_2(z,t=0) = u_{2n}$ .

To further explain this special case, BCs (3.2-3,4) are consistent with the constant solution in *z*,  $u_2(z,t=0) = u_{2n} = u_2(z,t>0)$ .  $\partial^2 u$ Also, for a constant solution in *z*,  $\frac{\partial^2 u_2}{\partial z^2} = 0$  in eq. (3.2-1). Thus, the RHS terms of eq. (3.2-1) are zero (with  $k_{m1} = 0$ ) so  $\frac{\partial u_2}{\partial x} = 0$ ∂*t* (from eq.  $(3.2-1)$ ), and the solution remains at IC eq.  $(3.2-2)$ .

This special case is an important check since a departure of  $u_2(z,t)$  from IC would indicate a coding error (in pde2a of Listing 4.2 that follows). This special case is left as an exercise.

- − vz: capillary blood flow superficial velocity in eq. (3.1-1).
- − u1e: entering blood *O*<sup>2</sup> concentration in BC (3.1-3).
- − u1n: normalized blood *O*<sup>2</sup> concentration in IC (3.1-2).
- − u2n: normalized brain tissue *O*<sup>2</sup> concentration in IC (3.2-2).

• The constants  $r_1 = \frac{2}{r_1}$ ,  $r_2 = \frac{2r_1}{(r_u^2 - r_1^2)}$  are computed for use in the ordinary differential equation/method of lines (ODE/MOL) routine pde2a.

```
#
# Constants
  r1=2/rl;
  r2=(2*r1)/(ru^2-rl^2);
```
• A spatial grid for eqs.  $(3.1-1)$ ,  $(3.2-1)$  is defined with 21 points so that  $z = 0,1/20=0.05,...,1$ . The BBB length is a normalized value,  $z =$  $z_u = 1$ .

```
#
# Spatial grid in z
  z1=0; zu=1; dz=(zu-z1)/(nz-1); dzs=dz^2;z=seq(from=zl,to=zu,by=dz);
```
• An interval in *t* is defined for 21 output points so that tout=0, 1/20=0.05,  $\dots$ , 1. The time scale is normalized with  $t_f = 1$  specified as the final time that is considered appropriate, e.g., day, week, or month.

```
#
# Independent variable for ODE integration
  t0=0;tf=1;nout=21;
  tout=seq(from=t0,to=tf,by=(tf-t0)/(nout-1));
```
• ICs  $(3.1-2)$ ,  $(3.2-2)$  are implemented  $(u1n, u2n)$  are defined previously as parameters).

```
#
# Initial condition (t=0)
 u0=rep(0,2*nz);
  for(iz in 1:nz){
    u0[iz] = u1n;u0[iz+nz]=u2n;}
 ncall=0;
```
Also, the counter for the calls to ode2a is initialized.

• The system of 2\*nz=42 ODEs is integrated by the library integrator lsodes (available in deSolve, [3]). As expected, the inputs to lsodes are the ODE function, pde2a, the IC vector u0, and the vector of output values of *t*, tout. The length of u0 (42) informs lsodes how many ODEs are to be integrated. func,y,times are reserved names.

```
#
# ODE integration
  out=lsodes(y=u0,times=tout,func=pde2a,
      sparsetype="sparseint",rtol=1e-6,
      atol=1e-6,maxord=5);
  nrow(out)
 ncol(out)
```
nrow,ncol confirm the dimensions of out.

•  $u_1(z,t)$ ,  $u_2(z,t)$  are placed in matrices for subsequent plotting.

```
#
# Arrays for plotting numerical solution
  u1=matrix(0,nrow=nz,ncol=nout);
  u2=matrix(0,nrow=nz,ncol=nout);
  for(it in 1:nout){
    for(iz in 1:nz){
      u1[iz,it]=out[it,iz+1];
      u2[iz, it] = out[it, iz+1+nz];}
  u1[1, it] = u1e;}
```
The offset +1 is required because the first element of the solution vectors in out is the value of *t* and the 2 to 43 elements are the 42 values of  $u_1, u_2$ . These dimensions from the preceding calls to nrow,ncol are confirmed in the subsequent output.

• The numerical values of  $u_1(z,t)$ ,  $u_2(z,t)$  returned by 1 sodes are displayed. Every fourth value in *t* and every second value in *z* appear from by=4,2.

```
#
# Display numerical solution
 iv=seq(from=1,to=nout,by=4);
 for(it in iv){
   cat(sprint(f''\n t z u1(z,t) u2(z,t)\n^n));iv=seq(from=1,to=nz,by=2);
   for(iz in iv){
     cat(sprintf("%6.2f %6.2f %12.3e %12.3e\n",
         tout[it],z[iz],u1[iz,it],u2[iz,it]));
   }
 }
```
• The number of calls to pde2a is displayed at the end of the solution.

```
#
# Calls to ODE routine
  cat(sprintf("\n\n ncall = %5d\n\n",ncall));
```
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•  $u_1(z,t)$ ,  $u_2(z,t)$  are plotted in 2D against *z* and parametrically in *t* with the R utility matplot and in 3D with R utility persp. par(mfrow=c(1,1)) specifies a  $1 \times 1$  matrix of plots, that is, one plot on a page.

```
#
# Plot PDE solutions
#
# u1
 par(mfrow=c(1,1));matplot(x=z[2:nz],y=u1[2:nz],type="1",xlab="z",ylab="u1(z,t)",xlim=c(zl,zu),lty=1,main="",lwd=2,
          col="black");
  persp(z,tout,u1,theta=60,phi=45,
        xlim=c(z1,zu), ylim=c(t0,tf), zlim=c(0,1.1),
        xlab="z", ylab="t", zlab="u1(z,t)");
#
# u2
 par(mfrow=c(1,1));matplot(x=z,y=u2,type="1",xlab="z",ylab="u2(z,t)",xlim=c(zl,zu),lty=1,main="",lwd=2,col="black");
  persp(z,tout,u2,theta=60,phi=45,
        xlim=c(z1,zu), ylim=c(t0,tf), zlim=c(0,1.1),
        xlab="z", ylabel="t",zlab="u2(z,t)");
```
The 2D plot of  $u_1(z,t)$  does not include the discontinuous change from IC  $(3.1-2)$  to BC  $(3.1-3)$ ,  $x=z[2:nz]$ ,  $y=u1[2:nz]$ . This discontinuity is not included in  $u_2(z,t)$ , so the solution at  $z = z_l$  is included,  $x = z$ ,  $y = u^2$ .

This completes the discussion of the main program for eqs. (3.1), (3.2). The ODE/MOL routine pde2a called by lsodes from the main program for the numerical MOL integration of eqs. (3.1), (3.2) is discussed in the following section.

#### **ODE/MOL routine**

pde2a called in the main program of Listing 4.1 follows:

```
pde2a=function(t,u,parm){
#
# Function pde2a computes the t derivatives
# of u1(z,t), u2(z,t)#
# One vector to two vectors
 u1=rep(0,nz);u2=rep(0,nz);for(iz in 1:nz){
    u1[iz]=u[iz];
```
```
u2[iz]=u[iz+nz];}
#
# BC, z=zl
 u1[1]=u1e;
#
# PDEs
 ut=rep(0,nz);for(iz in 1:nz){
    if(iz==1){u1t[1]=0;}
    if(iz>1){
      u1t[iz]=-vz*(u1[iz]-u1[iz-1])/dz-
        r1*km1*(u1[iz]-u2[iz]);}
 u2t=rep(0,nz);for(iz in 1:nz){
    if(iz==1){
      u2t[1]=
        2*D2*(u2[2]-u2[1])/dzs+
        r2*km1*(u1[1]-u2[1]);if(iz == nz)u2t[nz]=
        D2*2*(u2[nz-1]-u2[nz])/dzs+
        r2*km1*(u1[nz]-u2[nz]);}
    if((iz>1)&&(iz<nz)){
      u2t[iz]=
        D2*(u2[iz+1]-2*u2[iz]+u2[iz-1])/dzs+
        r2*km1*(u1[iz]-u2[iz]);}
 }
#
# Two vectors to one vector
 ut=rep(0,2*nz);for(iz in 1:nz){
    ut[iz] =u1t[iz];
    ut[iz+nz]=u2t[iz];}
#
# Increment calls to pde2a
 ncall <<- ncall+1;
#
# Return derivative vector
 return(list(c(ut)));
 }
```
We can note the following details about Listing 4.2.

The function is defined.

```
pde2a=function(t,u,parm){
#
# Function pde2a computes the t derivatives
# of u1(z,t), u2(z,t)
```
t is the current value of *t* in eqs. (3.1), (3.2). u is the 42-vector of ODE/PDE dependent variables. parm is an argument to pass parameters to pde2a (unused, but required in the argument list). The arguments must be listed in the order stated to properly interface with lsodes called in the main program of Listing 4.1. The derivative vector of the LHS of eqs. (3.1-1), (3.2-1) is calculated and returned to lsodes as explained subsequently.

• u is placed in two vectors to facilitate the programming of eqs.  $(3.1)$ ,  $(3.2)$ .

```
#
# One vector to two vectors
 u1=rep(0,nz);
 u2=rep(0,nz);
  for(iz in 1:nz){
    u1[iz]=u[iz];u2[iz]=u[iz+nz];}
```
• BC  $(3.1-3)$  is programmed.

```
#
# BC, z=zl
  u1[1]=u1e;
```
• Equation  $(3.1-1)$  is programmed.

```
#
# PDEs
 ut=rep(0,nz);for(iz in 1:nz){
    if(iz==1){u1t[1]=0;}
    if(iz>1)u1t[iz] = -vz*(u1[iz]-u1[iz-1])/dz -r1*km1*(u1[iz]-u2[iz]);}
```
The derivative  $\frac{\partial u_1}{\partial z}$  in eq. (3.1-1) is approximated with a two point upwind finite difference (FD).

$$
\frac{\partial u_1(z,t)}{\partial z} \approx \frac{u_1(z,t) - u_1(z - \Delta z, t)}{\Delta z} + O(\Delta z)
$$

programmed as

$$
(u1[iz]-u1[iz-1])/dz
$$

 $O(\Delta z)$  indicates that the error in the FD approximation is first order in  $\Delta z$ . The variation in the numerical solution of eq. (3.1-1) can be studied as a function of the FD increment ∆*z* by varying nz in Listing 4.1. Alternate approximations for the axial derivative  $\frac{\partial u_1}{\partial z}$  are considered in [2]. For  $z = z_l$ , BC (3.1-3) sets the value of  $u_1(z = z_l, t)$ , and therefore, the derivative is set to zero (if(iz==1)u1t[1]=0;) to ensure the boundary value is maintained.

• Equation  $(3.2-1)$  is programmed.

```
u2t=rep(0,nz);for(iz in 1:nz){
  if(iz==1){
    u2t[1]=
      2*D2*(u2[2]-u2[1])/dzs+
      r2*km1*(u1[1]-u2[1]);if(iz == nz){
    u2t[nz]=D2*2*(u2[nz-1]-u2[nz])/dzs+
      r2*km1*(u1[nz]-u2[nz]);if((iz>1)&&(iz<nz)){
    u2t[iz]=
      D2*(u2[iz+1]-2*u2[iz]+u2[iz-1])/dzs+
      r2*km1*(u1[iz]-u2[iz]);}
}
```
This code requires some additional explanation.

− The derivative  $\frac{\partial^2 u_2}{\partial z^2}$  in eq. (3.2-1) is approximated with a threepoint centered finite difference (FD).

$$
\frac{\partial^2 u_2(z,t)}{\partial z^2} \approx \frac{u_2(z + \Delta z, t) - 2u_2(z,t) + u_2(z - \Delta z, t)}{\Delta z^2} + O(\Delta z^2)
$$
\n(4.1-1)

 $O(\Delta z^2)$  indicates that the error in the FD approximation is second order in  $\Delta z^1$ .

− BC (3.2-3) is approximated with a two-point centered FD.

$$
\frac{\partial u_2(z=z_l,t)}{\partial z} \approx \frac{u_2(z_l+\Delta z,t)-u_2(z_l-\Delta z,t)}{2\Delta z} = 0
$$

<sup>&</sup>lt;sup>1</sup>Higher-order FD approximations,  $O(\Delta z^p)$ ,  $p = 4, 6, 8, 10$ , are considered in [1]. As a point of terminology, an error analysis of a numerical solution based on the variation of the FD interval, ∆*z* = *h* is termed *h refinement*. Variation of the order of the FD approximation, *O*(*h p* ), is termed *p refinement*.

or

$$
u_2(z_l - \Delta z, t) = u_2(z_l + \Delta z, t)
$$
 (4.1-2)

− Combination of eqs. (4.1-1,2) gives the FD approximation

$$
\frac{\partial^2 u_2(z = z_l, t)}{\partial z^2} \approx \frac{u_2(z_l + \Delta z, t) - 2u_2(z_l, t) + u_2(z_l - \Delta z, t)}{\Delta z^2}
$$

$$
= 2 \frac{u_2(z_l + \Delta z, t) - u_2(z_l, t)}{\Delta z^2} \tag{4.1-3}
$$

which is programmed as

$$
2*(u2[2]-u2[1])/dzs
$$

in if(iz==1){  $u2t[1] =$ 2\*D2\*(u2[2]-u2[1])/dzs+ r2\*km1\*(u1[1]-u2[1]);}

− Similarly, BC (3.2-4) is approximated with a two point centered FD.

$$
\frac{\partial u_2(z=z_u,t)}{\partial z} \approx \frac{u_2(z_u+\Delta z,t)-u_2(z_u-\Delta z,t)}{2\Delta z} = 0
$$

or

$$
u_2(z_u + \Delta z, t) = u_2(z_u - \Delta z, t)
$$
 (4.1-3)

− Combination of eqs. (4.1-1,3) gives the FD approximation

$$
\frac{\partial^2 u_2(z = z_u, t)}{\partial z^2} \approx \frac{u_2(z_u + \Delta z, t) - 2u_2(z_u, t) + u_2(z_u - \Delta z, t)}{\Delta z^2}
$$

$$
= 2 \frac{u_2(z_u - \Delta z, t) - u_2(z_u, t)}{\Delta z^2} \tag{4.1-4}
$$

which is programmed as

$$
2*(u2[nz-1]-u2[nz])/dzs
$$

in

if(iz==nz){ u2t[nz]= D2\*2\*(u2[nz-1]-u2[nz])/dzs+ r2\*km1\*(u1[nz]-u2[nz]);}

− For the interior points *z<sup>l</sup>* < *z* < *zu*, the RHS of eq. (4.1-1) is programmed as

(u2[iz+1]-2\*u2[iz]+u2[iz-1])/dzs

in

```
if((iz>1)&&(iz<nz)){
 u2t[iz]=
   D2*(u2[iz+1]-2*u2[iz]+u2[iz-1])/dzs+
    r2*km1*(u1[iz]-u2[iz]);}
```
In general, the correspondence of the programming with eqs. (3.1-1), (3.2- 1) is an important feature of the MOL.

• The 42 ODE derivatives are placed in the vector ut for return to 1 sodes to take the next in *t* along the solution.

```
#
# Two vectors to one vector
 ut=rep(0,2*nz);for(iz in 1:nz){
   ut[iz] = ut[iz];ut[iz+nz]=u2t[iz];}
```
• The counter for the calls to pde2a is incremented and returned to the main program of Listing 4.1 by <<-.

```
#
# Increment calls to pde2a
 ncall <<- ncall+1;
```
• The vector ut is returned as a list as required by lsodes. c is the R vector utility. The final } concludes pde2a.

```
#
# Return derivative vector
  return(list(c(ut)));
  }
```
This completes the discussion of pde2a. The output from the main program of Listing 4.1 and ODE/MOL routine pde2a of Listing 4.2 is considered next.

## **Numerical, graphical output**

The numerical output is given in Table 4.1.

```
[1] 21
```
[1] 43



0.00	0.60	1.000e+00	1.000e+00
0.00	0.70	1.000e+00	1.000e+00
0.00	0.80	1.000e+00	1.000e+00
0.00	0.90	1.000e+00	1.000e+00
0.00	1.00	1.000e+00	1.000e+00
t	z	u1(z,t)	u2(z,t)
0.20	0.00	7.500e-01	$9.087e - 01$
0.20	0.10	8.927e-01	$9.357e - 01$
0.20	0.20	$9.556e-01$	$9.682e-01$
0.20	0.30	9.849e-01	$9.880e - 01$
0.20	0.40	$9.960e - 01$	$9.964e-01$
0.20	0.50	$9.991e-01$	$9.991e-01$
0.20	0.60	9.999e-01	9.998e-01
0.20	0.70	1.000e+00	1.000e+00
0.20	0.80	1.000e+00	1.000e+00
0.20	0.90	1.000e+00	1.000e+00
0.20	1.00	1.000e+00	1.000e+00
Output for $t = 0.4, 0.6$ ,			
	0.8 removed		
t	z	u1(z,t)	u2(z,t)
1.00	0.00	7.500e-01	8.212e-01
1.00	0.10	8.140e-01	8.367e-01
1.00	0.20	8.494e-01	8.624e-01
1.00	0.30	8.792e-01	8.895e-01
1.00	0.40	$9.063e-01$	$9.149e - 01$
1.00	0.50	$9.303e-01$	$9.373e - 01$
1.00	0.60	$9.504e-01$	$9.558e-01$
1.00	0.70	$9.663e-01$	9.701e-01
1.00	0.80	9.779e-01	$9.802e - 01$
1.00	0.90	$9.855e-01$	$9.864e-01$
1.00	1.00	$9.892e-01$	$9.886e - 01$
$ncall =$	131		

Table 4.1: Numerical output from Listings 4.1, 4.2



**Figure 4.1-1**  $u_1(z,t)$  from eqs. (3.1), 2D

We can note the following details about this output.

- 21 *t* output points as the first dimension of the solution matrix out from lsodes as programmed in the main program of Listing 4.1 (with nout=21).
- The solution matrix out returned by lsodes has 43 elements as a second dimension. The first element is the value of *t*. Elements 2 to 43 are  $u_1(z,t)$ ,  $u_2(z,t)$  from eqs. (3.1), (3.2) (for each of the 21 output points).



**Figure 4.1-2**  $u_1(z,t)$  from eqs. (3.1), 3D

- The solution is displayed for  $t=0,1/20=0.05,...,1$  as programmed in Listing 4.1 (every fourth value of *t* is displayed as explained previously).
- The solution is displayed for  $z=0,1/20=0.05,...,1$  as programmed in Listing 4.1 (every second value of *z* is displayed as explained previously).
- ICs  $(3.1-2)$ ,  $(3.2-2)$  are confirmed  $(t = 0)$ .
- BC (3.1-3) is confirmed ( $t = 0$ ,  $z = z_l = 0$ ). There is a discontinuous change from the IC  $(t = 0)$  to the BC  $(t > 0)$ , which is subsequently smoothed, e.g.,  $t = 0.2$ . To improve the appearance of the graphical output (Figure 4.1-1 considered next), the ouput does not include the solution at  $z = z_l = 0$  $(\text{matplot}(x=z[2:nz], y=u1[2:nz], \ldots \text{ in Listing 4.1}).$  Use of Listings 4.1, 4.2 with the solution at  $z = z_l = 0$  included is left as an exercise.
- The computational effort as indicated by  $ncall = 131$  is modest so that lsodes computed the solution to eqs. (3.1), (3.2) efficiently.



**Figure 4.2-1**  $u_2(z,t)$  from eqs. (3.2), 2D

The graphical output is shown in Figures 4.1, 4.2.

The solution  $u_1(z,t)$  starts from IC (3.1-2) and confirms BC (3.1-3). In general,  $u_1(z,t)$  is a front moving left to right (as expected with  $v_z > 0$ ) in response to the reduced entering blood  $O_2$  concentration,  $u_1(z = z_l = 0, t) = u_{1e} = 0.75$ .

Figure 4.1-2 reflects the decreasing blood  $O_2$  concentration with *t*.



**Figure 4.2-2**  $u_2(z,t)$  from eqs. (3.1), 3D

The solution  $u_2(z,t)$  starts from IC (3.2-2). In general,  $u_2(z,t)$  is a front moving left to right in response to the reduced entering blood  $O_2$  concentration,  $u_1(z = z_l)$  $0,t$  =  $u_{1e}$  = 0.75.

Figure 4.2-2 reflects the decreasing brain tissue  $O_2$  concentration with *t*. Two special cases can be considered to confirm the model and coding:

- $v_z = 0$ : With no blood flood,  $u_1(z,t)$ ,  $u_2(z,t)$  depart from ICs (3.1-2), (3.2-2) as a result of the diffusion in *z* of eq. (3.2-1).
- $k_{m1} = 0$ : With no  $O_2$  transfer through the BBB,  $u_1(z,t)$  is a front moving left to right ( $v_z > 0$ ) with the long time solution  $u_1(z, t \to \infty) = u_{1e}$  ( $t_f = 2$ ) indicates the solution for large *t*).  $u_2(z,t)$  remains at the IC (3.2-2) since there is no transfer of  $O_2$  between the blood and the brain tissue.

These cases are left as exercises.

#### **4.1.2 SUMMARY AND CONCLUSIONS**

The two PDE model for blood and brain tissue  $O_2$  concentrations,  $u_1(z,t)$ ,  $u_2(z,t)$ defined by eqs. (3.1), (3.2) is implemented within the MOL. Parameters in this model are defined numerically in Listing 4.1 and can be used to investigate dynamic effects, e.g., the blood convection with  $v_z$ , mass transfer through the BBB with  $k_{m1}$ .

As the next step in model development, a third PDE is added in Chapter 5 for the brain neuron cell density as it is affected by the brain tissue  $O_2$  concentration, which could account for Covid cognitive impairment.

#### **REFERENCES**

- 1. Schiesser, W.E. (2016), *Method of Lines PDE Analysis in Biomedical Science and Engineering*, John Wiley, Hoboken, NJ.
- 2. Schiesser, W.E. (2019), *Numerical PDE Analysis of the Blood Brain Barrier*, World Scientific Publishing Co., Singapore.
- 3. Soetaert, K., J. Cash, and F. Mazzia (2012), *Solving Differential Equations in R*, Springer-Verlag, Heidelberg, Germany.

# 5 Three PDE Model

### **5.1 INTRODUCTION**

The two PDE model of Chapter 3, eqs. (3.1), (3.2), is extended in this chapter by adding a PDE for the neuron cell density.

#### **5.1.1 THREE PDE MODEL FORMULATION**

The neuron cell density,  $u_3(z,t)$ , is modeled as

$$
\frac{\partial u_3}{\partial t} = -k_{r3}(u_{2n} - u_2) \tag{5.1-1}
$$

Equation (5.1-1) states that the functional neuron cell density decreases,  $\frac{\partial u_3}{\partial t} < 0$ , when the brain tissue  $O_2$  concentration drops below the normal level,  $-k_{r3}(u_{2n}$  $u_2$ )  $<$  0.  $k_{r3}$  is a rate constant relating the decrease in neuron cell density to the deficiency in the brain tissue  $O_2$  concentration and is a key parameter in the three PDE model.

Equation (5.1-1) is first order in *t* and requires one IC.

$$
u_3(z, t = 0) = u_{3n} \tag{5.1-2}
$$

Equation (5.1-1) is a PDE (rather than an ODE) since  $u_3(z,t)$  is a function of z, t (and not just *t*), even though it does not explicitly have derivatives in *z*.

Equations  $(5.1)$  are added to eqs.  $(3.1)$ ,  $(3.2)$  to constitute the three PDE model for  $u_1(z,t)$ ,  $u_2(z,t)$ ,  $u_3(z,t)$ . The implementation of this model in R routines is considered next.

#### **5.1.2 THREE PDE MODEL IMPLEMENTATION**

A main program for eqs.  $(3.1)$ ,  $(3.2)$ ,  $(5.1)$  follows.

#### **Main program**

```
#
# Three PDE model
#
# Delete previous workspaces
  rm(list=ls(all=TRUE))
#
# Access ODE integrator
  library("deSolve");
#
```

```
# Access functions for numerical solution
  setwd("f:/brain hypoxia/chap5");
 source("pde3a.R");
#
# Parameters
 nz=21;
 r1=1;ru=2;
 D2=0.1;
 km1=0;km1=10;
 vz=1;
 u1e=0.75;
 kr3=1;
 u1n=1;
 u2n=1;
 u3n=1;
#
# Constants
 r1=2/rl;
 r2=(2*r1)/(ru^2-r1^2);#
# Spatial grid in z
 zl=0;zu=1;dz=(zu-zl)/(nz-1);dzs=dz^2;
 z=seq(from=zl,to=zu,by=dz);
#
# Independent variable for ODE integration
 t0=0; tf=1; nout=21;tout=seq(from=t0,to=tf,by=(tf-t0)/(nout-1));
#
# Initial condition (t=0)
 u0=rep(0,3*nz);
 for(iz in 1:nz){
   u0[iz] =u1n;
   u0[iz+nz] =u2n;
   u0[iz+2*nz]=u3n;
 }
 ncall=0;
#
# ODE integration
 out=lsodes(y=u0,times=tout,func=pde3a,
      sparsetype="sparseint",rtol=1e-6,
      atol=1e-6,maxord=5);
 nrow(out)
```

```
ncol(out)
#
# Arrays for plotting numerical solution
  u1=matrix(0,nrow=nz,ncol=nout);
  u2=matrix(0,nrow=nz,ncol=nout);
  u3=matrix(0,nrow=nz,ncol=nout);
  for(it in 1:nout){
    for(iz in 1:nz){
      u1[iz, it] = out[it, iz+1];u2[iz, it] = out[it, iz+1+nz];u3[iz, it] = out[it, iz+1+2*nz];}
   u1[1, it] = u1e;}
#
# Display numerical solution
  iv=seq(from=1,to=nout,by=4);
  for(it in iv){
    cat(sprint(f')n t z u1(z,t) u2(z,t)u3(z,t)\n\langle n''\rangle);iv=seq(from=1,to=nz,by=2);
    for(iz in iv){
      cat(sprintf("%6.2f %6.2f %12.3e %12.3e %12.3e \n",
          tout[it],z[iz],u1[iz,it],u2[iz,it],u3[iz,it]));
    }
  }
#
# Calls to ODE routine
  cat(sprintf("\n\n ncall = \delta5d\n\n",ncall));
#
# Plot PDE solutions
#
# u1
  par(mfrow=c(1,1));
  matplot(x=z[2:nz],y=u1[2:nz,],type="l",xlab="z",ylab="u1(z,t)",
          xlim=c(zl,zu),lty=1,main="",lwd=2,col="black");
  persp(z,tout,u1,theta=60,phi=45,
        xlim=c(z1,zu), ylim=c(t0,tf), zlim=c(0,1.1),
        xlab="z", ylab="t", zlab="u1(z,t)");
#
# u2
  par(mfrow=c(1,1));matplot(x=z,y=u2,type="l",xlab="z",ylab="u2(z,t)",
          xlim=c(zl,zu),lty=1,main="",lwd=2,col="black");
```

```
persp(z,tout,u2,theta=60,phi=45,
        xlim=c(z1,zu), ylim=c(t0,tf), zlim=c(0,1.1),
        xlab="z", ylabel="t",zlab="u2(z,t)");#
# u3
  par(mfrow=c(1,1));matplot(x=z,y=u3,type="1",xlab="z",ylab="u3(z,t)",xlim=c(zl,zu),lty=1,main="",lwd=2,col="black");
  persp(z,tout,u3,theta=60,phi=45,
        xlim=c(z1,zu), ylim=c(t0,tf), zlim=c(0,1.1),
        xlab="z", ylabel="t",zlab="u3(z,t)");
```

```
Listing 5.1: Main program for eqs. (3.1), (3.2), (5.1)
```
We can note the following details about Listing 5.1 (with some repetition of the discussion of Listings 2.1, 4.1 so that the explanation is self-contained).

• Previous workspaces are deleted.

```
#
# Three PDE model
#
# Delete previous workspaces
 rm(list=ls(all=TRUE))
```
• The R ODE integrator library deSolve is accessed [1].

```
#
# Access ODE integrator
 library("deSolve");
#
# Access functions for numerical solution
  setwd("f:/brain hypoxia/chap5");
  source("pde3a.R");
```
Then the directory with the files for the solution of eqs.  $(3.1)$ ,  $(3.2)$ ,  $(5.1)$  is designated. Note that setwd (set working directory) uses / rather than the usual  $\backslash$ .

• The model parameters are specified numerically.

```
#
# Parameters
 nz=21;
 r = 1;
  ru=2;
  D2=0.1;
```

```
km1=0;km1=10;
vz=1;
u1e=0.75;
kr3=1;
u1n=1;
u2n=1;
u3n=1;
```
where the additional parameters for eqs.  $(5.1)$  are

- − kr3=1;: *kr*<sup>3</sup> in eq. (5.1-1) for the rate of change of the functional neuron cell density,  $u_3(z,t)$ , from hypoxia,  $-k_{r3}(u_{2n}-u_2)$ .
- − u3n: normalized neuron cell density in IC (5.1-2).
- The constants  $r_1 = \frac{2}{r_l}$ ,  $r_2 = \frac{2r_l}{(r_u^2 r_l^2)}$  are computed for use in the ordinary differential equation/method of lines (ODE/MOL) routine pde3a.

```
#
# Constants
  r1=2/rl;
  r2=(2*r1)/(ru^2-rl^2);
```
• A spatial grid for eqs.  $(3.1-1)$ ,  $(3.2-1)$ ,  $(5.1-1)$  is defined with 21 points so that  $z = 0, 1/20=0.05, \ldots, 1$ . The BBB length is a normalized value,  $z=z_u=1$ .

```
#
# Spatial grid in z
  z1=0; zu=1; dz=(zu-z1)/(nz-1); dzs=dz^2;z=seq(from=zl,to=zu,by=dz);
```
• An interval in *t* is defined for 21 output points so that tout=0, 1/20=0.05,  $\ldots$ , 1. The time scale is normalized with  $t_f = 1$  specified as the final time that is considered appropriate, e.g., week, month, year.

```
#
# Independent variable for ODE integration
  t0=0;tf=1;nout=21;
  tout=seq(from=t0,to=tf,by=(tf-t0)/(nout-1));
```
• ICs  $(3.1-2)$ ,  $(3.2-2)$ ,  $(5.1-2)$  are implemented  $(u1n, u2n, u3n)$  are defined previously as parameters).

```
#
# Initial condition (t=0)
  u0=rep(0,3*nz);
```

```
for(iz in 1:nz){
  u0[iz] =u1n;
  u0[iz+nz] = u2n;u0[iz+2*nz]=u3n;
}
ncall=0;
```
Also, the counter for the calls to pde3a is initialized.

• The system of 3\*nz=63 ODEs is integrated by the library integrator lsodes (available in deSolve, [1]). As expected, the inputs to lsodes are the ODE function, pde3a, the IC vector u0, and the vector of output values of *t*, tout. The length of u0 (63) informs lsodes how many ODEs are to be integrated. func,y,times are reserved names.

```
#
# ODE integration
  out=lsodes(y=u0,times=tout,func=pde3a,
      sparsetype="sparseint",rtol=1e-6,
      atol=1e-6,maxord=5);
  nrow(out)
  ncol(out)
```
nrow,ncol confirm the dimensions of out.

•  $u_1(z,t)$ ,  $u_2(z,t)$ ,  $u_3(z,t)$  are placed in matrices for subsequent plotting.

```
#
# Arrays for plotting numerical solution
  u1=matrix(0,nrow=nz,ncol=nout);
  u2=matrix(0,nrow=nz,ncol=nout);
  u3=matrix(0,nrow=nz,ncol=nout);
  for(it in 1:nout){
    for(iz in 1:nz){
      u1[iz, it] = out[it, iz+1];u2[iz,it]=out[it,iz+1+nz];
      u3[iz, it] = out[it, iz+1+2*nz];}
   u1[1, it] = u1e;}
```
The offset +1 is required because the first element of the solution vectors in out is the value of *t* and the 2 to 64 elements are the 63 values of  $u_1, u_2, u_3$ . These dimensions from the preceding calls to nrow,ncol are confirmed in the subsequent output.

• The numerical values of  $u_1(z,t)$ ,  $u_2(z,t)$ ,  $u_3(z,t)$  returned by 1 sodes are displayed. Every fourth value in *t* and every second value in *z* appear from by=4,2.

```
#
# Display numerical solution
 iv=seq(from=1,to=nout,by=4);
  for(it in iv){
    cat(sprintf("n t z u1(z,t) u2(z,t))u3(z,t)\n\langle n''\rangle;
    iv=seq(from=1,to=nz,by=2);
    for(iz in iv){
      cat(sprintf("%6.2f %6.2f %12.3e %12.3e %12.3e \n",
          tout[it],z[iz],u1[iz,it],u2[iz,it],u3[iz,it]));
    }
  }
```
• The number of calls to pde3a is displayed at the end of the solution.

```
#
# Calls to ODE routine
  cat(sprintf("\n\n ncall = \delta5d\n\n",ncall));
```
•  $u_1(z,t)$ ,  $u_2(z,t)$ ,  $u_3(z,t)$  are plotted in 2D against *z* and parametrically in *t* with the R utility matplot and in 3D with R utility persp. par(mfrow=c(1,1)) specifies a  $1 \times 1$  matrix of plots, that is, one plot on a page.

```
#
# Plot PDE solutions
#
# u1
 par(mfrow=c(1,1));matplot(x=z[2:nz],y=u1[2:nz,],type="l",xlab="z",
          ylab="u1(z,t)",xlim=c(zl,zu),lty=1,main="",lwd=2,
          col="black");
  persp(z,tout,u1,theta=60,phi=45,
        xlim=c(z1,zu), ylim=c(t0,tf), zlim=c(0,1.1),
        xlab="z", ylab="t", zlab="u1(z,t)");
#
# u2
 par(mfrow=c(1,1));matplot(x=z,y=u2,type="l",xlab="z",ylab="u2(z,t)",
          xlim=c(zl,zu),lty=1,main="",lwd=2,col="black");
 persp(z,tout,u2,theta=60,phi=45,
        xlim=c(z1,zu), ylim=c(t0,tf), zlim=c(0,1.1),
        xlab="z", ylab="t", zlab="u2(z,t)");
#
# u3
 par(mfrow=c(1,1));
```

```
matplot(x=z,y=u3,type="l",xlab="z",ylab="u3(z,t)",
        xlim=c(zl,zu),lty=1,main="",lwd=2,col="black");
persp(z,tout,u3,theta=60,phi=45,
      xlim=c(z1,zu), ylim=c(t0,tf), zlim=c(0,1.1),
      xlab="z", ylabel="t",zlab="u3(z,t)");
```
The 2D plot of  $u_1(z,t)$  does not include the discontinuous change from IC  $(3.1-2)$  to BC  $(3.1-3)$ ,  $x=z$  [2:nz],  $y=u1$  [2:nz,]. This discontinuity is not included in  $u_2(z,t)$ ,  $u_3(z,t)$ , so the solution at  $z = z_l$  is included,  $x = z$ ,  $y = u^2$ , x=z,y=u3.

This completes the discussion of the main program for eqs. (3.1), (3.2), (5.1). The ODE/MOL routine pde3a called by lsodes from the main program for the numerical MOL integration of eqs. (3.1), (3.2), (5.1) is discussed in the following section.

#### **ODE/MOL routine**

pde3a called in the main program of Listing 5.1 follows:

```
pde3a=function(t,u,parm){
#
# Function pde3a computes the t derivatives
# of u1(z,t), u2(z,t), u3(z,t)#
# One vector to three vectors
 u1=rep(0,nz);u2=rep(0,nz);u3=rep(0,nz);for(iz in 1:nz){
    u1[iz]=u[iz];u2[iz]=u[iz+nz];u3[iz]=u[iz+2*nz];
 }
#
# BC, z=zl
 u1[1]=u1e;
#
# PDEs
 ut=rep(0,nz);for(iz in 1:nz){
    if(iz==1){u1t[1]=0;}
    if(iz>1)u1t[iz]=-vz*(u1[iz]-u1[iz-1])/dz-
        r1*km1*(u1[iz]-u2[iz]);}
  u2t=rep(0,nz);
```

```
for(iz in 1:nz){
    if(iz==1){
      u2t[1]=2*D2*(u2[2]-u2[1])/dzs+
        r2*km1*(u1[1]-u2[1]);if(iz=nz)u2t[nz]=
        D2*2*(u2[nz-1]-u2[nz])/dzs+
        r2*km1*(u1[nz]-u2[nz]);if((iz>1)&&(iz<nz)){
      u2t[iz]=
        D2*(u2[iz+1]-2*u2[iz]+u2[iz-1])/dzs+
        r2*km1*(u1[iz]-u2[iz]);}
  }
 u3t=rep(0,nz);for(iz in 1:nz){
    u3t[iz]=-kr3*(u2n-u2[iz]);
 }
#
# Three vectors to one vector
 ut=rep(0,3*nz);for(iz in 1:nz){
    ut[iz] =u1t[iz];
   ut[iz+nz] = u2t[iz];ut[iz+2*nz] = u3t[iz];}
#
# Increment calls to pde3a
 ncall <<- ncall+1;
#
# Return derivative vector
 return(list(c(ut)));
 }
          Listing 5.2: ODE/MOL routine for eqs. (3.1), (3.2), (5.1)
```
We can note the following details about Listing 5.2.

The function is defined.

```
pde3a=function(t,u,parm){
#
# Function pde3a computes the t derivatives
# of u1(z,t), u2(z,t), u3(z,t)
```
t is the current value of  $t$  in eqs.  $(3.1)$ ,  $(3.2)$ ,  $(5.1)$ . u is the 63-vector of ODE/PDE dependent variables. parm is an argument to pass parameters to pde3a (unused, but required in the argument list). The arguments must be listed in the order stated to properly interface with lsodes called in the main program of Listing 5.1. The derivative vector of the LHS of eqs. (3.1-1), (3.2-1), (5.1-1) is calculated and returned to lsodes, as explained subsequently.

• u is placed in three vectors to facilitate the programming of eqs.  $(3.1)$ ,  $(3.2)$ ,  $(5.1).$ 

```
#
# One vector to three vectors
  u1=rep(0,nz);u2=rep(0,nz);u3=rep(0,nz);for(iz in 1:nz){
    u1[iz]=u[iz];u2[iz]=u[iz+nz];u3[iz]=u[iz+2*nz];
  }
```
• BC  $(3.1-3)$  is programmed.

```
#
# BC, z=zl
  u1[1]=u1e;
```
• Equation  $(3.1-1)$  is programmed.

```
#
# PDEs
 ut=rep(0,nz);for(iz in 1:nz){
    if(iz==1){u1t[1]=0;}
    if(iz>1)u1t[iz] = -vz*(u1[iz]-u1[iz-1])/dz -r1*km1*(u1[iz]-u2[iz]);}
```
This code has additional explanation in the discussion of Listing 4.2. For  $z = z_l$ , BC (3.1-3) sets the value of  $u_1(z = z_l, t)$  and therefore the derivative is set to zero (if(iz==1)u1t[1]=0;) to ensure the boundary value is maintained.

• Equation  $(3.2-1)$  is programmed.

```
u2t=rep(0,nz);for(iz in 1:nz){
  if(iz==1){
    u2t[1]=
```
}

```
2*D2*(u2[2]-u2[1])/dzs+
   r2*km1*(u1[1]-u2[1]);}
if(iz==nz){
 u2t[nz]=D2*2*(u2[nz-1]-u2[nz])/dzs+
   r2*km1*(u1[nz]-u2[nz]);if((iz>1)&&(iz<nz)){
 u2t[iz]=
   D2*(u2[iz+1]-2*u2[iz]+u2[iz-1])/dzs+
   r2*km1*(u1[iz]-u2[iz]);}
```
This code has additional explanation in the discussion of Listing 4.2.

• Equation  $(5.1-1)$  is programmed.

```
u3t=rep(0,nz);for(iz in 1:nz){
 u3t[iz]=-kr3*(u2n-u2[iz]);
}
```
In general, the correspondence of the programming with eqs. (3.1-1), (3.2-1), (5.1-1) is an important feature of the MOL.

• The 63 ODE derivatives are placed in the vector ut for return to 1 sodes to take the next in *t* along the solution.

```
#
# Three vectors to one vector
 ut=rep(0,3*nz);for(iz in 1:nz){
   ut[iz] =u1t[iz];
   ut[iz+nz] = u2t[iz];ut[iz+2*nz] = u3t[iz];}
```
• The counter for the calls to pde3a is incremented and returned to the main program of Listing 5.1 by <<-.

```
#
# Increment calls to pde3a
  ncall <<- ncall+1;
```
• The vector ut is returned as a list as required by lsodes. c is the R vector utility. The final  $\}$  concludes pde3a.

```
#
# Return derivative vector
 return(list(c(ut)));
 }
```
This completes the discussion of pde3a. The output from the main program of Listing 5.1 and ODE/MOL routine pde3a of Listing 5.2 is considered next.

#### **Numerical, graphical output**

The numerical output is in Table 5.1.

[1] 21

[1] 64



Output for  $t = 0.4$ , 0.6, 0.8 removed



 $ncall = 150$ 

Table 5.1: Numerical output from Listings 5.1, 5.2

We can note the following details about this output.

- 21 *t* output points as the first dimension of the solution matrix out from lsodes as programmed in the main program of Listing 5.1 (with nout=21).
- The solution matrix out returned by 1 sodes has 64 elements as a second dimension. The first element is the value of *t*. Elements 2 to 64 are  $u_1(z,t)$ ,  $u_2(z,t)$ ,  $u_3(z,t)$  from eqs. (3.1), (3.2), (5.1) (for each of the 21 output points).
- The solution is displayed for  $t=0,1/20=0.05,...,1$  as programmed in Listing 5.1 (every fourth value of *t* is displayed as explained previously).
- The solution is displayed for  $z=0,1/20=0.05,...,1$  as programmed in Listing 5.1 (every second value of *z* is displayed as explained previously).
- ICs  $(3.1-2)$ ,  $(3.2-2)$ ,  $(5.1-2)$  are confirmed  $(t = 0)$ .
- BC (3.1-3) is confirmed ( $t = 0$ ,  $z = z_l = 0$ ). There is a discontinuous change from the IC  $(t = 0)$  to the BC  $(t > 0)$  which is subsequently smoothed, e.g.,  $t = 0.2$ . To improve the appearance of the graphical output (Figure 5.1-1) considered next), the output does not include the solution at  $z = z_l = 0$  $(\text{matplot}(x=z[2:nz], y=u1[2:nz], \ldots \text{ in Listing 5.1}).$  Use of Listings 5.1, 5.2 with the solution at  $z = z_l = 0$  included is left as an exercise.
- The computational effort as indicated by ncall = 150 is modest so that lsodes computed the solution to eqs. (3.1), (3.2), (5.1) efficiently.

The graphical output for  $u_1(z,t)$  is the same as in Figures 4.1, and the output for  $u_2(z,t)$  is the same as in Figures 4.2 and is not repeated here.



**Figure 5.3-1**  $u_3(z,t)$  from eqs. (5.1), 2D

The solution  $u_3(z,t)$  starts from IC (5.1-2). In general,  $u_3(z,t)$  is a front moving left to right (as expected with  $v_z > 0$ ) in response to the reduced entering blood  $O_2$ concentration,  $u_1(z = z_l = 0,t) = u_{1e} = 0.75$ . The reduced functional neuron cell density from hypoxia might explain the cognitive impairment of long Covid.

Figure 5.3-2 reflects the reduced neuron cell density,  $u_3(z,t)$ .



**Figure 5.3-2**  $u_3(z,t)$  from eqs. (5.1), 3D

#### **5.1.3 SUMMARY AND CONCLUSIONS**

Equations (3.1), (3.2), (5.1) are the three PDE model for  $O_2$  in the capillary blood flow, *O*<sup>2</sup> in the brain tissue, and neuron cell density in the brain tissue. The effect of brain  $O_2$  deficiency (hypoxia) can be studied through the rate constant  $k_{r3}$ , which has implications for various neurological effects such as cognitive impairment.

Variation in  $k_{r3}$  that might explain recovery from long Covid, and the RHS terms of eqs. (3.1), (3.2), (5.1) are considered in Chapter 6.

#### **REFERENCE**

1. Soetaert, K., J. Cash, and F. Mazzia (2012), *Solving Differential Equations in R*, Springer-Verlag, Heidelberg, Germany.



# 6 Case Studies

# **6.1 INTRODUCTION**

The three PDE model of eqs.  $(3.1)$ ,  $(3.2)$ ,  $(5.1)$  is applied to two case studies in this concluding chapter.

#### **6.1.1 TIME VARIATION OF THE BRAIN** *O*<sup>2</sup> **CONCENTRATION**

The effect of a time variation of the entering  $O_2$  capillary blood concentration,  $u_1(z)$  $z_l$ ,  $t$ ) =  $u_{1e}(t)$  in boundary condition (3.1-3) can be programmed in the ODE/MOL routine pde3a of Listing 5.2. This variation might, for example, be the result of a partial recovery of the respiratory/lung function with time, e.g., through the use of supplemental  $O_2$ .

#### **Main program**

.

The time variation of the entering blood capillary  $O_2$  concentration,  $u_{1e}(t)$ , is programmed as minor changes/additions to the main program of Listing 5.1 and the ODE/MOL routine of Listing 5.2. The changes/additions to the main program are considered next.

```
.
      .
#
# Access functions for numerical solution
  setwd("f:/hypoxia/chap6");
  source("pde3a.R");
#
# Set case
  ncase=1;
#
# Parameters
  nz=21;
  r = 1;
  ru=2;
  D2=0.1;
  km1=0;km1=10;
  vz=1:
```

```
u1e=0.75;
  kr3=1;
  u1n=1;
  u2n=1;
  u3n=1;
      .
      .
      .
  if(ncase==1){u1[1,it]=u1e;}
  if(ncase==2){u1[1,it]=u1n+(u1e-u1n)*sin(pi*tout[it]);}
  if(ncase==3){
    if(tout[i t] < = 0.5) {u1[1, it]} = u1n + (u1e-u1n) * sin(pi * tout[i t]);}if(tout[it]> 0.5){u1[1,it]=u1e;}
      .
      .
      .
#
# Plot PDE solutions
#
# u1
  par(mfrow=c(1,1));matplot(x=z[2:nz],y=u1[2:nz,],type="l",xlab="z",ylab="u1(z,t)",
          xlim=c(zl,zu),lty=1,main="",lwd=2,col="black");
  persp(z,tout,u1,theta=120,phi=25,
        xlim=c(zl,zu),ylim=c(t0,tf),
        xlab="z", ylabel="t",zlab="u1(z,t)");#
# u2
  par(mfrow=c(1,1));matplot(x=z,y=u2,type="l",xlab="z",ylab="u2(z,t)",
          xlim=c(zl,zu),lty=1,main="",lwd=2,col="black");
  persp(z,tout,u2,theta=120,phi=25,
        xlim=c(zl,zu),ylim=c(t0,tf),
        xlab="z", ylab="t", zlab="u2(z,t)");
#
# u3
  par(mfrow=c(1,1));matplot(x=z,y=u3,type="l",xlab="z",ylab="u3(z,t)",
          xlim=c(z1,zu), lty=1, main="1", lwd=2, col="black");
  persp(z,tout,u3,theta=120,phi=25,
        xlim=c(zl,zu),ylim=c(t0,tf),
        xlab="z",ylab="t",zlab="u3(z,t)");
#
# u1e(t)=u1(z=z_1,t)
```

```
par(mfrow=c(1,1));matplot(x=tout,y=u1[1,],type="l",xlab="t",ylab="u1e(t)",
        xlim=c(t0,tf),lty=1,main="",lwd=2,col="black");
```
Listing 6.1: Changes/additions to the main program for  $u_1(z = z_l, t) = u_{1e}(t)$ 

We can note the following details about Listing 6.1 (refer also to Listing 5.1).

• The ODE/MOL routine is again pde3a (considered next).

```
#
# Access functions for numerical solution
  setwd("f:/hypoxia/chap6");
  source("pde3a.R");
```
• A case index, ncase, is included, with ncase=1,2,3 as discussed subsequently.

```
#
# Set case
 ncase=1;
#
# Parameters
 nz=21;
 r = 1;
 ru=2;
 D2=0.1;km1=0;km1=10;
 vz=1;
 u1e=0.75;
 kr3=1;
  u1n=1;
  u2n=1;
  u3n=1;
```
The parameters have the same numerical values as given in Listing 5.1. • BC (3.1-3) is programmed for three values of ncase.

```
if(ncase==1){u1[1,it]=u1e;}
if(ncase==2){u1[1,it]=u1n+(u1e-u1n)*sin(pi*tout[it]);}
if(ncase==3){
  if(tout[it]<=0.5){u1[1,it]=u1n+(u1e-u1n)
                             *sin(pi*tout[it]);}
 if(tout[it]> 0.5){u1[1,it]=u1e;}
```
For ncase=1, the entering blood  $O_2$  concentration is the constant  $u_{1e} = u_1$ (the same as in Listing 5.1).

For ncase=2, the entering blood  $O_2$  concentration change is a half sine wave, as explained subsequently (after the pde3a changes, Listing 6.2). This could represent an initial impairment (injury, damage) of the respiratory/lung function, followed by recovery.

For ncase=3, the entering blood  $O_2$  concentration change is a half sine wave, followed by a permanent decrease, as explained subsequently (after the pde3a changes, Listing 6.2). This could represent an initial impairment (injury, damage) of the respiratory/lung function, without recovery.

• The arguments of persp were modified to enhance the appearance of the 3D plots. For example, for the 3D plotting of  $u_1(z,t)$ ,

```
Listing 5.1
  persp(z,tout,u1,theta=60,phi=45,
        xlim=c(z1,zu), ylim=c(t0,tf), zlim=c(0,1.1),
        xlab="z", ylabel="t",zlab="u1(z,t)");Listing 6.1
```

```
persp(z,tout,u1,theta=120,phi=25,
      xlim=c(zl,zu),ylim=c(t0,tf),
      xlab="z", ylab="t", zlab="u1(z,t)");
```
These changes have the effect of reversing the direction of the *z* axis in the 3D plots.

• The time variation in  $u_{1e}(t)$  is plotted against *t* at the end of the main program to confirm the variation for ncase=1,2,3.

```
#
# u1e(t)=u1(z=z_1,t)par(mfrow=c(1,1));matplot(x=tout,y=u1[1,],type="l",xlab="t",ylab="u1e(t)",
          xlim=c(t0,tf),lty=1,main="",lwd=2,col="black");
```
This concludes the discussion of the changes/additions to the main program of Listing 5.1 for  $u_{1e}(t) = u_1e$ . The ODE/MOL routine, pde3a, is considered next.

#### **ODE/MOL routine**

.

The additions to pde3a are for BC  $(3.1-3)$  with ncase=1, 2, 3.

```
.
       .
#
# BC, z=zl
```

```
if(ncase==1){u1[1]=u1e;}
if(ncase==2){u1[1]=u1n+(u1e-u1n)*sin(pi*t);}
if(ncase==3){
  if(t<=0.5){u1[1]=u1n+(u1e-u1n)*sin(pi*t);}
  if(t>0.5 ){u1[1]=u1e;}
}
    .
    .
    .
```
Listing 6.2: Additions to the ODE/MOL routine of Listing 5.2

We can note the following details about Listing 6.2 (refer also to Listing 5.2).

• For ncase=1, the entering blood  $O_2$  concentration is the constant  $u_{1e} = u_1$  e (the same as in Listing 5.2).

```
#
# BC, z=zl
  if(ncase==1){u1[1]=u1e;}
```
• For ncase=2, the entering blood  $O_2$  concentration  $u_{1e}(t)$  is a half sine wave that passes through the points (1)  $u_{1e}(t = t_0 = 0) = u_{1n} (u_{1n} \text{ is the IC (3.1-2)})$ .  $(2)$   $u_{1e}(t = (t_f - t_0)/2 = 0.5) = u_{1e}$ 

(3) 
$$
u_{1e}(t = t_f = 1) = u_{1n}
$$

```
if(ncase==2){u1[1]=u1n+(u1e-u1n)*sin(pi*t);}
```
This variation in  $u_{1e}(t) = u_1(z = z_l, t)$  could result, for example, from initial impairment of the respiratory/lung system, followed by recovery.

• For ncase=3, the entering blood  $O_2$  concentration  $u_{1e}(t)$  is a half sine wave that passes through the points (1)  $u_{1e}(t = t_0 = 0) = u_{1n} (u_{1n} \text{ is the IC (3.1-2))}.$ 

```
(2) u_{1e}(t = (t_f - t_0)/2 = 0.5) = u_{1e}(3) u_{1e}(t = t_f = 1) = u_{1e}
```

```
if(ncase==3){
  if(t<=0.5){u1[1]=u1n+(u1e-u1n)*sin(pi*t);}
 if(t>0.5 ){u1[1]=u1e;}
}
```
This variation in  $u_{1e}(t) = u_1(z = z_l, t)$  could result, for example, from initial impairment of the respiratory/lung system, without recovery.

The numerical and graphical output from the main program of Listings 5.1, 6.1, and the ODE/MOL routine, pde3a, of Listings 5.2, 6.2 follows.

#### **Numerical and graphical output**

For ncase=1 in Listing 6.1, the numerical output is the same as given in Table 5.1, so this solution is not repeated here. The graphical  $u_{1e}(t)$  (set as a parameter and plotted in Listing 6.1) is the constant 0.75 (invariant in *t*) and is not presented here.

For ncase=2 in Listing 6.1, the numerical output is given as follows:

[1] 21

[1] 64





```
nca11 = 124
```
Table 6.2: Numerical output from Listings 5.1, 5.2, 6.1, 6.2, ncase=2

We can note the following details about this output.

- 21 *t* output points as the first dimension of the solution matrix out from lsodes as programmed in the main program of Listing 5.1 (with nout=21).
- The solution matrix out returned by 1 sodes has 64 elements as a second dimension. The first element is the value of *t*. Elements 2 to 64 are  $u_1(z,t)$ ,  $u_2(z,t)$ ,  $u_3(z,t)$  from eqs. (3.1), (3.2), (5.1) (for each of the 21 output points).
- The solution is displayed for  $t=0,1/20=0.05,...,1$  as programmed in Listing 5.1 (every fourth value of *t* is displayed as explained previously).
- The solution is displayed for  $z=0,1/20=0.05,...,1$  as programmed in Listing 5.1 (every second value of *z* is displayed as explained previously).
- ICs  $(3.1-2)$ ,  $(3.2-2)$ ,  $(5.1-2)$  are confirmed  $(t = 0)$ .
- BC (3.1-3) is confirmed  $(u_1(z = z_l = 0,t) = u_{1e}(t))$  according to the half sine wave as programmed in Listings 6.1, 6.2 for ncase=2.
- The computational effort as indicated by ncall = 124 is modest so that lsodes computed the solution to eqs. (3.1), (3.2), (5.1) efficiently.

The graphical output is shown in Figures 6.1, 2, 3, 4.

Figure 6.1-1 indicates the transient of  $u_1(z,t)$  away from IC (3.1-2),  $u_1(z,t=0)$  =  $u_{1n} = 1$  in response to BC (3.1-3),  $u_1(z = z_l, t) = u_{1e}(t)$ .

Figure 6.1-2 confirms the response in *z*, *t* of Figure 6.1-1. The discontinuity at  $z = z_l = 0$  is not included in Figure 6.1-1, but is included in Figure 6.1-2, as discussed previously.

Figure 6.2-1 indicates the transient of  $u_2(z,t)$  away from IC (3.2-2), in response to the  $O_2$  transfer through the BBB. Figure 6.2-2 confirms the response in *z*, *t* of Figure 6.2-1.

Figure 6.3-1 indicates the continuing decrease in the neuron cell density according to eq. (5.1-1).

Figure 6.3-2 confirms the response in *z*, *t* of Figure 6.3-1.

Figure 6.4-1 confirms  $u_{1e}(t)$  programmed in Listings 6.1, 6.2 for ncase=2. In general, the numerical and graphical output indicates modest changes in



**Figure 6.1-1**  $u_1(z,t)$  from eqs. (3.1), 2D, ncase=2

 $u_1(z,t)$ ,  $u_2(z,t)$ ,  $u_3(z,t)$  resulting from the recovery of  $u_{1e}(t)$  with increasing *t* (Figure 6.4-1).

For ncase3,  $u_{1e}(t)$  does not recover with increasing *t* so that the changes in  $u_1(z,t)$ ,  $u_2(z,t)$ ,  $u_3(z,t)$  are larger than for ncase=2. This is confirmed by the following output (for ncase=3 in Listings 6.1, 6.2).

[1] 21

[1] 64





 $ncall = 153$ 

Table 6.3: Numerical output from Listings 5.1, 5.2, 6.1, 6.2, ncase=3


**Figure 6.1-2**  $u_1(z,t)$  from eqs. (3.1), 3D, ncase=2

We can note the following details about this output.

- The dimensions of array out from lsodes are the same as for ncase=2 (Table 6.2).
- ICs (3.1-2), (3.2-2), (5.1-2) are confirmed  $(t = 0)$ .
- BC (3.1-3) is confirmed  $(u_1(z = z_l = 0, t) = u_{1e}(t))$  according to the half sine wave as programmed in Listings 6.1, 6.2 for ncase=3 (e.g.,  $u_1(z)$  $0,t = 1$  = 0.75).
- The computational effort as indicated by ncall = 153 is modest so that lsodes computed the solution to eqs. (3.1), (3.2), (5.1) efficiently.

The graphical output is shown in Figures 6.5,6,7,8.

Figure 6.5-1 indicates the monotonic decrease of the capillary blood  $O_2$  concentration toward 0.75 with increasing *t*.

Figure 6.5-2 confirms the response in *z*, *t* of Figure 6.5-1.





**Figure 6.2-1**  $u_2(z,t)$  from eqs. (3.2), 2D, ncase=2

Figure 6.6-1 indicates the monotonic decrease of the brain tissue  $O_2$  concentration with increasing  $t$  in response to the  $O_2$  through the BBB. Figure 6.6-2 confirms the response in *z*, *t* of Figure 6.6-1.

Figure 6.7-1 indicates the continuing decrease in the neuron cell density according to eq. (5.1-1).

Figure 6.7-2 confirms the response in *z*, *t* of Figure 6.7-1.

Figure 6.8-1 confirms  $u_{1e}(t)$  programmed in Listings 6.1, 6.2 for ncase=3.

In general, the numerical and graphical output indicates lower  $O_2$  concentrations and neuron cell density for ncase=3 than for ncase=2. For example,



**Figure 6.2-2**  $u_2(z,t)$  from eqs. (3.1), 3D, ncase=2

Table 6.2, ncase=2 t z  $u1(z,t)$   $u2(z,t)$   $u3(z,t)$ 1.00 0.10 9.139e-01 9.036e-01 9.284e-01 Table 6.3, ncase=3 t z  $u1(z,t)$   $u2(z,t)$   $u3(z,t)$ 1.00 0.10 8.242e-01 8.500e-01 9.213e-01

The reduced  $O_2$  concentrations and neuron cell density could result in cognitive impairment originating from Covid-reduced respiratory/lung function.

A similar analysis can be carried out with a variable blood flow rate,  $v_z(t)$ , which could also result from a Covid-reduced respiratory/lung function. This is left as an exercise.



**Figure 6.3-1**  $u_3(z,t)$  from eqs. (5.1), 2D, ncase=2

Additionally, the effect of the discontinuity between IC (3.1-2),  $u_{\zeta} = z_l = 0, t =$  $(0) = u_{1n} = 1$ , and BC (3.1-3),  $u_{\overline{\zeta}} = z_l = 0, t > 0$ ) =  $u_{1e} = 0.75$ , can be observed by changing the plotting of  $u_1$  from

matplot(x=z[2:nz],y=u1[2:nz,],type="l",xlab="z",ylab="u1(z,t)", xlim=c(zl,zu),lty=1,main="",lwd=2,col="black");

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**Figure 6.3-2**  $u_3(z,t)$  from eqs. (5.1), 3D, ncase=2

to

$$
\begin{array}{c}\n\texttt{matplot}(x=z, y=u1, type="1", xlab="z", ylab="u1(z, t)", \\
\texttt{xlim=c(z1, zu), lty=1, main="", lwd=2, col="black");\n}\end{array}
$$

This is left as an exercise.

The complex solutions for  $u_1(z,t)$ ,  $u_2(z,t)$ ,  $u_3(z,t)$ , as reflected in Figures 6.1,...,8, are a result of the integration of the left hand side (LHS) *t* derivatives of eqs. (3.1-1), (3.2-1), (5.1-1). These derivatives can be computed from the solutions and displayed as explained in the next case.

## **6.1.2 LHS PDE TIME DERIVATIVES**

The LHS *t* derivatives are computed, then displayed, with R code added to the main programs of Listings 5.1, 6.1. The ODE/MOL routine is again pde3a in Listings 5.2, 6.2.



**Figure 6.4-1**  $u_{1e}(t)$  from eq. (3.1-1), ncase=2



**Figure 6.5-1**  $u_1(z,t)$  from eqs. (3.1), 2D, ncase=3



**Figure 6.5-2**  $u_1(z,t)$  from eqs. (3.1), 3D, ncase=3



**Figure 6.6-1**  $u_2(z,t)$  from eqs. (3.2), 2D, ncase=3



**Figure 6.6-2**  $u_2(z,t)$  from eqs. (3.2), 3D, ncase=3



**Figure 6.7-1**  $u_3(z,t)$  from eqs. (5.1), 2D, ncase=3



**Figure 6.7-2**  $u_3(z,t)$  from eqs. (5.1), 3D, ncase=3



**Figure 6.8-1**  $u_{1e}(t)$  from eq. (3.1-1), ncase=3

# **Main program**

```
The following code is added to the end of the main programs of Listings 5.1, 6.1 to
\frac{\partial u_1(z,t)}{\partial x}, \frac{\partial u_2(z,t)}{\partial y}, \frac{\partial u_3(z,t)}{\partial y}\frac{\partial u_2(x,t)}{\partial t}, \frac{\partial u_3(x,t)}{\partial t} from eqs. (3.1-1), (3.2-1), (5.1-1).
       .
       .
       .
  Main program from Listings 5.1, 6.1
       .
       .
       .
#
# Derivatives in t
  u1t=matrix(0,nrow=nz,ncol=nout);
  u2t=matrix(0,nrow=nz,ncol=nout);
  u3t=matrix(0,nrow=nz,ncol=nout);
#
# Derivative calculation
#
  for(it in 1:nout){
#
# u1t
  for(iz in 1:nz){
    if(iz==1){u1t[1,it]=0;}
    if(iz>1){
       u1t[iz,it]=-vz*(u1[iz,it]-u1[iz-1,it])/dz-
         r1*km1*(u1[iz, it]-u2[iz, it]);}
#
# u2t
  for(iz in 1:nz){
    if(iz==1){
       u2t[1,it]=2*D2*(u2[2,it]-u2[1,it])/dzs+
         r2*km1*(u1[1,it]-u2[1,it]);}
    if(iz=nz){
       u2t[nz, it] =D2*2*(u2[nz-1,it]-u2[nz,it])/dzs+
         r2*km1*(u1[nz,it]-u2[nz,it]);}
    if((iz>1)&&(iz<nz)){
       u2t[iz, it] =D2*(u2[iz+1,it]-2*u2[iz,it]+u2[iz-1,it])/dzs+
         r2*km1*(u1[iz,it]-u2[iz,it]);}
```

```
#
# u3t
  for(iz in 1:nz){
    u3t[iz,it]=-kr3*(u2n-u2[iz,it]);
  }
 }
#
# Derivative plotting
#
# u1t
 par(mfrow=c(1,1));matplot(x=z[2:nz],y=u1t[2:nz,],type="l",xlab="z",
          ylab="u1t(z,t)",xlim=c(zl,zu),lty=1,main="",lwd=2,
          col="black");
  persp(z,tout,u1t,theta=120,phi=25,
        xlim=c(zl,zu),ylim=c(t0,tf),
        xlab="z", ylab="t", zlab="u1t(z,t)");#
# u2t
 par(mfrow=c(1,1));
 matplot(x=z,y=u2t,type="1",xlab="z",ylab="u2t(z,t)",xlim=c(zl,zu),lty=1,main="",lwd=2,col="black");
  persp(z,tout,u2t,theta=120,phi=25,
        xlim=c(zl,zu),ylim=c(t0,tf),
        xlab="z", ylabel="t",zlab="u2t(z,t)");#
# u3t
 par(mfrow=c(1,1));matplot(x=z,y=u3t,type="l",xlab="z",ylab="u3t(z,t)",
          xlim=c(zl,zu),lty=1,main="",lwd=2,col="black");
 persp(z,tout,u3t,theta=120,phi=25,
        xlim=c(zl,zu),ylim=c(t0,tf),
        xlab="z", ylabel="t",zlab="u3t(z,t)");
```
Listing 6.3: Additions to the main programs of Listings 5.1, 6.1 to compute and plot the *t* derivatives

We can note the following details about Listing 6.3.

∂*u*1(*z*,*t*) ∂*u*2(*z*,*t*) ∂*u*3(*z*,*t*) • Matrices are defined for  $\frac{\partial u_1(x,t)}{\partial t}$ ,  $\frac{\partial u_2(x,t)}{\partial t}$ ,  $\frac{\partial u_3(x,t)}{\partial t}$ . # # Derivatives in t u1t=matrix(0,nrow=nz,ncol=nout); u2t=matrix(0,nrow=nz,ncol=nout); u3t=matrix(0,nrow=nz,ncol=nout);

nz,nout are defined numerically in Listing 5.1.

The coding for  $\frac{\partial u_1(z,t)}{\partial x}$ • The coding for  $\frac{\partial u_1(x, t)}{\partial t}$  of eq. (3.1-1) is taken from pde3a of Listing 5.2 with a subscript it for *t* added.

```
#
  # Derivative calculation
  #
     for(it in 1:nout){
  #
  # u1t
     for(iz in 1:nz){
       if(iz==1){u1t[1,it]=0;}
       if(iz>1){
          u1t[iz,it]=-vz*(u1[iz,it]-u1[iz-1,it])/dz-
            r1*km1*(u1[iz,it]-u2[iz,it]);}
   The coding for \frac{\partial u_2(z,t)}{\partial x}• The coding for \frac{\partial u_2(s,t)}{\partial t} of eq. (3.2-1) is taken from pde3a of Listing 5.2
  with a subscript it for t added.
  #
  # u2t
     for(iz in 1:nz){
       if(iz==1){
          u2t[1,it]=2*D2*(u2[2,it]-u2[1,it])/dzs+
            r2*km1*(u1[1,it]-u2[1,it]);
       if(iz==nz){
          u2t[nz, it] =D2*2*(u2[nz-1,it]-u2[nz,it])/dzs+
            r2*km1*(u1[nz,it]-u2[nz,it]);}
       if((iz>1)&&(iz<nz)){
          u2t[iz, it] =D2*(u2[iz+1,it]-2*u2[iz,it]+u2[iz-1,it])/dzs+
            r2*km1*(u1[iz,it]-u2[iz,it]);}
     }
```
∂*u*<sup>3</sup> • The coding for  $\frac{\partial u_3(x, t)}{\partial t}$  of eq. (5.1-1) is taken from pde3a of Listing 5.2 with a subscript it for *t* added. (*z*,*t*)

```
#
# u3t
  for(iz in 1:nz){
    u3t[iz,it]=-kr3*(u2n-u2[iz,it]);
  }
  }
```
The second } concludes the loop in it.

• The plotting of  $\frac{\partial u_1(z,t)}{\partial x}$ ,  $\frac{\partial u_2(z,t)}{\partial y}$ ,  $\frac{\partial u_3(z,t)}{\partial y}$  $\frac{\partial u_2(x,t)}{\partial t}$ ,  $\frac{\partial u_3(x,t)}{\partial t}$  as a function of *z*,*t* is with matplot (2D) and persp (3D).

```
#
# Derivative plotting
#
# u1t
 par(mfrow=c(1,1));matplot(x=z[2:nz],y=u1t[2:nz,],type="l",xlab="z",
          ylab="u1t(z,t)",xlim=c(zl,zu),lty=1,main="",lwd=2,
          col="black");
  persp(z,tout,u1t,theta=120,phi=25,
        xlim=c(zl,zu),ylim=c(t0,tf),
        xlab="z", ylabel="t",zlab="u1t(z,t)");#
# u2t
  par(mfrow=c(1,1));matplot(x=z,y=u2t,type="l",xlab="z",ylab="u2t(z,t)",
          xlim=c(zl,zu),lty=1,main="",lwd=2,col="black");
  persp(z,tout,u2t,theta=120,phi=25,
        xlim=c(zl,zu),ylim=c(t0,tf),
        xlab="z", ylab="t", zlab="u2t(z,t)");
#
# u3t
  par(mfrow=c(1,1));matplot(x=z,y=u3t,type="1",xlab="z",ylab="u3t(z,t)",xlim=c(z1,zu), lty=1, main="1", lwd=2, col="black");
  persp(z,tout,u3t,theta=120,phi=25,
        xlim=c(zl,zu),ylim=c(t0,tf),
        xlab="z",ylab="t",zlab="u3t(z,t)");
```
In summary, the main program consists of Listings 5.1, 6.1, 6.3.

# **ODE/MOL routine**

The ODE/MOL routine is the same as given in Listings 5.2, 6.2.

## **Numerical and graphical output**

The graphical output from Listings 5.1, 6.1, 6.3 for  $\frac{\partial u_1(z,t)}{\partial t}$ ,  $\frac{\partial u_2(z,t)}{\partial t}$ ,  $\frac{\partial u_3(z,t)}{\partial t}$  follows (the numerical and graphical output for  $u_1(z,t)$ ,  $u_2(z,t)$ ,  $u_2(z,t)$  was presented previously in Tables 6.2, 6.3 and Figures 6.1-1,...,8). Figure 6.9-1 indicates  $\frac{\partial u_1}{\partial t} < 0$  with a reversal in  $u_{1e}(t)$  at  $t = 0.5$ . Figure 6.9-2 confirms Figure 6.9-1. Figure 6.10-1 indicates  $\frac{\partial u_2}{\partial x} < 0$  with a reversal in *u* ∂*t*  $_{1e}(t)$  at  $t = 0.5$ .



**Figure 6.9-1**  $\frac{\partial u_1(z,t)}{\partial t}$  from eqs. (3.1), 2D, ncase=2

Figure 6.10-2 confirms Figure 6.10-1.

Figure 6.11-1 indicates  $\frac{\partial u_3}{\partial x}$  < 0 and continuing decrease of *u* ∂*t* <sup>3</sup> with *t*. This decrease in  $u_3(z,t)$  results from the single RHS term in eq. (5.1-1),  $-k_{r3}(u_{2n}-u_2) < 0$ . Figure 6.11-2 confirms Figure 6.11-1. ∂*u*

The constant  $k_{r3}$  is a sensitive parameter since if  $-k_{r3}(u_{2n} - u_2) < 0$  remains in effect for a long enough time,  $u_3(z,t) < 0$  (negative neuron cell density) could occur



**Figure 6.9-2**  $\frac{\partial u_1(z,t)}{\partial t}$  from eqs. (3.1), 3D, ncase=2

(which is physically impossible). This example illustrates a possibly fundamental limitation of a mathematical model, that is, the model solutions can assume physically unrealistic values (e.g., negative concentrations).

In the present case, this situation could possibly be avoided by using a nonlinear, logistic rate,  $-k_{r3}(u_{2n} - u_2)u_3$  so that as  $u_3(z,t) \rightarrow 0$  the rate approaches zero (rather than remain negative). This extension of eq. (5.1-1) is left as an exercise.

For ncase=3, the graphical output is shown in Figures 6.12,13,14.

Figure 6.12-1 indicates  $\frac{\partial u_1}{\partial t}$  < 0 and movement toward a zero-derivative equilibrium (steady state) solution.

Figure 6.12-2 confirms Figure 6.12-1.

Figure 6.13-1 indicates  $\frac{\partial u_2}{\partial t} < 0$  and movement toward a zero-derivative equilibrium (steady state) solution.



**Figure 6.10-1**  $\frac{\partial u_2(z,t)}{\partial t}$  from eqs. (3.2), 2D, ncase=2

Figure 6.13-2 confirms Figure 6.13-1.

Figure 6.14-1 indicates  $\frac{\partial u_3}{\partial x}$  < 0 and continuing decrease of *u* ∂*t*  $\frac{3}{x}$  < 0 and continuing decrease of  $u_3$  with *t*. This decrease in  $u_3(z,t)$  results from the single RHS term in eq. (5.1-1),  $-k_{r3}(u_{2n}-u_2) < 0$ . Figure 6.14-2 confirms Figure 6.14-1.

In summary, the reduction in  $O_2$  concentration of the capillary blood and brain tissue,  $u_1(z,t)$ ,  $u_2(z,t)$ , leads to a reduction in the neuron cell density,  $u_3(z,t)$ . These changes could then explain long Covid cognitive impairment.



**Figure 6.10-2**  $\frac{\partial u_2(z,t)}{\partial t}$  from eqs. (3.2), 3D, ncase=2



**Figure 6.11-1**  $\frac{\partial u_3(z,t)}{\partial t}$  from eqs. (5.1), 2D, ncase=2



**Figure 6.11-2**  $\frac{\partial u_3(z,t)}{\partial t}$  from eqs. (5.1), 3D, ncase=2



**Figure 6.12-1**  $\frac{\partial u_1(z,t)}{\partial t}$  from eqs. (3.1), 2D, ncase=3



**Figure 6.12-2**  $\frac{\partial u_1(z,t)}{\partial t}$  from eqs. (3.1), 3D, ncase=3





**Figure 6.13-1**  $\frac{\partial u_2(z,t)}{\partial t}$  from eqs. (3.2), 2D, ncase=3



**Figure 6.13-2**  $\frac{\partial u_2(z,t)}{\partial t}$  from eqs. (3.3), 3D, ncase=3

## **6.1.3 ANALYSIS OF PDE RHS TERMS**

 $u_1(z,t)$ ,  $u_2(z,t)$ ,  $u_3(z,t)$  are determined by the time derivatives,  $\frac{\partial u_1(z,t)}{\partial t}$ ,  $\frac{\partial u_2(z,t)}{\partial t}$ , ∂*u*3(*z*,*t*)  $\frac{\partial f(x, y)}{\partial t}$  of eqs. (3.1-1), (3.2-1), (5.1-1). These derivatives, in turn, are defined by ∂∂*t***l**<sub>*t*</sub> the  $\text{RHS}$  terms of eqs. (3.1-1), (3.2-1), (5.1-1) so that these terms provide insight into the origin of the features of the solutions. Therefore, the calculation and display of the PDE RHS terms is an important approach to the analysis of the PDE solutions. This type of analysis is demonstrated by the following programming.

#### **Main program**

For the analysis of the RHS of eq. (3.1-1), two terms are calculated and displayed.



**Figure 6.14-1**  $\frac{\partial u_3(z,t)}{\partial t}$  from eqs. (5.1), 2D, ncase=3

\n- term11 = 
$$
-v_z \frac{\partial u_1}{\partial z}
$$
.
\n- term12 =  $-(2/r_l)k_{m1}(u_1 - u_2)$ .
\n

The naming of the terms is according to term-PDE number-term in PDE. For example, term11 is for PDE 1 (eq. (3.1-1)), term 1 (convection).



**Figure 6.14-2**  $\frac{\partial u_3(z,t)}{\partial t}$  from eqs. (5.1), 3D, ncase=3

These terms are calculated by the addition of the following code to the end of Listing 6.3.

```
#
# PDE RHS terms
#
# u1t
#
# Matrices for term11, term12
 term11=matrix(0,nrow=nz,ncol=nout);
 term12=matrix(0,nrow=nz,ncol=nout);
#
# Calculation of term11, term12
```

```
for(it in 1:nout){
 for(iz in 1:nz){
    if(iz==1){term11[1,it]=-vz*(u1[2,it]-u1[1,it])/dz;}
    if(iz>1)term11[iz,it]=-vz*(u1[iz,it]-u1[iz-1,it])/dz;}
    term12[iz,it]=-r1*km1*(u1[iz,it]-u2[iz,it]);
 }
 }
#
# Plot term11
 par(mfrow=c(1,1));
 matplot(x=z[2:nz],y=term11[2:nz,],type="l",xlab="z",
          ylab="term11(z,t)",xlim=c(zl,zu),lty=1,main="",
          lwd=2,col="black");
 persp(z,tout,term11,theta=120,phi=25,
        xlim=c(zl,zu),ylim=c(t0,tf),
        xlab="z", ylab="t", zlab="term11(z,t)");#
# Plot term12
 par(mfrow=c(1,1));matplot(x=z,y=term12,type="l",xlab="z",ylab="term12(z,t)",
          xlim=c(zl,zu),lty=1,main="",lwd=2,col="black");
 persp(z,tout,term12,theta=120,phi=25,
        xlim=c(z1,zu), ylim=c(t0,tf),
        xlab="z",ylab="t",zlab="term12");
```
Listing 6.4: Additional code for the calculation of eq. (3.1-1) RHS terms

We can note the following details about Listing 6.4.

• Matrices are defined for term11, term12.

```
#
   # PDE RHS terms
   #
   # u1t
   #
   # Matrices for term11, term12
     term11=matrix(0,nrow=nz,ncol=nout);
     term12=matrix(0,nrow=nz,ncol=nout);
• term11, term12 are calculated according to eq. (3.1-1).
   #
```

```
# Calculation of term11, term12
 for(it in 1:nout){
```

```
for(iz in 1:nz){
       if(iz==1){term11[1,it]=-vz*(u1[2,it]-u1[1,it])/dz;}
       if(iz>1)term11[iz, it] = -vz*(u1[iz, it] - u1[iz-1, it])/dz;term12[iz, it] = -r1*km1*(u1[iz, it] - u2[iz, it]);}
     }
• term11, term12 are plotted in 2D and 3D.
  #
  # Plot term11
    par(mfrow=c(1,1));
    matplot(x=z[2:nz],y=term11[2:nz],type="1",xlab="z",ylab="term11(z,t)",xlim=c(zl,zu),lty=1,main="",
             lwd=2,col="black");
     persp(z,tout,term11,theta=120,phi=25,
           xlim=c(zl,zu),ylim=c(t0,tf),
           xlab="z", ylab="t", zlab="term11(z,t)");#
  # Plot term12
     par(mfrow=c(1,1));
     matplot(x=z,y=term12,type="l",xlab="z",ylab="term12(z,t)",
             xlim=c(zl,zu),lty=1,main="",lwd=2,col="black");
     persp(z,tout,term12,theta=120,phi=25,
           xlim=c(zl,zu),ylim=c(t0,tf),
           xlab="z",ylab="t",zlab="term12");
```
# **ODE/MOL routine**

The ODE/MOL routine is pde3a of Listings 5.2, 6.2.

# **Numerical and graphical output**

The graphical output for ncase=3, (set in Listing 5.1) is in Figures 6.15,16.

Figure 6.15-1 indicates that term11 at  $z = z_l$  is not included (from  $x=z[2:nz]$ ,  $y=term11[2:nz,]$ ). Figure 6.15-2 confirms Figure 6.15-1.

Figure 6.16-1 indicates that term12 at  $z = z_l$  is included (from x=z, y=term12). Figure 6.16-2 confirms Figure 6.16-1.

A similar analysis can be applied for the remaining PDE RHS terms.

• term21 = 
$$
D_2 \frac{\partial^2 u_2}{\partial z^2}
$$
 (eq. (3.2-1)).

• term22 = 
$$
\frac{2r_l}{(r_u^2 - r_l^2)} k_{m1}(u_1 - u_2)
$$
 (eq. (3.2-1)).

• term31 = 
$$
-k_{r3}(u_{2n} - u_2)
$$
 (eq. (5.1-1)).





**Figure 6.15-1** term11 from Listing 6.4, 2D, ncase=3

The calculation and display of these terms is left as an exercise.

The computation and display of PDE RHS terms is an important methodology for evaluating the physical/chemical/biological contributions to a PDE model. For example, eq. (3.1-1) can be stated as

$$
\frac{\partial u_1}{\partial t} = term_{11} + term_{12}
$$



**Figure 6.15-2** term11 from Listing 6.4, 3D, ncase=3

so that  $term_{11} + term_{12}$  defines the derivative  $\frac{\partial u_1}{\partial t}$ , which, in turn, determines through MOL numerical integration  $u_1(z,t)$ . By examining  $term_{11}$ ,  $term_{12}$ , the relative contributions of convection and  $O_2$  mass transfer across the BBB can be observed. ∂*u*

This is illustrated in Figures 6.15,16. Figure 6.15 indicates  $term_{11} < 0$  while Figure 6.16 indicates  $term_{12} > 0$ . Furthermore, the two terms have the same general form so that they tend to sum to a small value. If they sum to zero,  $\frac{\partial u_1}{\partial x_1}$  $= 0$ ∂*t* corresponding to an equilibrium solution for  $u_1(z,t)$ . That is, convection is balanced by mass transfer. This detailed insight into the solution of eq. (3.1-1) can then be used to adjust parameters and possibly alter the form of the RHS terms (the variation of a PDE *t* derivative is illustrated in Figures 6.9,12. for eq. (3.1-1)).



**Figure 6.16-1** term12 from Listing 6.4, 2D, ncase=3

The methodology of examining the PDE RHS terms can be readily applied to all of the model PDEs once numerical solutions (PDE dependent variables) have been calculated, to provide insight into the differences of the solutions in *t* and *z*. An important special case in physical applications modeled by systems of simultaneous PDEs is when (1) certain PDEs have equilibrium solutions and (2) other PDEs have dynamic solutions. These hybrid systems are termed "stiff" and generally can be accommodated within the MOL framework.



**Figure 6.16-2** term12 from Listing 6.4, 3D, ncase=3

#### **6.1.4 SUMMARY AND CONCLUSIONS**

Two cases of the three PDE model of eqs. (3.1), (3.2), (5.1) are developed in this chapter. For the second case, the PDE analysis is illustrated by: (1) the calculation and display of the derivatives  $\frac{\partial u_1}{\partial x_1}$  $\frac{\partial u_1}{\partial t}, \frac{\partial u_2}{\partial t}$  $\frac{\partial u_2}{\partial t}, \frac{\partial u_3}{\partial t}$  $\frac{\partial u}{\partial t}$ , and (2) the calculation and display of the PDE RHS terms. These additional calculations are based on the computed solutions  $u_1(z,t)$ ,  $u_2(z,t)$ ,  $u_3(z,t)$  and provide additional insight into the origin of the features of the PDE solutions, particularly the approach to an equilibrium (steady state).

#### **REFERENCE**

1. Soetaert, K., J. Cash, and F. Mazzia (2012), *Solving Differential Equations in R*, Springer-Verlag, Heidelberg, Germany.

# Appendix A: Introduction to PDE Analysis

The intent of this appendix is to provide an introduction to computer-based modeling based on partial differential equations (PDEs).

## **A.1 PDE NOTATION**

If a biological/chemical/physical application is to be modeled in both space and time (spatiotemporal analysis), PDEs are an established mathematical form for the model. The notation used in the model PDEs is reviewed next.

If a model PDE defines a dependent variable,  $u(z,t)$ , as a function of the independent variables, *z* (space) and *t* (time), then the partial derivative of  $u(z,t)$  with respect

∂*u* ∂*u* to *z* and *t*, is denoted, respectively, as  $\frac{\partial u}{\partial z}$  and  $\frac{\partial u}{\partial t}$ .

 $\frac{\partial u}{\partial z}$  is the rate of change of *u*(*z*,*t*) with respect to *z* at constant *t*.  $\frac{\partial u}{\partial t}$  is the rate of change of  $u(z,t)$  with respect to *t* at constant *z*. These derivatives are first order in *z* and *t*, respectively.

To facilitate the coding (programming) of PDEs, a subscript notation for partial derivatives is often used.

$$
\frac{\partial u}{\partial z} \Rightarrow u_z; \ \frac{\partial u}{\partial t} \Rightarrow u_t
$$

Derivatives of order higher than one can be considered for PDE models.

$$
\frac{\partial \left(\frac{\partial u(z,t)}{\partial z}\right)}{\partial z} = \frac{\partial^2 u(z,t)}{\partial z^2} = u_{zz}
$$

$$
\frac{\partial \left(\frac{\partial u(z,t)}{\partial t}\right)}{\partial t} = \frac{\partial^2 u(z,t)}{\partial t^2} = u_{tt}
$$

$$
\frac{\partial \left(\frac{\partial u(z,t)}{\partial z}\right)}{\partial t} = \frac{\partial^2 u(z,t)}{\partial t \partial z} = u_{tz} = \frac{\partial \left(\frac{\partial u(z,t)}{\partial t}\right)}{\partial z} = \frac{\partial^2 u(z,t)}{\partial z \partial t} = u_{zt}
$$

The third form of the second derivative is termed a mixed partial derivative, for which the order of differentiation in *z* and *t* is assumed to be interchangeable.

PDE spatial derivatives can be expressed in different coordinate systems. For example,
- Cartesian coordinates,  $(x, y, z)$ :  $x, y, z$  are defined along mutually perpendicular (orthogonal) axes [1].
- cylindrical coordinates,  $(r, \theta, z)$ :  $r, \theta, z$  are defined along mutually perpendicular axes. *r* is a radial coordinate [2].  $\theta$  is an angular coordinate. *z* is an axial coordinate.
- **spherical coordinates**,  $(r, \theta, \phi)$ :  $r, \theta, \phi$  are defined along mutually perpendicular axes. *r* is a radial coordinate [3].  $\theta$ ,  $\phi$  are angular coordinates.

Other coordinate systems can be derived from general curvilinear coordinates [4]. The choice of a particular coordinate system is usually determined by the match of the boundary conditions (discussed subsequently) to the geometry of the physical system.

# **A.2 PDE CLASSIFICATION**

PDEs can be classified geometrically which facilitates the selection of numerical methods (algorithms) for the computer solution of PDEs. The generally accepted geometrical classifications are summarized next.

#### **A.2.1 HYPERBOLIC**

Hyperbolic PDEs are of two types:

First order: If the PDE is first order in the initial value (temporal) variable *t*, and first order in the boundary value (spatial) variable  $z$ , it is generally termed firstorder hyperbolic. As an example, the linear, first-order hyperbolic (advection) PDE equation, is

$$
\frac{\partial u}{\partial t} + v_z \frac{\partial u}{\partial z} = 0 \tag{A.1-1}
$$

For a complete (well-posed) problem, one initial condition (IC) and one boundary condition (BC) are required.

$$
u(z, t = 0) = f(z)
$$
 (A.1-2)

$$
u(z = 0, t) = g(t)
$$
 (A.1-3)

where  $f(z)$ ,  $g(t)$  are functions to be specified. As an example that is subsequently integrated numerically,  $f(z) = 0, g(t) = 1$ , for which an analytical (exact) solution is available.

If  $\lambda = z - v_z t$  (Lagrangian coordinate, traveling wave),  $u(z,t) = u(\lambda)$ , and eqs. (A.1) can be stated in terms of  $\lambda$ .

$$
\frac{\partial u}{\partial t} = \frac{du}{d\lambda} \frac{\partial \lambda}{\partial t} = -v_z \frac{du}{d\lambda}
$$

$$
\frac{\partial u}{\partial z} = \frac{du}{d\lambda} \frac{\partial \lambda}{\partial z} = \frac{du}{d\lambda}
$$

Substitution in eq. (A.1-1) gives

$$
\frac{\partial u}{\partial t} + v_z \frac{\partial u}{\partial z} = -v_z \frac{du}{d\lambda} + v_z \frac{du}{d\lambda} = 0
$$

Thus,  $u(\lambda)$  is a solution to eqs. (A.1) with  $u(\lambda > 0) = 0$  (IC (A.1-2),  $f(z) = 0$ ),  $u(\lambda < 0) = 1$  (BC (A.1-3)  $g(t) = 1$ ) (a unit step or Heaviside function, traveling left to right in *z* with velocity  $v_z$ ). This special case of the advection equation is used subsequently in evaluating (testing) a numerical solution.

Second order: If the PDE is second order in the initial value (temporal) variable *t*, and second order in the boundary value (spatial) variable *z*, it is generally termed second-order hyperbolic. For example, the linear wave equation, is

$$
\frac{\partial^2 u}{\partial t^2} = c^2 \frac{\partial^2 u}{\partial z^2}; \ u_{tt} = c^2 u_{zz}
$$
 (A.2-1)

where *c* is a wave velocity.

Equation (A.2-1) is second order in *t* and requires two ICs,

$$
u(z,t=0) = f_1(z); \ \frac{\partial u(z,t=0)}{\partial t} = u_t(z,t=0) = f_2(z) \tag{A.2-2,3}
$$

where  $f_1(z)$ ,  $f_2(z)$  are functions to be specified.

Equation  $(A.2-1)$  is second order in *z* and requires two BCs, for example

$$
u(z = z_l, t) = g_1(z); \ \frac{\partial u(z = z_u, t)}{\partial z} = g_2(z) \tag{A.2-4,5}
$$

where  $z_l$ ,  $z_u$  are lower and upper boundary values of *z*, respectively, and  $g_1(z)$ ,  $g_2(z)$ are functions to be specified. Equation (A.2-4) is a Dirichlet  $BC<sup>1</sup>$  and eq. (A.2-5) is a Neumann BC.

A second-order hyperbolic PDE can be expressed as a system of two first-order hyperbolic PDEs. For example,  $u(z,t)$ ,  $v(z,t)$  can be defined by two simultaneous first-order hyperbolic PDEs.

$$
\frac{\partial v}{\partial z} = \frac{\partial u}{\partial t} \tag{A.3-1}
$$

$$
\frac{\partial v}{\partial t} = \frac{\partial u}{\partial z} \tag{A.3-2}
$$

If eq. (A.3-1) is differentiated with respect to *t* and eq. (A.3-2) is differentiated with respect to *z*,

$$
\frac{\partial^2 v}{\partial t \partial z} = \frac{\partial^2 u}{\partial t^2}
$$
 (A.3-3)

$$
\frac{\partial^2 v}{\partial z \partial t} = \frac{\partial^2 u}{\partial z^2}
$$
 (A.3-4)

<sup>&</sup>lt;sup>1</sup>A Dirichlet BC specifies the dependent variable,  $u(z,t)$ , at the boundary. A Neumann BC specifies the first-order spatial derivative of  $u(z,t)$  with respect to z at the boundary. A Robin BC includes both the dependent variable and the first-order spatial derivative, frequently as a linear combination, e.g.,  $D\frac{\partial u(z = z_u, t)}{\partial z} + k_m u(z = z_u, t) = 0.$ 

If eq.  $(A.3-4)$  is subtracted from eq.  $(A.3-3)$ ,

$$
\frac{\partial^2 v}{\partial t \partial z} - \frac{\partial^2 v}{\partial z \partial t} = \frac{\partial^2 u}{\partial t^2} - \frac{\partial^2 u}{\partial z^2}
$$

or if the mixed partial derivatives are assumed equal

$$
\frac{\partial^2 u}{\partial t^2} = \frac{\partial^2 u}{\partial z^2}
$$

which is eq.  $(A.2-1)$  with  $c = 1$ . This result suggests second-order hyperbolic PDEs can be studied through associated systems of first-order PDEs.

A second-order hyperbolic PDE can also be expressed as a system of PDEs first order in *t* and second order in *z*. For example, if two variables,  $u_1(z,t)$  and  $u_2(z,t)$ , are defined as

$$
u_1(z,t) = u(z,t); \ u_2(z,t) = \frac{\partial u}{\partial t} = \frac{\partial u_1}{\partial t}
$$

eq. (A.2-1) can be written as

$$
\frac{\partial u_1}{\partial t} = u_2(z,t); \ \frac{\partial u_2}{\partial t} = \frac{\partial^2 u_1}{\partial z^2}
$$

This formulation is particularly useful when numerically integrating second-order hyperbolic PDEs.

#### **A.2.2 PARABOLIC**

Parabolic PDEs are first order in an initial value variable and second order in a boundary value variable. The diffusion equation (heat conduction equation, Fick's second law, Fourier's second law) is an example.

$$
\frac{\partial u}{\partial t} = D \frac{\partial^2 u}{\partial z^2}
$$
 (A.4-1)

where *D* is a diffusivity. Equation  $(A.4-1)$  is first order in *t* and requires one IC.

$$
u(z, t = 0) = f(z)
$$
 (A.4-2)

Equation (A.4-1) is second order in *z* and requires two BCs, for example

$$
u(z = z_l, t) = g(t); \, D \frac{\partial u(z = z_u, t)}{\partial z} + k_m u_z(z = z_u, t) = 0 \tag{A.4-3,4}
$$

where  $z_l$ ,  $z_u$  are lower and upper boundary values of *z*, respectively,  $k_m$  is a mass transfer coefficient, and  $f(z)$ ,  $g(t)$  are functions to be specified. Equation (A.4-3) is a Dirichlet BC and eq. (A.4-4) is a Robin BC (explained previously).

Equation (A.4-1) is based on a material (mass) balance for an incremental volume  $A_c\Delta z$ .

$$
A_c \Delta z \frac{\partial u}{\partial t} = -A_c D \frac{\partial u}{\partial z}\bigg|_{z} - \left(-A_c D \frac{\partial u}{\partial z}\bigg|_{z + \Delta z}\right) \tag{A.4-5}
$$

**Appendix A** 

The diffusive flux into and out of the incremental volume is based on Fick's first law (Fourier's first law).

$$
q = -D\frac{\partial u}{\partial z} \tag{A.4-6}
$$

with  $q > 0$  for  $\frac{\partial u}{\partial z} < 0$  (diffusion in the direction of decreasing *u*(*z*,*t*)).

Division of eq. (A.4-5) by *Ac*∆*z* and minor rearrangement gives

$$
\frac{\partial u}{\partial t} = D \left( \frac{\frac{\partial u}{\partial z} \Big|_{z + \Delta z} - \frac{\partial u}{\partial z} \Big|_{z}}{\Delta z} \right) \tag{A.4-7}
$$

With  $\Delta z \rightarrow 0$ , eq. (A.4-7) is eq. (A.4-1).

The diffusion equation can be expressed in terms of the coordinate-independent vector differential operator ∇.

$$
\frac{\partial u}{\partial t} = D \nabla \cdot \nabla u = D \text{ div grad } u \tag{A.4-8}
$$

where  $\nabla \cdot$  is the divergence of a vector and  $\nabla$  is the gradient of a scalar.  $\nabla$  can then be stated for a particular coordinate system. This is done in the following tables for Cartesian, cylindrical and spherical coordinates.

∇· (divergence of a vector):

Coordinate system Components  $\left[ \nabla \right]_x = \frac{\partial}{\partial x}$  $\begin{bmatrix} [\nabla]_x = \frac{\partial}{\partial x} \\ \nabla \cdot \mathbf{1} & \partial \end{bmatrix}$  $\partial x$  $\left| \left[ \nabla \right]_{y} = \frac{\partial}{\partial y} \right|$ Cartesian  $\begin{bmatrix} [\nabla]_y = \frac{\partial}{\partial y} \\ [\nabla]_z = \frac{\partial}{\partial z} \end{bmatrix}$  $\lceil \frac{1}{2} \frac{\partial}{\partial x} \rceil$  $\overline{\phantom{a}}$  $[\nabla]_r = \frac{1}{r} \frac{\partial}{\partial r}(r)$  $\begin{bmatrix} \n\Gamma^T r & r \, \partial r & r \ \n\end{bmatrix}$   $\begin{bmatrix} \n\nabla \end{bmatrix}_0 = \frac{1}{r} \frac{\partial}{\partial r}$ cylindrical  $\begin{bmatrix} [\nabla]_{\theta} = \frac{1}{r} \frac{\partial}{\partial \theta} \\ \frac{\partial}{\partial \theta} \end{bmatrix}$ *r* ∂ θ  $\left[ \nabla \right]_z = \frac{\partial}{\partial z}$  $\left[\nabla\right]_r = \frac{1}{r^2} \frac{\partial}{\partial r} (r^2) \qquad \left[\nabla\right]_r = \frac{1}{r^2} \frac{\partial}{\partial r} (r^2)$  $\overline{1}$ )  $\begin{bmatrix} \n\begin{bmatrix} \n\mathbf{v} \end{bmatrix}_r - r^2 \, \partial r \end{bmatrix}$ <br>  $\begin{bmatrix} \n\nabla \end{bmatrix}_\theta = \frac{1}{\sqrt{2\pi}} \frac{\partial}{\partial \theta} (\sin \theta) \end{bmatrix}$ 

spherical

$$
\mathcal{L}^{\text{max}}_{\text{max}}
$$

 $\left[\nabla\right]_{\theta} = \frac{1}{r \sin \theta} \frac{\partial}{\partial \theta} (\sin \theta)\n\left[\n\begin{array}{c}\n\end{array}\right]$  $\begin{bmatrix} r \sin \theta & \theta \end{bmatrix}$  $r\sin\theta \, \partial\theta$ 

 $\left[ \nabla \right]_{\phi} = \frac{1}{r \sin \theta} \frac{\partial}{\partial \phi}$ 

$$
f_{\rm{max}}
$$

∇ (gradient of a scalar):



∇·∇ (divergence of the gradient of a scalar):

Coordinate system Component

Cartesian

\n
$$
\frac{\partial^2}{\partial x^2} + \frac{\partial^2}{\partial y^2} + \frac{\partial^2}{\partial z^2}
$$
\ncylindrical

\n
$$
\left(\frac{\partial^2}{\partial r^2} + \frac{1}{r}\frac{\partial}{\partial r}\right) + \frac{1}{r^2}\frac{\partial^2}{\partial \theta^2} + \frac{\partial^2}{\partial z^2}
$$
\nspherical

\n
$$
\left(\frac{\partial^2}{\partial r^2} + \frac{2}{r}\frac{\partial}{\partial r}\right) + \frac{1}{r^2 \sin \theta} \frac{\partial}{\partial \theta} \left(\sin \theta \frac{\partial}{\partial \theta}\right) + \frac{1}{r^2 \sin^2 \theta} \frac{\partial^2}{\partial \phi^2}
$$

Cartesian coordinates:

With the orthonormal vectors  $(i_x, j_y, k_z)$ ,  $\nabla \cdot \nabla$  in the RHS of eq. (A.4-8) follows as

$$
\nabla \cdot \nabla = \left( \mathbf{i} \frac{\partial}{\partial x} + \mathbf{j} \frac{\partial}{\partial y} + \mathbf{k} \frac{\partial}{\partial z} \right) \cdot \left( \mathbf{i} \frac{\partial}{\partial x} + \mathbf{j} \frac{\partial}{\partial y} + \mathbf{k} \frac{\partial}{\partial z} \right) = \frac{\partial^2}{\partial x^2} + \frac{\partial^2}{\partial y^2} + \frac{\partial^2}{\partial z^2}
$$

Cylindrical coordinates:

With the orthonormal vectors  $(i_r, j_\theta, k_z)$ ,  $\nabla \cdot \nabla$  in the RHS of eq. (A.4-8) follows as

$$
\nabla \cdot \nabla = \left( \mathbf{i}_r \frac{1}{r} \frac{\partial}{\partial r} (r) + \mathbf{j}_\theta \frac{1}{r} \frac{\partial}{\partial \theta} + \mathbf{k}_z \frac{\partial}{\partial z} \right) \cdot \left( \mathbf{i}_r \frac{\partial}{\partial r} + \mathbf{j}_\theta \frac{1}{r} \frac{\partial}{\partial \theta} + \mathbf{k}_z \frac{\partial}{\partial z} \right)
$$
  
\n
$$
= \frac{1}{r} \frac{\partial}{\partial r} \left( r \frac{\partial}{\partial r} \right) + \frac{1}{r} \frac{\partial}{\partial \theta} \left( \frac{1}{r} \frac{\partial}{\partial \theta} \right) + \frac{\partial}{\partial z} \left( \frac{\partial}{\partial z} \right)
$$
  
\n
$$
= \frac{1}{r} \left( \frac{\partial}{\partial r} + r \frac{\partial^2}{\partial r^2} \right) + \frac{1}{r^2} \frac{\partial}{\partial \theta} \frac{\partial}{\partial \theta} + \frac{\partial}{\partial z} \frac{\partial}{\partial z}
$$
  
\n
$$
= \left( \frac{\partial^2}{\partial r^2} + \frac{1}{r} \frac{\partial}{\partial r} \right) + \frac{1}{r^2} \frac{\partial^2}{\partial \theta^2} + \frac{\partial^2}{\partial z^2}
$$

Spherical coordinates:

With the orthonormal vectors  $(i_r, j_\theta, k_\phi)$ ,  $\nabla \cdot \nabla$  in the RHS of eq. (A.4-8) follows as

$$
\nabla \cdot \nabla = \left( \mathbf{i}_r \frac{1}{r^2} \frac{\partial}{\partial r} (r^2) + \mathbf{j}_{\theta} \frac{1}{r \sin \theta} \frac{\partial}{\partial \theta} (\sin \theta) + \mathbf{k}_{\phi} \frac{1}{r \sin \theta} \frac{\partial}{\partial \phi} \right)
$$
  
\n
$$
\times \left( \mathbf{i}_r \frac{\partial}{\partial r} + \mathbf{j}_{\theta} \frac{1}{r} \frac{\partial}{\partial \theta} + \mathbf{k}_{\phi} \frac{1}{r \sin \theta} \frac{\partial}{\partial \phi} \right)
$$
  
\n
$$
= \frac{1}{r^2} \frac{\partial}{\partial r} \left( r^2 \frac{\partial}{\partial r} \right) + \frac{1}{r \sin \theta} \frac{\partial}{\partial \theta} \left( \sin \theta \frac{1}{r} \frac{\partial}{\partial \theta} \right) + \frac{1}{r \sin \theta} \frac{\partial}{\partial \phi} \left( \frac{1}{r \sin \theta} \frac{\partial}{\partial \phi} \right)
$$
  
\n
$$
= \left( \frac{\partial^2}{\partial r^2} + \frac{2}{r} \frac{\partial}{\partial r} \right) + \frac{1}{r^2 \sin \theta} \frac{\partial}{\partial \theta} \left( \sin \theta \frac{\partial}{\partial \theta} \right) + \frac{1}{r^2 \sin^2 \theta} \frac{\partial^2}{\partial \phi^2}
$$

Equation (A.4-8) can be extended to include a convection term.

$$
\frac{\partial u}{\partial t} = (-\nabla \cdot \mathbf{v} + D \nabla \cdot \nabla) u = (-\text{div } \mathbf{v} + D \text{ div grad }) u \tag{A.4-9}
$$

where **v** is a velocity vector. In the three coordinate systems,

Cartesian : 
$$
\mathbf{v} = \mathbf{i}_x v_x + \mathbf{j}_y v_y + \mathbf{k}_z v_z
$$
  
cylindrical :  $\mathbf{v} = \mathbf{i}_r v_r + \mathbf{j}_\theta v_\theta + \mathbf{k}_z v_z$   
spherical :  $\mathbf{v} = \mathbf{i}_r v_r + \mathbf{j}_\theta v_\theta + \mathbf{k}_\phi v_\phi$ 

As a prototype model that can be used to test numerical integration algorithms for parabolic PDEs, the following IC and BCs for eq. (A.4-1) are considered subsequently.

$$
u(z, t = 0) = f(z) = \sin(\pi(z - z_l)/(z_u - z_l))
$$
 (A.4-10)

$$
u(z = z_l, t) = u(z = z_u, t) = 0
$$
\n(A.4-11, 12)

Equations (A.4-11,12) define homogeneous Dirichlet BCs.

As a second case,

$$
u(z, t = 0) = f(z) = \cos(\pi(z - z_l)/(z_u - z_l))
$$
 (A.4-13)

$$
\frac{\partial u(z=z_l,t)}{\partial z} = \frac{\partial u(z=z_u,t)}{\partial z} = 0
$$
 (A.4-14,15)

Equations (A.4-14,15) define homogeneous Neumann BCs.

$$
D\frac{\partial u(z=z_l,t)}{\partial z} + k_m u(z=z_l,t) = 0
$$
  

$$
D\frac{\partial u(z=z_u,t)}{\partial z} + k_m u(z=z_u,t) = 0
$$
 (A.4-16,17)

Equations (A.4-16,17) define homogeneous Robin BCs.

An exact solution to eqs. (A.4-1), (A.4-10,11,12),

$$
u(z,t) = e^{-D(\pi/(z_u - z_l))^2 t} \sin(\pi(z - z_l)/(z_u - z_l))
$$
 (A.4-18)

and an exact solution to eqs. (A.4-1), (A.4-13,14,15),

$$
u(z,t) = e^{-D(\pi/(z_u - z_l))^2 t} \cos(\pi(z - z_l)/(z_u - z_l))
$$
 (A.4-19)

are used subsequently to test numerical FD integration algorithms implemented within the method of lines (MOL) framework. An exact solution to eq. (A.4-1), (A.4- 16,17) is available, but it is relatively complicated so it is not included here.

As the term diffusion equation implies (eq. (A.4-1)), parabolic PDEs smooth steep moving fronts and discontinuities, and therefore are easier to integrate numerically than hyperbolic PDEs (such as eq. (A.1-1)).

#### **A.2.3 ELLIPTIC**

Elliptic PDEs are zeroth order in an initial value variable (no derivative in *t*) and second order in two boundary value variables. Laplace's equation is an example.

$$
\frac{\partial^2 u}{\partial y^2} + \frac{\partial^2 u}{\partial z^2} = 0
$$
 (A.5-1)

Equation (A.5-1) is second order in *y* and *z* and requires two BCs for each. For example,

$$
u(y = y_l, z) = f_1(z); \ \frac{\partial u(y = y_u, z)}{\partial y} = f_2(z) \tag{A.5-2,3}
$$

$$
u(y, z = z_l) = g_1(y); \ \frac{\partial u(y, z = z_u)}{\partial z} = g_2(z) \tag{A.5-4,5}
$$

One approach to the numerical integration of elliptic PDEs is to append a derivative in an initial value variable. For example, for eq. (A.5-1),

$$
\frac{\partial u}{\partial t} = \frac{\partial^2 u}{\partial y^2} + \frac{\partial^2 u}{\partial z^2}
$$
 (A.5-6)

that is, to effectively convert the elliptic PDE to a parabolic PDE, then integrate the parabolic equation to a steady state. For example, for eq. (A.5-6),  $\frac{\partial u}{\partial t} \approx 0$ , at which point the solution  $u(y, z, t \rightarrow \infty)$  is the solution to the elliptic PDE.

This approach to a numerical solution of the elliptic PDE is termed the method of false transients since *t* is not part of the original elliptic problem, but rather, is a parameter that continues the solution of the parabolic PDE to the solution of the elliptic PDE.

# **A.2.4 MULTITYPE**

More than one geometric form can be included in a PDE. For example, a combination of eqs.  $(A.1-1)$  and  $(A.4-1)$  gives

$$
\frac{\partial u}{\partial t} = -v_z \frac{\partial u}{\partial z} + D \frac{\partial^2 u}{\partial z^2}
$$
 (A.6-1)

Equation (A.6-1) mathematically is a hyperbolic-parabolic PDE, and physically, a convection-diffusion equation.

Equation (A.6-1) is first order in *t* and requires one IC.

$$
u(z, t = 0) = f(z)
$$
 (A.6-2)

where  $f(z)$  is a function to be specified.

Equation (A.6-1) is second order in *z* and requires two BCs, e.g.,

$$
u(z = z_l, t) = g(t); \frac{\partial u(z = u, t)}{\partial z} = 0
$$
 (A.6-3,4)

where  $g(t)$  is a function to be specified.

BC (A.6-4) specifies a zero slope (derivative in *z*) at  $z = z_u$ . If the solution  $u(z,t)$ is a discontinuity (step) traveling in the positive *z* direction ( $v_z > 0$ ) as discussed previously, eq. (A.6-4) requires the discontinuity move across the exit boundary at  $z = z_u$  with zero slope. Since this is essentially impossible, the solution displays a numerical error (artifact) such as an oscillation.

To avoid this situation of an unrealistic exit BC, the following condition can be used.

$$
\frac{\partial u(z=z_u,t)}{\partial t} + v_z \frac{\partial u(z=z_u,t)}{\partial z} = 0
$$
 (A.6-5)

Equation (A.6-5) qualifies as a BC for eq.  $(A.6-1)$  since it is of lower order in *z* than eq. (A.6-1), Experience has indicated that BC (A.6-5) provides a smooth exit of a discontinuity at  $z = z_u$ .

If a volumetric source term is added to eq. (A.6-1),

$$
\frac{\partial u}{\partial t} = -v_z \frac{\partial u}{\partial z} + D \frac{\partial^2 u}{\partial z^2} + k_r u^p \tag{A.6-6}
$$

eq. A.6-6 mathematically is still hyperbolic-parabolic, and physically is a convection-diffusion-reaction equation. If  $p \neq 1$ , eq. (A.6-6) is also nonlinear, i.e., it is not of first degree (the distinction between order and degree is noteworthy). ̸

### **A.3 FIRST-ORDER SPATIAL DERIVATIVES**

The implementation of eq.  $(A.6-6)$  in a series of R routines<sup>2</sup> is considered next, ∂*u* starting with the approximation of the first-order spatial derivative  $\frac{\partial u}{\partial z}$ .

# **A.3.1 FINITE DIFFERENCES**

The derivative in *z*,  $\frac{\partial u}{\partial z}$ , in eqs. (A.1-1), (A.6-1), (A.6-6) can be approximated by a two-point, upwind<sup>3</sup> finite difference (FD). ∂*u*

$$
\frac{\partial u}{\partial z} \approx \frac{u(z,t) - u(z - \Delta z, t)}{\Delta z} + O(\Delta z)
$$
 (A.7-1)

where  $\Delta z$  is the interval in *z* for a FD grid of  $n_z$  points

$$
\Delta z = \frac{z_u - z_l}{n_z - 1} \tag{A.7-2}
$$

 $O(\Delta z)$  indicates that the truncation error of the FD approximation of eq. (A.7-1) is first order (first degree) in ∆*z*.

Substitution of approximation  $(A.7-1)$  in eq.  $(A.1-1)$  gives

$$
\frac{\partial u(z,t)}{\partial t} = -v_z \frac{u(z,t) - u(z - \Delta z, t)}{\Delta z}
$$
 (A.7-3)

Equation (A.7-3) is a system of ODEs<sup>4</sup>.

$$
\frac{du_i}{dt} = -v_z \frac{u_i - u_{i-1}}{\Delta z}; i = 1, 2, ..., n_z
$$
\n(A.7-4)

If IC (A.1-2) is a unit step (Heaviside function),  $h(t)$ ,

$$
h(t) = \begin{cases} 1, & t < 0 \\ 0, & t > 0 \end{cases}
$$
 (A.7-5)

the exact (analytical) solution to eq.  $(A.1-1)$  (also discussed after eq.  $(A.1-3)$ ) is

$$
u(z,t) = u(z - v_z t) = h(z - v_z t)
$$
 (A.7-6)

which can be used to test the MOL numerical solution, eq. (A.7-3).

 ${}^{2}R$  is a quality, open-source scientific computing system that is easily downloaded from the Internet.

<sup>&</sup>lt;sup>3</sup>Upwind refers to the use of *u*(*z* − ∆,*t*) in the FD which is upstream of *u*(*z*,*t*) (with *v*<sub>*z*</sub> > 0). As expected,  $u(z-\Delta,t)$  affects  $u(z,t)$  by convection. If the downwind (downstream) value  $u(z+\Delta z,t)$  is used in the FD approximation, the resulting ordinary differential equation (ODE) system is unstable (unbounded  $u(z,t)$  with increasing *t*).

 $4E$  Equation (A.7-3) is an example of the method of lines (MOL) approximation of a PDE as a series of ODEs. The MOL is a general numerical method (algorithm) in which the spatial derivatives of a PDE are replaced with an algebraic approximation, in this case, a FD. The approximating ODEs are then integrated by a library initial value ODE integrator.

```
A main program for eqs. (a.1) and (A.7) follows.
```

```
#
# First order hyperbolic PDE
# (advection equation)
#
# Delete previous workspaces
  rm(list=ls(all=TRUE))
#
# Access ODE integrator
  library("deSolve");
#
# Access functions for numerical solution
  setwd("f:/Covid-19 neurological effects/appA");
  source("pde1a.R");
  source("step.R");
#
# Set case
  ncase=1;
#
# Parameters
 nz=21;
  vz=1;
  ue=1;
#
# Spatial grid in z
  zl=0;zu=1;dz=(zu-zl)/(nz-1);
  z=seq(from=zl,to=zu,by=dz);
#
# Independent variable for ODE integration
  t0=0; t f=1; nout=5;tout=seq(from=t0,to=tf,by=(tf-t0)/(nout-1));
#
# Initial condition (t=0)
  u0=rep(0,nz);ncall=0;
#
# ODE integration
  out=lsodes(y=u0,times=tout,func=pde1a,
      sparsetype="sparseint",rtol=1e-6,
      atol=1e-6,maxord=5);
  nrow(out)
  ncol(out)
#
# Arrays for plotting numerical, exact solutions
```

```
u=matrix(0,nrow=nz,ncol=nout);
  uex=matrix(0,nrow=nz,ncol=nout);
  for(it in 1:nout){
    for(iz in 1:nz){
       u[iz,it]=out[it,iz+1];
     \text{uex}[iz, it] = \text{step}(z[iz], \text{tout}[it], vz);}
  u[1, it] = ue;}
#
# Display numerical solution
  iv=seq(from=1,to=nout,by=2);
  for(it in iv){
    cat(sprint(f''\n t z z-v*t u(z,t) uex(z,t)\n^n));iv=seq(from=1,to=nz,by=10);
    for(iz in iv){
      lam=z[iz]-vz*tout[it];
      cat(sprintf("%6.2f%6.2f%8.2f%12.3e%12.3e\n",
           tout[it],z[iz],lam,u[iz,it],uex[iz,it]));
    }
  }
#
# Calls to ODE routine
  cat(sprintf("\n\n ncall = \delta5d\n\n",ncall));
#
# Plot PDE solution
#
# u
  par(mfrow=c(1,1));matplot(x=z[2:nz],y=u[2:nz,],type="l",xlab="z",
          ylab="u(z,t)",xlim=c(zl,zu),lty=1,main="",lwd=2,
          col="black");
  matpoints(x=z[2:nz],u[2:nz,],pch="n",lty=1,lwd=2,
            col="black");
#
# uex
  matpoints(x=z[2:nz],uex[2:nz,],type="l",lty=1,lwd=2,
            col="black");
  matpoints(x=z[2:nz],uex[2:nz],pch="x",lty=1,lwd=2,col="black");
```
Listing A.1: Main program for eqs. (A.1-1,2,3), first-order hyperbolic

The following details about Listing A.1 can be noted.

• Previous workspaces are deleted.

```
#
# First order hyperbolic PDE
# (advection equation)
#
# Delete previous workspaces
 rm(list=ls(all=TRUE))
```
• The R ODE integrator library deSolve is accessed [6].

```
#
# Access ODE integrator
  library("deSolve");
#
# Access functions for numerical solution
 setwd("f:/Covid-19 neurological effects/appA");
  source("pde1a.R");
  source("step.R");
```
Then the directory with the files for the solution of eqs. (A.1-1,2,3) is designated. Note that setwd (set working directory) uses / rather than the usual  $\backslash$ .

The ODE/MOL routine pde1a is discussed subsequently. step is the exact (analytical) solution to eq. (A.1-1) with eqs. (A.1-2,3) specified as a Heaviside step function,  $u(z,t) = h(z - v_z t)$ .

• An index for a case, with ncase=1, 2, is specified. This index is used in the ODE/MOL routine pde1a considered subsequently.

```
#
# Set case
  ncase=1;
```
• The parameters of eqs.  $(A.1-1,2,3)$  are specified

```
#
# Parameters
 nz=101;
  vz=1;
  ue=1;
```
where

- − nz: number of points in the spatial grid in *z*.
- − vz: velocity *v<sup>z</sup>* in eq. (A.1-1).
- $-$  ue: boundary value  $u(z = z_l = 0, t) = g(t) = u_e$  (according to BC)  $(A.1-3)$ .
- A spatial grid for eq.  $(A.1-1)$  is defined with nz=101 points so that z =  $0,1/100=0.01,\ldots,1.$

```
#
# Spatial grid in z
  z1=0; zu=1; dz=(zu-z1)/(nz-1);z=seq(from=zl,to=zu,by=dz);
```
The grid spacing is  $dz = \Delta z$ .

• The interval in *t* is defined with nout=5 output points.

```
#
# Independent variable for ODE integration
  t0=0; t f=1; nout=5;tout=seq(from=t0,to=tf,by=(tf-t0)/(nout-1))
```
• IC (A.1-2) is implemented, with  $u_{z,t=0} = f(z) = 0$ .

```
#
# Initial condition (t=0)
  u0=rep(0,nz);ncall=0;
```
Also, the counter for the calls to pde1a is initialized.

• The system of nz=101 ODEs is integrated by the library integrator 1 sodes (available in deSolve, [6]). As expected, the inputs to lsodes are the ODE function, pde1a, the IC vector u0, and the vector of output values of *t*, tout. The length of u0 (101) informs lsodes how many ODEs are to be integrated. func,y,times are reserved names.

```
#
# ODE integration
  out=lsodes(y=u0,times=tout,func=pde1a,
      sparsetype="sparseint",rtol=1e-6,
      atol=1e-6,maxord=5);
  nrow(out)
 ncol(out)
```
nrow,ncol confirm the dimensions of out.

•  $u(z,t)$  and the exact solution  $h(z-v_zt)$  are placed in matrices for subsequent plotting.

```
#
# Arrays for plotting numerical, exact solutions
```

```
u=matrix(0,nrow=nz,ncol=nout);
uex=matrix(0,nrow=nz,ncol=nout);
for(it in 1:nout){
  for(iz in 1:nz){
     u[iz, it] = out[it, iz+1];uex[iz, it] = step(z[iz], tout[it], vz);}
u[1, it] = ue;}
```
Function step for the exact (analytical) solution to eq. (A.1-1), listed next, follows from eq. (A.7-6) and the discussion after eq. (A.1-3) pertaining to  $\lambda = z - v_z t$  (with  $h(\lambda = 0) = 0.5$ ).

```
step=function(z,t,vz){
#
# Function step computes the exact (analytical)
# for the linear advection equation with step BC
#
# lambda = z-vz*t
  lam=z-vz*t
#
# Step function
  if(lam<0){step=1;}
  if(lam==0){step=0.5;}
  if(lam>0){step=0;}
#
# Return function
  return(c(step));
  }
```
Listing A.2:  $h(z - v_z t)$  for eqs. (A.1)

c is the vector operator in R, i.e., step is returned as a vector to the main program of Listing A.1.

The numerical values of  $u(z,t)$  returned by 1 sodes and the exact solution are displayed. Every second value in *t* and every tenth value in *z* appear from  $by=2,10$ .

```
#
# Display numerical solution
 iv=seq(from=1,to=nout,by=2);
 for(it in iv){
   cat(sprintf("\n t z z-v*t u(z,t) uex(z,t)\n"));
   iv=seq(from=1,to=nz,by=10);
   for(iz in iv){
```

```
lam=z[iz]-vz*tout[it];
    cat(sprintf("%6.2f%6.2f%8.2f%12.3e%12.3e\n",
         tout[it],z[iz],lam,u[iz,it],uex[iz,it]));
 }
}
```
• The number of calls to pde1a is displayed at the end of the solution.

```
#
# Calls to ODE routine
  cat(sprintf("\n\n ncall = \delta5d\n\n",ncall));
```
• The numerical solution is plotted as lines and superimposed points with the letter n.

```
#
# Plot PDE solution
#
# u
  par(mfrow=c(1,1));matplot(x=z[2:nz],y=u[2:nz,],type="l",xlab="z",
          ylab="u(z,t)",xlim=c(zl,zu),lty=1,main="",lwd=2,
          col="black");
 matpoints(x=z[2:nz],u[2:nz],pch="n",lty=1,lwd=2,col="black");
```
The exact solution is plotted as lines and superimposed points with the letter x.

```
#
# uex
  matpoints(x=z[2:nz],uex[2:nz,],type="1",lty=1,lwd=2,col="black");
  matpoints(x=z[2:nz],uex[2:nz,],pch="x",lty=1,lwd=2,
            col="black");
```
The discontinuity at  $z = z_l$  of eqs (A.7-5,6) is not plotted ([2:nz,]) to improve the appearance of the plots.

This completes the discussion of the main program of Listing A.1. The ODE/MOL routine, pde1a, called by lsodes in the main program is considered next.

```
pde1a=function(t,u,parm){
#
# Function pde1a computes the t derivative
# of u(z,t)
```

```
#
# BC, z=zl
 u[1] = ue;#
# PDE
 ut=rep(0,nz);if(ncase==1){
    for(iz in 1:nz){
      if(iz==1){ut[iz]=0;}
      if(iz>1){
        ut[iz] = -vz*(u[iz] - u[iz-1])/dz;}
  }
  if(ncase==2){
    for(iz in 1:(nz-1)){
      if(iz==1){ut[iz]=0;}
      if(iz>1){
         ut[iz] = -vz*(u[iz+1]-u[iz-1])/(2*dz);}
         ut[nz]=-vz*(3*u[nz]-4*u[nz-1]+u[nz-2])/(2*dz);
  }
#
# Increment calls to pde1a
  ncall <<- ncall+1;
#
# Return derivative vector
  return(list(c(ut)));
  }
```
Listing A.3: ODE/MOL routine pde1a for eq. (A.1)

The following details about Listing A.3 can be noted.

The function is defined.

```
pde1a=function(t,u,parm){
#
# Function pde1a computes the t derivative
# of u1(z,t)
```
t is the current value of *t* in eqs. (A.1). u is the 101-vector of ODE/PDEdependent variables. parm is an argument to pass parameters to pde1a (unused, but required in the argument list). The arguments must be listed in the order stated to properly interface with lsodes called in the main program of Listing A.1. The derivative vector of the LHS of eq. (A.1-1) is calculated and returned to lsodes as explained subsequently.

```
• BC (A.1-3) is programmed (with f(z) = ue).
   #
```

```
# BC, z=zl
  u[1] = ue;
```
• Equation (A.1-1) is programmed for ncase=1.

```
#
# PDE
  ut=rep(0,nz);if(ncase==1){
    for(iz in 1:nz){
      if(iz==1){ut[iz]=0;}
      if(iz>1){
        ut[iz] = -vz * (u[iz] - u[iz-1])/dz;}
  }
```
∂*u* The derivative  $\frac{\partial x}{\partial \overline{z}}$  in eq. (A.1-1) is approximated with a two point upwind finite difference (FD) as in eqs. (A.7).

For  $z = z_l$ , BC (A.1-3) sets the value of  $u(z = z_l, t)$  and therefore the derivative is set to zero  $(if(iz=1)u1t[iz]=0;)$  to ensure the boundary value is maintained.

The correspondence of the programming with eqs. (A.7) is an important feature of the MOL. The principal disadvantage of the two point upwind FD, numerical diffusion which is an error (artifact) in the numerical solution, is demonstrated by the graphical output in Figure A.1-1 produced from the main program of Listing A.1 (discussed next).

• Equation (A.1-1) is programmed for ncase=2.

```
if(ncase==2){
  for(iz in 1:(nz-1)){
    if(iz==1){ut[iz]=0;}
    if(iz>1){
       ut[iz] = -vz*(u[iz+1]-u[iz-1])/(2*dz);}
       ut[nz]=-vz*(3*u[nz]-4*u[nz-1]+u[nz-2])/(2*dz);
}
```
∂*u* The derivative  $\frac{\partial z}{\partial \zeta}$  in eq. (A.1-1) is approximated with a two point centered  $\zeta$  *i* finite difference (FD).

$$
\frac{\partial u}{\partial z} \approx \frac{u(z + \Delta, t) - u(z - \Delta z, t)}{2\Delta z} + O(\Delta z^2)
$$
 (A.8-1)

 $O(\Delta z^2)$  indicates that the truncation error of the FD approximation of eq. (A.8-1) is second order in ∆*z*.

Substitution of approximation (A.8-1) in eq. (A.1-1) gives

$$
\frac{\partial u(z,t)}{\partial t} = -v_z \frac{u(z + \Delta z, t) - u(z - \Delta z, t)}{2\Delta z}
$$
 (A.8-2)

or in terms of the index i on the spatial grid in *z*,

$$
\frac{du_i}{dt} = -v_z \frac{u_{i+1} - u_{i-1}}{2\Delta z}; i = 1, 2, ..., n_z
$$
 (A.8-3)

For the right boundary ( $z = z_u = 1$ ), FD (A.8-1) introduces a fictitious value  $u(z<sub>u</sub> + \Delta z, t)$ . To circumvent this problem, a three point concentred FD ap- $\partial u(z_u,t)$ proximation for  $\frac{\partial u(x_i, y_i)}{\partial z}$  is used.

$$
\frac{\partial u(z_u, t)}{\partial z} \approx \frac{3u(z_u, t) - 4u(z_u - \Delta z, t) + u(z_u - 2\Delta z, t)}{2\Delta z} + O(\Delta z^2) \quad (A.8-4)
$$

The centered FD approximation of eq. (A.8-1) introduces a second form of error, numerical oscillation, as demonstrated by the graphical output in Figure A.1-2 discussed subsequently.

• The counter for the calls to pde1a is incremented and returned to the main program of Listing A.1 by <<-.

```
#
# Increment calls to pde1a
 ncall <<- ncall+1;
```
• The vector ut is returned as a list as required by lsodes. c is the R vector utility. The final } concludes pde1a.

```
#
# Return derivative vector
  return(list(c(ut)));
  }
```
The numerical output from the routines of Listings A.1, A.2, A.3 follows. For ncase=1 the numerical output is in Table A.1.

[1] 5

[1] 102





ncall = 307

Table A.1: Numerical output from Listings A.1, A.2, A.3, ncase=1 eqs. (A.7)

The following details about this output can be noted.

- 5 *t* output points as the first dimension of the solution matrix out from lsodes as programmed in the main program of Listing A.1 (with nout=5).
- The solution matrix out returned by lsodes has 102 elements as a second dimension. The first element is the value of *t*. Elements 2 to 102 are  $u(z,t)$ from eqs. (A.7) (for each of the 101 output points).
- The solution is displayed for  $t=0, 1/4=0.25,..., 1$  as programmed in Listing A.1 (every second value of *t* is displayed as explained previously).
- The solution is displayed for  $z=0,1/100=0.01,\ldots,1$  as programmed in Listing A.1 (every tenth value of *z* is displayed as explained previously).
- IC (A.7-5) is confirmed ( $t = 0$ ). Note in particular the IC at  $z v_z t = 0$ .
- The BC  $u(z=0,t) = u_e = 1$  as programmed in Listing A.3 is confirmed.
- The computational effort as indicated by ncall = 307 is modest so that lsodes computed the solution to eqs. (A.7) efficiently.

The graphical output is in Figures A.1-1.

Comparison of the numerical solution  $u(z,t)$  (plotted with *n*) and exact solution *h*(*z* − *v*<sub>*z*</sub>*t*) (plotted with *x*) indicates the numerical diffusion of the two point upwind ∂*u* FD approximation of the spatial derivative  $\frac{\partial}{\partial z}$ . Generally, the two solutions (numerical and exact) are fronts moving left to right (as expected with  $v_z > 0$ ).

For ncase=2, the numerical output is in Table A.2.

[1] 5

[1] 102





 $ncall = 550$ 

Table A.2: Numerical output from Listings A.1, A.2, A.3, ncase=2, eqs. (A.8)

The following details about this output can be noted (some of the discussion for ncase=1 is repeated to provide a self contained explanation)

- 5 *t* output points as the first dimension of the solution matrix out from lsodes as programmed in the main program of Listing A.1 (with nout=5).
- The solution matrix out returned by 1 sodes has 102 elements as a second dimension. The first element is the value of *t*. Elements 2 to 102 are  $u(z,t)$ from eqs. (A.8) (for each of the 101 output points).
- The solution is displayed for  $t=0, 1/4=0.25,...,1$  as programmed in Listing A.1 (every second value of *t* is displayed as explained previously).
- The solution is displayed for  $z=0,1/100=0.01,\ldots,1$  as programmed in Listing A.1 (every tenth value of *z* is displayed as explained previously).
- IC (A.7-5) is confirmed ( $t = 0$ ). Note, in particular, the IC at  $z v_z t = 0$ .
- The BC  $u(z=0,t) = u_e = 1$  as programmed in Listing A.3 is confirmed.
- The computational effort as indicated by  $ncall = 550$  is modest so that lsodes computed the solution to eqs. (A.8) efficiently.

The graphical output is in Figures A.1-2. Comparison of the numerical solution  $u(z,t)$  (plotted with *n*) and exact solution  $h(z - v_z t)$  (plotted with *x*) indicates the numerical oscillation of the two point centered FD approximation of the spatial deriva- ∂*u* tive  $\frac{\partial u}{\partial z}$ . (the numerical oscillation invalidates the numerical solution). Generally, centered FD approximations should not be applied to hyperbolic (strongly convective) PDEs.

An improvement in the numerical integration of the advection equation, eq. (A.1-1) (reduced numerical diffusion, elimination of numerical oscillation), can be ∂*u* achieved by using flux limiter approximations for the derivative  $\frac{\partial u}{\partial z}$  ([5], pp. 37–43).



**Figure A.1-1**  $u(z,t)$  from eqs. (A.7)



**Figure A.1-2**  $u(z,t)$  from eqs. (A.8)

# **A.3.2 FLUX LIMITERS**

. .

Consideration is now given to two flux limiters: van leer and smart. Small extensions to the main program of Listing A.1 are added, i.e., (1) files for the two flux limiters are specified and (2) an index, ncase=1,2, is added and displayed for the limiters.

```
.
#
# Access functions for numerical solution
  setwd("f:/Covid-19 neurological effects/appA");
  source("pde1b.R");
  source("vanl.R");
  source("smart.R");
 source("step.R");
#
# Specify case
 ncase=1;
         .
         .
         .
#
# Display numerical solution
  iv=seq(from=1,to=nout,by=2);
   cat(sprint('\\n ncase = %2d"));
 for(it in iv){
    cat(sprint(f' \n t z z-v*t u(z,t) uex(z,t)\n^n));iv=seq(from=1,to=nz,by=5);
    for(iz in iv){
      lam=z[iz]-vz*tout[it];
      cat(sprintf("%6.2f%6.2f%8.2f%12.3e%12.3e\n",
           tout[it],z[iz],lam,u[iz,it],uex[iz,it]));
   }
 }
         .
         .
         .
```

```
Listing A.4: Additions to the main program of Listing A.1 for eqs. (A.1-1,2,3)
  ncase is used in the ODE/MOL routine, pde1b, to call a particular flux limiter.
  pde1b=function(t,u,parm){
#
# Function pde1b computes the t derivative
```

```
# of u(z,t)#
# BC, z=zl
  u[1] = ue;#
# PDE
  if(ncase==1){uz= van1(z1,zu,nz,u,vz)};if(ncase==2){uz=smart(z1,zu,nz,u,vz)};ut=rep(0,nz);for(iz in 1:nz){
    if(iz==1){ut[iz]=0;}
    if(iz>1){
      ut[iz] = -vz * uz[iz];}
#
# Increment calls to pde1b
 ncall <<- ncall+1;
#
# Return derivative vector
  return(list(c(ut)));
  }
```
Listing A.5: ODE/MOL routine pde1b for eqs. (A.1-1,2,3)

The following details about Listing A.5 can be noted. (with some repetition of the discussion of Listing A.3).

The function is defined.

```
pde1b=function(t,u,parm){
#
# Function pde1b computes the t derivative
# of u1(z,t)
```
t is the current value of *t* in eqs. (A.1). u is the 101-vector of ODE/PDE dependent variables. parm is an argument to pass parameters to pde1b (unused, but required in the argument list). The arguments must be listed in the order stated to properly interface with lsodes called in the main program of Listing A.1. The derivative vector of the LHS of eq. (A.1-1) is calculated and returned to lsodes as explained subsequently.

```
• BC (A.1-3) is programmed (with f(z) = ue).
```

```
#
# BC, z=zl
  u[1] = ue;
```
Equation  $(A.1-1)$  is programmed for  $ncase=1,2$ .

```
#
# PDE
  if(ncase==1){uz= vanl(z1,zu,nz,u,vz)};if(ncase==2){uz=smart(zl,zu,nz,u,vz);}
  ut=rep(0,nz);for(iz in 1:nz){
    if(iz==1){ut[iz]=0;}
    if(iz>1){
      ut[iz]=-vz*uz[iz];}
```
∂*u* The derivative  $\frac{\partial u}{\partial z}$  in eq. (A.1-1) is approximated with a flux limiter selected by ncase. The code (programming) in functions vanl, smart is discussed subsequently.

For  $z = z_l$ , BC (A.1-3) sets the value of  $u(z = z_l, t)$  and therefore the derivative is set to zero  $(if(iz=1)u1t[iz]=0;)$  to ensure the boundary value is maintained.

• The counter for the calls to pde1b is incremented and returned to the main program of Listing A.1 by  $<<$ -.

```
#
# Increment calls to pde1b
  ncall <<- ncall+1;
```
• The vector ut is returned as a list as required by lsodes. c is the R vector utility. The final  $\}$  concludes pde1b.

```
#
# Return derivative vector
  return(list(c(ut)));
  }
```
Function vanl for the van Leer flux limiter is listed next

```
vanl=function(zl,zu,n,u,v) {
#
# Function vanl computes the van Leer flux limiter
# approximation of a first derivative
#
# Declare arrays
 uz=rep(0,n);phi=rep(0,n);
  r=rep(0,n);#
```

```
# Grid spacing
 dz=(zu-z1)/(n-1);#
# Tolerance for limiter switching
 delta=1.0e-05;
#
# Positive v
  if(v \ge 0){
    for(i in 3:(n-1)){
     if(abs(u[i]-u[i-1])<delta)phi[i]=0
      else{
        r[i]=(u[i+1]-u[i])/(u[i]-u[i-1])if(r[i]<0)
          phi[i]=0
        else
        phi[i]=max(0,min(2*r[i],min(0.5*(1.0+r[i]),2)))}
      if(abs(u[i-1]-u[i-2]) <delta)
        phi[i-1]=0else{
        r[i-1]=(u[i]-u[i-1])/(u[i-1]-u[i-2])if(r[i-1]<0)
          phi[i-1]=0else
          phi[i-1]=max(0,min(2*r[i-1],min(0.5*(1.0+r[i-1]),2)))}
      flux2=u[i ]+(u[i ]-u[i-1])*phi[i ]/2;
      flux1=u[i-1]+(u[i-1]-u[i-2])*phi[i-1]/2;
      uz[i] = (flux2-flux1)/dz;}
      uz[1] = (-u[1]+u[2])/dz;uz[2] = (-u[1]+u[2])/dz;uz[n]=(u[n]-u[n-1])/dz;}
#
# Negative v
  if(v < 0){
    for(i in 2:(n-2)){
     if(abs(u[i]-u[i+1])<delta)
        phi[i]=0
      else{
        r[i]=(u[i-1]-u[i])/(u[i]-u[i+1])if(r[i]<0)
          phi[i]=0
        else
```

```
phi[i]=max(0,min(2*r[i],min(0.5*(1.0+r[i]),2)))}
      if(abs(u[i+1]-u[i+2])<delta)
        phi[i+1]=0else{
        r[i+1]=(u[i]-u[i+1])/(u[i+1]-u[i+2])if(r[i+1]<0)
          phi[i+1]=0else
          phi[i+1]=max(0,min(2*r[i+1],min(0.5*(1.0+r[i+1]),2)))}
      flux2=u[i ]+(u[i ]-u[i+1])*phi[i ]/2;
      flux1=u[i+1]+(u[i+1]-u[i+2])*phi[i+1]/2;
      uz[i] = -(flux2-flux1)/dz;}
      uz[1] = (-u[1]+u[2])/dz;uz[n-1] = (-u[n-1]+u[n])/dz;uz[n] = (-u[n-1]+u[n])/dz;}
#
# All points concluded (z=zl,...,z=zu)
 return(c(uz));
}
```
Listing A.6: Function vanl

The following details about vanl can be noted.

The function is defined.

```
vanl=function(zl,zu,n,u,v) {
#
# Function vanl computes the van Leer flux limiter
# approximation of a first derivative
```
zl,zu are the lower and upper boundary values of the spatial grid in *z*. n is the number of grid points in *z*. u is the vector of PDE-dependent variable values to be differentiated numerically. v is the convective velocity (only the sign is used to determine the direction of the convection).

• Arrays (vectors) are declared for subsequent use.

```
#
# Declare arrays
 uz=rep(0,n);phi=rep(0,n);
  r=rep(0,n);
```
• The grid spacing is calculated.

```
#
# Grid spacing
  dz=(zu-z1)/(n-1);
```
• The tolerance (threshold) for switching between sections of the flux limiter is specified.

```
#
# Tolerance for limiter switching
  delta=1.0e-05;
```
delta can be varied to determine the sensitivity of the solution to its value.

• For positive velocity (in eq.  $(A.1-1)$ ), the limiting function phi is calculated.

```
#
# Positive v
  if(y >= 0)for(i in 3:(n-1)){
     if(abs(u[i]-u[i-1])<delta)
        phi[i]=0else{
        r[i]=(u[i+1]-u[i])/(u[i]-u[i-1])
        if(r[i]<0)
          phi[i]=0
        else
        phi[i]=max(0,min(2*r[i],min(0.5*(1.0+r[i]),2)))}
      if(abs(u[i-1]-u[i-2])<del>del</del>ta)phi[i-1]=0else{
        r[i-1]=(u[i]-u[i-1])/(u[i-1]-u[i-2])if(r[i-1]<0)
          phi[i-1]=0else
          phi[i-1] = max(0, min(2*r[i-1],min(0.5*(1.0+r[i-1]),2)))flux2=u[i ]+(u[i ]-u[i-1])*phi[i ]/2;
      flux1=u[i-1]+(u[i-1]-u[i-2]) *phi[i-1]/2;uz[i]=(flux2-flux1)/dz;}
```
phi is a nonlinear function of  $u[i+1], u[i], u[i-1], u[i-2]$  (the two point upwind and centered FDs considered previously are linear in  $u(z,t)$ ). max,min are utilities in the basic R.

At the end, the limiting function phi is used to calculate the fluxes flux1,flux2 and derivative in *z*, uz, for grid points  $3:(n-1)$ . Mathematical and graphical details for the limiting function are available in [5], pp. 41–43.

• The derivative in  $z$  is computed for the boundary points  $1, 2, n$ .

```
uz[1] = (-u[1]+u[2])/dz;uz[2]=(-u[1]+u[2])/dz;
uz[n]=(u[n]-u[n-1])/dz;
```
This completes the calculation of the  $\frac{\partial u}{\partial z}$  approximation for v>0.

The code for  $v < 0$  is similar with the values  $u[i-1], u[i-2]$  replaced by u[i+1],u[i+2].

The performance of the van Leer limiter is demonstrated by execution of the R routines in Listings A.1-5 with ncase=1. The numerical output is given in Table A.3.

[1] 5

[1] 102

```
ncase = 1
```
}





 $ncall = 4919$ 

Table A.3: Numerical output from Listings A.1-5, ncase=1, van Leer limiter

The following details about Table A.3 can be noted.

- The dimensions of the solution matrix out returned by 1 sodes in the main program of Listing A.1 are again  $5 \times 102$  as explained previously for Tables A.1, A.2.
- The case is confirmed (as set in the main program of Listing A.1).

 $ncase = 1$ 

- The solution is displayed for  $z=0,1/100=0.01,\ldots,1$  as programmed in Listing A.1 (every tenth value of *z* is displayed as explained previously).
- IC (A.7-5) is confirmed ( $t = 0$ ). Note, in particular, the IC at  $z v_z t = 0$ .
- The BC  $u(z=0,t) = u_e = 1$  as programmed in Listing A.5 is confirmed.
- The computational effort as indicated by  $ncall = 4919$  is higher than for the FD output of Tables A.1, A.2 due to the computations in the van Leer limiter of Listing A.6.

The graphical output is in Figure A.2-1. Comparison of the numerical solution  $u(z,t)$ (plotted with *n*) and exact solution  $h(z - v_z t)$  (plotted with *x*) indicates small numerical diffusion and no numerical oscillation, i.e., a major improvement over the FD solutions in Figures A.1-1, A.1-2.

The exact solution  $h(z - v_z t)$  is impossible to reproduce numerically since for  $z$  $v_z t = 0$  the solution is undefined (infinite slope). With this in mind, the performance of the van Leer limiter is quite impressive.

Function smart for the smart flux limiter is listed next (ncase=2 in the main program of Listings A.1, A.4).



**Figure A.2-1**  $u(z,t)$  from eqs. (A.1), van Leer flux limiter

```
smart=function(zl,zu,n,u,v) {
#
# Function smart computes the smart flux limiter
# approximation of a first derivative
#
# Declare arrays
```

```
uz=rep(0,n);phi=rep(0,n);
    r=rep(0,n);#
# Grid spacing
 dz=(zu-z1)/(n-1);#
# Tolerance for limiter switching
 delta=1.0e-05;
#
# Positive v
  if(v \ge 0){
    for(i in 3:(n-1)){
     if(abs(u[i]-u[i-1])<delta)
        phi[i]=0
      else{
        r[i]=(u[i+1]-u[i])/(u[i]-u[i-1])phi[i]=max(0,min(4,0.75*r[i]+0.25,2*r[i]))}
      if(abs(u[i-1]-u[i-2]) <delta)
        phi[i-1]=0else{
        r[i-1]=(u[i]-u[i-1])/(u[i-1]-u[i-2])phi[i-1]=max(0,min(4,0.75*r[i-1]+0.25,2*r[i-1]))}
      flux2=u[i ]+(u[i ]-u[i-1])*phi[i ]/2
      flux1=u[i-1]+(u[i-1]-u[i-2])*phi[i-1]/2
      uz[i] = (flux2-flux1)/dz}
      uz[1] = (-u[1]+u[2])/dz;uz[2] = (-u[1]+u[2])/dz;uz[n]=(u[n]-u[n-1])/dz;}
#
# Negative v
 if(v < 0){
    for(i in 2:(n-2)){
     if(abs(u[i]-u[i+1])<delta)
        phi[i]=0
      else{
        r[i]=(u[i-1]-u[i])/(u[i]-u[i+1])phi[i]=max(0,min(4,0.75*r[i]+0.25,2*r[i]))}
      if(abs(u[i+1]-u[i+2])<delta)
        phi[i+1]=0
      else{
        r[i+1]=(u[i]-u[i+1])/(u[i+1]-u[i+2])
```

```
phi[i+1]=max(0,min(4,0.75*r[i+1]+0.25,2*r[i+1]))}
      flux2=u[i ]+(u[i ]-u[i+1])*phi[i ]/2
      flux1=u[i+1]+(u[i+1]-u[i+2])*phi[i+1]/2
      uz[i]=-(flux2-flux1)/dz
    }
      uz[1] = (-u[1]+u[2])/dz;uz[n-1] = (-u[n-1]+u[n])/dz;uz[n] = (-u[n-1]+u[n])/dz;}
#
# All points concluded (z=zl,...,z=zu)
 return(c(uz));}
```
## Listing A.7: Function smart

smart is the same as vanl in Listing A.6 except for the limiting function phi listed next (for v>0).

```
#
# Positive v
 if(v \ge 0){
    for(i in 3:(n-1)){
     if(abs(u[i]-u[i-1])<delta)
        phi[i]=0
      else{
        r[i]=(u[i+1]-u[i])/(u[i]-u[i-1])phi[i]=max(0,min(4,0.75*r[i]+0.25,2*r[i]))}
      if(abs(u[i-1]-u[i-2])<delta)
        phi[i-1]=0else{
        r[i-1]=(u[i]-u[i-1])/(u[i-1]-u[i-2])phi[i-1]=max(0,min(4,0.75*r[i-1]+0.25,2*r[i-1]))}
      flux2=u[i ]+(u[i ]-u[i-1])*phi[i ]/2
      flux1=u[i-1]+(u[i-1]-u[i-2])*phi[i-1]/2
      uz[i] = (flux2-flux1)/dz}
      uz[1]=(-u[1]+u[2])/dz;
      uz[2] = (-u[1]+u[2])/dz;uz[n]=(u[n]-u[n-1])/dz;}
```
The code for  $v < 0$  is similar with the values  $u[i-1]$ ,  $u[i-2]$  replaced by u[i+1],u[i+2]. Mathematical and graphical details for the limiting function are available in [5], pp. 41–43.

The performance of the smart limiter is demonstrated by execution of the R routines in Listings A.1-5 with ncase=2. The numerical output is given in Table A.4.

[1] 5

[1] 102

 $ncase = 2$ 



ncall = 3352

Table A.4: Numerical output from Listings A.1-5, ncase=2, smart limiter

The following details about Table A.4 can be noted (with some repetition of the discussion of Table A.3).

- The dimensions of the solution matrix out returned by 1 sodes in the main program of Listing A.1 are again  $5 \times 102$  as explained previously for Tables A.1, A.2, A.3
- The case is confirmed (as set in the main program of Listing A.1).

 $ncase = 2$ 

- The solution is displayed for  $z=0,1/100=0.01,\ldots,1$  as programmed in Listing A.1 (every tenth value of *z* is displayed as explained previously).
- IC (A.7-5) is confirmed ( $t = 0$ ). Note in particular the IC at  $z v_z t = 0$ .
- The BC  $u(z=0,t) = u_e = 1$  as programmed in Listing A.5 is confirmed.
- The computational effort as indicated by  $ncall = 3352$  (less than for the van Leer limiter).

The graphical output is in Figure A.2-2. Comparison of the numerical solution  $u(z,t)$ (plotted with *n*) and exact solution  $h(z - v_z t)$  (plotted with *x*) indicates small numerical diffusion and no numerical oscillation, i.e., a major improvement over the FD solutions in Figures A.1-1, A.1-2.

Again, the exact solution  $h(z - v_z t)$  is impossible to reproduce numerically since for  $z - v_z t = 0$  the solution is undefined (infinite slope). With this in mind, the performance of the smart limiter is quite impressive.

∂*u* This completes the discussion of the approximation of the derivative  $\frac{\partial u}{\partial z}$  in eq. (A.1-1) by FDs and flux limiters. Discussion follows next for the approximation of  $\partial^2 u$ the second derivative  $\frac{\partial^2 u}{\partial z^2}$  in eqs. (A.4-1), (A.6-1).

# **A.4 SECOND-ORDER SPATIAL DERIVATIVES**

From FD approximation (A.4-7),

$$
\frac{\partial u}{\partial t} \approx D \left( \frac{\frac{\partial u}{\partial z} |_{z + \Delta z} - \frac{\partial u}{\partial z} |_{z}}{\Delta z} \right)
$$
  
\n
$$
\approx D \left( \frac{u(z + \Delta z, t) - u(z, t)}{\Delta z} - \frac{u(z, t) - u(z - \Delta z, t)}{\Delta z} \right)
$$
  
\n
$$
= D \left( \frac{u(z + \Delta z, t) - 2u(z, t) + u(z - \Delta z, t)}{\Delta z^2} \right)
$$
 (A.9-1)


**Figure A.2-2**  $u(z,t)$  from eqs. (A.1), smart flux limiter

A FD approximation of the second derivative is therefore

$$
\frac{\partial^2 u}{\partial z^2} \approx \frac{u(z + \Delta z, t) - 2u(z, t) + u(z - \Delta z, t)}{\Delta z^2}) + O(\Delta z^2)
$$
 (A.9-2)

which is used in the following MOL analysis.

A main program for eqs. (A.4-1,2) and various BCs based on eqs. (A.9) follows.

```
#
# Second order parabolic PDE
# (diffusion equation)
#
# Delete previous workspaces
 rm(list=ls(all=TRUE))
#
# Access ODE integrator
  library("deSolve");
#
# Access functions for numerical solution
  setwd("f:/Covid-19 neurological effects/appA");
  source("pde1c.R");
#
# Specify case
  ncase=1;
#
# Parameters
 nz=21;
 D=0.1;km=0.1;
#
# Spatial grid in z
  zl=0;zu=1;dz=(zu-zl)/(nz-1);dzs=dz^2;
  z=seq(from=zl,to=zu,by=dz);
#
# Independent variable for ODE integration
 t0=0; tf=1; nout=11;tout=seq(from=t0,to=tf,by=(tf-t0)/(nout-1));
#
# Initial condition (t=0)
 u0=rep(0,nz);
  if(ncase==1){
    for(iz in 1:nz){
      u0[iz] = sin(pi/(zu-z1)*(z[iz]-z1));}
  if(ncase==2){
    for(iz in 1:nz){
      u0[iz]=cos(pi/(zu-zl)*(z[iz]-zl));}
  }
  if(ncase==3){
    for(iz in 1:nz){
      u0[iz]=1;}
```

```
}
 ncall=0;
#
# ODE integration
  out=lsodes(y=u0,times=tout,func=pde1c,
      sparsetype="sparseint",rtol=1e-6,
      atol=1e-6,maxord=5);
  nrow(out)
 ncol(out)
#
# Arrays for plotting numerical, exact solutions
    u=matrix(0,nrow=nz,ncol=nout);
  uex=matrix(0,nrow=nz,ncol=nout);
  if(ncase==1){
    for(it in 1:nout){
      for(iz in 1:nz){
         u[iz,it]=out[it,iz+1];
       uex[iz,it]=exp(-D*(pi/(zu-zl))^2*tout[it])*
                  sin(pi*(z[iz]-z1)/(zu-z1));}
      u[1,it]=0;
     u[nz, it] = 0;}
  }
  if(ncase==2){
    for(it in 1:nout){
      for(iz in 1:nz){
         u[iz,it]=out[it,iz+1];
       uex[iz,it]=exp(-D*(pi/(zu-zl))^2*tout[it])*
                  cos(pi*(z[iz]-z1)/(zu-z1));}
    }
  }
  if(ncase==3){
    for(it in 1:nout){
      for(iz in 1:nz){
         u[iz,it]=out[it,iz+1];
      }
    }
  }
#
# Display numerical solution
# ncase=1,2
  if(ncase<3){
```

```
iv=seq(from=1,to=nout,by=2);
     cat(sprint(f' \n' \nncase = %2d\n' \n' \n, ncase));for(it in iv){
      cat(sprintf("\n t z u(z,t) uex(z,t) error\n"));
      iv=seq(from=1,to=nz,by=10);
      for(iz in iv){
        err=u[iz,it]-uex[iz,it];
        cat(sprintf("%6.2f%6.2f%12.3e%12.3e%12.3e\n",
          tout[it],z[iz],u[iz,it],uex[iz,it],err));
      }
    }
  }
#
# ncase=3
  if(ncase==3){
    iv=seq(from=1,to=nout,by=2);
     cat(sprint(f' \n) ncase = %2d\n);
    for(it in iv){
      cat(sprint(f' \n t z u(z,t) \n t);
      iv=seq(from=1,to=nz,by=5);
      for(iz in iv){
        cat(sprintf("%6.2f%6.2f%12.3e\n",
          \text{tout}[\text{it}],\text{z}[\text{iz}],\text{u}[\text{iz},\text{it}]\});
      }
    }
  }
#
# Calls to ODE routine
  cat(sprintf("\n\n ncall = \delta5d\n\n",ncall));
#
# Plot PDE solution
#
# u
  par(mfrow=c(1,1));
  matplot(x=z,y=u,type="l",xlab="z",ylab="u(z,t)",
          xlim=c(zl,zu),lty=1,main="",lwd=2,col="black");
  matpoints(x=z,y=u,pch="n",lty=1,lwd=2,col="black");
#
# uex
  if(ncase<3){
  matpoints(x=z,y=uex,pch="x",lty=1,lwd=2,col="black");
  matpoints(x=z,y=uex,type="l",lty=1,lwd=2,col="black");
  }
```

```
Listing A.8: Main program for eqs. (A.4-1,2), parabolic
```
The following details about Listing A.8 can be noted (with some repetition of the discussion of Listing A.1).

Previous workspaces are deleted.

```
#
# Second order parabolic PDE
# (diffusion equation)
#
# Delete previous workspaces
  rm(list=ls(all=TRUE))
```
• The R ODE integrator library deSolve is accessed [6].

```
#
# Access ODE integrator
 library("deSolve");
#
# Access functions for numerical solution
  setwd("f:/Covid-19 neurological effects/appA");
  source("pde1c.R");
```
Then the directory with the files for the solution of eqs. (A.4-1,2) is designated. Note that setwd (set working directory) uses / rather than the usual  $\backslash$ .

The ODE/MOL routine pde1c is discussed subsequently.

• An index for a case, with ncase=1,2,3, is specified. This index is used in the ODE/MOL routine pde1c considered subsequently.

```
#
# Specify case
  ncase=1;
```
• The parameters of eqs.  $(A.4-1,2)$ .

```
#
# Parameters
  nz=21;
  D=0.1;km=0.1;
```
where D, km are parameters in Robin BCs for ncase=3.

• A spatial grid for eq.  $(A.4-1)$  is defined with 21 points so that  $z =$  $0,1/20=0.05,\ldots,1.$ 

```
#
# Spatial grid in z
  z1=0; zu=1; dz=(zu-z1)/(nz-1); dzs=dz^2;z=seq(from=zl,to=zu,by=dz);
```

```
The grid spacing is dz = \Delta z.
```
• An interval in *t* is defined with nout=11 output points.

```
#
# Independent variable for ODE integration
  t0=0; t f=1; nout=11;tout=seq(from=t0,to=tf,by=(tf-t0)/(nout-1));
```
• IC  $(A.4-2)$  is implemented for ncase=1, 2, 3.

```
# Initial condition (t=0)
 u0=rep(0,nz);if(ncase==1){
    for(iz in 1:nz){
      u0[iz] = sin(pi/(zu-z1)*(z[iz]-z1));}
  if(ncase==2){
    for(iz in 1:nz){
      u0[iz] = cos(pi/(zu-z1)*(z[iz]-z1));}
  if(ncase==3){
    for(iz in 1:nz){
      u0[iz]=1;}
 ncall=0;
```
The three ICs are discussed subsequently. Also, the counter for the calls to pde1c is initialized.

• The system of nz=21 ODEs is integrated by the library integrator 1 sodes (available in deSolve, [6]). The inputs to lsodes are the ODE function, pde1c, the IC vector u0, and the vector of output values of *t*, tout. The length of  $u_0$  ( $nz = 21$ ) informs 1 sodes how many ODEs are to be integrated. func,y,times are reserved names.

```
#
# ODE integration
 out=lsodes(y=u0,times=tout,func=pde1c,
      sparsetype="sparseint",rtol=1e-6,
      atol=1e-6,maxord=5);
 nrow(out)
 ncol(out)
```
nrow,ncol confirm the dimensions of out.

•  $u(z,t)$  and the exact solution are placed in matrices for subsequent plotting.

```
#
# Arrays for plotting numerical, exact solutions
```

```
u=matrix(0,nrow=nz,ncol=nout);
uex=matrix(0,nrow=nz,ncol=nout);
if(ncase==1){
  for(it in 1:nout){
    for(iz in 1:nz){
       u[iz, it] = out[it, iz+1];uex[iz,it]=exp(-D*(pi/(zu-zl))^2*tout[it])*
                sin(pi*(z[iz]-z1)/(zu-z1));}
    u[1, it] = 0;u[nz, it]=0;}
}
if(ncase==2){
  for(it in 1:nout){
    for(iz \in 1:nz)u[iz,it]=out[it,iz+1];
     uex[iz, it] = exp(-D*(pi/(zu-z1))^2*tvout[it])*cos(pi*(z[iz]-z1)/(zu-z1));}
  }
}
if(ncase==3){
  for(it in 1:nout){
    for(iz in 1:nz){
       u[iz,it]=out[it,iz+1];
    }
 }
}
```
An exact (analytical) solution is included for ncase=1,2, and not for ncase=3, as discussed subsequently.

• The numerical and exact solutions are displayed for ncase=1,2.

```
#
# Display numerical solution
# ncase=1,2
  if(ncase<3){
    iv=seq(from=1,to=nout,by=2);
     cat(sprint(f' \n) ncase = %2d\n'n', ncase);
    for(it in iv){
      cat(sprint(f' \n t z u(z,t) uex(z,t) error\nu'));iv=seq(from=1,to=nz,by=5);
      for(iz in iv){
        err=u[iz,it]-uex[iz,it];
```

```
cat(sprintf("%6.2f%6.2f%12.3e%12.3e%12.3e\n",
        tout[it],z[iz],u[iz,it],uex[iz,it],err));
    }
 }
}
```
Every second value of *t* and every fifth value of *z* is selected with by=2,5. The numerical solution is displayed for ncase=3.

```
#
# ncase=3
  if(ncase==3){
    iv=seq(from=1,to=nout,by=2);
     cat(sprintf("\n ncase = \frac{2}{d});
    for(it in iv){
       cat(sprint(f''\n t z u(z,t)\n^n));iv=seq(from=1,to=nz,by=5);
       for(iz in iv){
         cat(sprintf("%6.2f%6.2f%12.3e\n",
           \text{tout}[\text{it}],\text{z}[\text{iz}],\text{u}[\text{iz},\text{it}]),}
    }
  }
```
• The number of calls to pde1c at the end of the solutions is displayed.

```
#
# Calls to ODE routine
  cat(sprintf("\n\n ncall = \delta5d\n\n",ncall));
```
• The numerical solution is plotted with lines and points superimposed as n.

```
#
# Plot PDE solution
#
# u
 par(mfrow=c(1,1));matplot(x=z,y=u,type="l",xlab="z",ylab="u(z,t)",
          xlim=c(zl,zu),lty=1,main="",lwd=2,col="black");
 matpoints(x=z,y=u,pch="n",lty=1,lwd=2,col="black");
```
• The exact solutions for ncase=1, 2 are plotted with lines and points superimposed as x.

```
#
# uex
```

```
if(ncase<3){
matpoints(x=z,y=uex,pch="x",lty=1,lwd=2,col="black");
matpoints(x=z,y=uex,type="l",lty=1,lwd=2,col="black");
}
```
This completes the discussion of the main program. The ODE/MOL routine pde1c is discussed next.

```
pde1c=function(t,u,parm){
#
# Function pde1c computes the t derivative
# of u(z,t)#
# BCs
  if(ncase==1){
    u[1]=0;u[nz]=0;#
# PDE
 ut=rep(0,nz);if(ncase==1){
    for(iz in 2:(nz-1)){
      ut[iz]=D*(u[iz+1]-2*u[iz]+u[iz-1])/dzs;
    }
    ut[1]=0;ut[nz]=0;}
  if(ncase==2){
    for(iz \in 1:nz)if(iz==1)um=u[2];
        ut[1]=D*(u[2]-2*u[1]+um)/dzs;}
      if(iz=nz)up=u[nz-1];
        ut[nz]=D*(up-2*u[nz]+u[nz-1])/dzs;}
      if((iz>1)&(iz<nz)){
        ut[iz] = D * (u[iz+1]-2 * u[iz]+u[iz-1])/dzs;}
  }
  if(ncase==3){
    for(iz in 1:nz){
      if(iz==1){
         um=u[2]-(km/D)*(2*dz)*u[1];
        ut[1]=D*(u[2]-2*u[1]+um)/dzs;}
      if(iz==nz){
```

```
up=u[nz-1] - (km/D) * (2*dz) * u[nz];
        ut[nz]=D*(up-2*u[nz]+u[nz-1])/dzs;}
      if((iz>1)&(iz<nz)){
        ut[iz]=D*(u[iz+1]-2*u[iz]+u[iz-1])/dzs;}
    }
  }
#
# Increment calls to pde1c
 ncall <<- ncall+1;
#
# Return derivative vector
  return(list(c(ut)));
  }
```

```
Listing A.9: ODE/MOL routine pde1c for eqs. (A.4-1,3,4)
```
The following details about Listing A.9 can be noted.

The function is defined.

```
pde1c=function(t,u,parm){
#
# Function pde1c computes the t derivative
# of u(z,t)
```
t is the current value of *t* in eq. (A.4-1). u is the 21-vector of ODE/PDEdependent variables. parm is an argument to pass parameters to pde1c (unused, but required in the argument list). The arguments must be listed in the order stated to properly interface with lsodes called in the main program of Listing A.8. The derivative vector of the LHS of eq. (A.4-1) is calculated and returned to lsodes as explained subsequently.

• For ncase=1, homogeneous Dirichlet BCs are specified.

$$
u(z = z_l, t) = u(z = z_u, t) = 0
$$
 (A.9-3)

Equation (A.4-1) is programmed for ncase=1.

```
#
# PDE
 ut=rep(0,nz);if(ncase==1){
    for(iz in 2:(nz-1)){
      ut[iz]=D*(u[iz+1]-2*u[iz]+u[iz-1])/dzs;
    }
    ut[1]=0;ut[nz]=0;}
```
 $\partial^2 u$ The derivative  $\frac{\partial z}{\partial z^2}$  in eq. (A.4-1) is approximated with the three-point centered finite difference (FD) of eq. (A.9-2). For  $z = z_l, z_u$ , the BCs set the values of  $u(z = z_l, t)$ ,  $u(z = z_u, t)$  and therefore the derivatives are set to zero to ensure the boundary values are maintained.

The MOL ODEs are defined at the interior grid poins in *z*,

if((iz>1)}&(iz<nz))

according to eq. (A.9-1).

• Equation (A.4-1) is programmed for ncase=2.

```
if(ncase==2){
  for(iz in 1:nz){
    if(iz==1){
      um=u[2];
      ut[1] = D * (u[2]-2*u[1]+um)/dzs;if(iz==nz){
      up=u[nz-1];
      ut[nz]=D*(up-2*u[nz]+u[nz-1])/dzs;}
    if((iz>1)&(iz<nz)){
      ut[iz]=D*(u[iz+1]-2*u[iz]+u[iz-1])/dzs;}
  }
}
```
For a homogeneous Neumann BC at  $z = z_l$ ,

$$
\frac{\partial u(z=z_l,t)}{\partial z}=0
$$

the FD approximation is  $(iz=1)$ 

$$
\frac{\partial u(z_l,t)}{\partial z} \approx \frac{u(z_l + \Delta z,t) - u(z_l - \Delta z,t)}{2\Delta z} = 0
$$

or  $u(z_l - \Delta z, t) = u(z_l + \Delta z, t)$ .  $u(z_l - \Delta z, t)$  is an exterior (fictitious) value outside the grid in  $z$  (um in the preceding code).

Similarly, for a homogeneous Neumann BC at  $z = z_u$ ,

$$
\frac{\partial u(z=z_u,t)}{\partial z}=0
$$

the FD approximation is (iz=nz)

$$
\frac{\partial u(z_u,t)}{\partial z} \approx \frac{u(z_u + \Delta z,t) - u(z_u - \Delta z,t)}{2\Delta z} = 0
$$

or  $u(z_u + \Delta z,t) = u(z_u - \Delta z,t)$ .  $u(z_u + \Delta z,t)$  is an exterior value outside the grid in *z* (up in the preceding code).

An extension of the homogeneous Neumann BCs can be considered as nonhomogeneous (inhomogeneous, time varying) BCs. For example,

$$
\frac{\partial u(z=z_l,t)}{\partial z} = g_{nl}(t) \tag{A.9-4}
$$

$$
\frac{\partial u(z=z_u,t)}{\partial z} = g_{nu}(t) \tag{A.9-5}
$$

where  $g_{nl}(t)$ ,  $g_{nu}(t)$  are functions to be specified. This case can be readily programmed since *t* is an input argument of the ODE/MOL routine (pde1c). The exterior values are

$$
u(z = z_l - \Delta z, t) = u(z = z_l + \Delta z, t) - 2\Delta z g_{nl}(t)
$$
 (A.9-6)

$$
u(z = z_u + \Delta z, t) = u(z = z_u - \Delta z, t) + 2\Delta z g_{nu}(t)
$$
 (A.9-7)

• Equation (A.4-1) is programmed for ncase=3.

```
if(ncase==3){
  for(iz in 1:nz){
    if(iz==1){
       um = u[2] - (km/D) * (2 * dz) * u[1];ut[1]=D*(u[2]-2*u[1]+um)/dzs;}
    if(iz == nz)up=u[nz-1]-(km/D)*(2*dz)*u[nz];ut[nz]=D*(up-2*u[nz]+u[nz-1])/dzs;}
    if((iz>1)&(iz<nz)){
      ut[iz] = D * (u[iz+1]-2*u[iz]+u[iz-1])/dzs;}
}
```
For a homogeneous Robin BC at  $z = z_l$ ,

$$
D\frac{\partial u(z=z_l,t)}{\partial z}-k_mu(z=z_l,t)=0
$$

the FD approximation is  $(iz=1)$ 

$$
D\frac{u(z_l+\Delta z,t)-u(z_l-\Delta z,t)}{2\Delta z}-k_mu(z_l,t)=0
$$

or  $u(z_l - \Delta z, t) = u(z_l + \Delta z, t) - (k_m/D)(2\Delta z)u(z = z_l, t)$ .  $u(z_l - \Delta z, t)$  is an exterior (fictitious) value outside the grid in  $z$  (um in the preceding code). Similarly, for a homogeneous Robin BC at  $z = z_u$ ,

$$
D\frac{\partial u(z=z_u,t)}{\partial z} + k_m u(z=z_u,t) = 0
$$

the FD approximation is (iz=nz)

$$
D\frac{u(z_u + \Delta z, t) - u(z_u - \Delta z, t)}{2\Delta z} + k_m u(z_l, t) = 0
$$

or  $u(z_u + \Delta z,t) = u(z_u - \Delta z,t) - (k_m/D)(2\Delta z)u(z = z_u,t)$ .  $u(z_u + \Delta z,t)$  is an exterior value outside the grid in *z* (up in the preceding code). The MOL ODEs are defined at the interior grid points in *z*,

if((iz>1)}&(iz<nz))

according to eq. (A.9-1).

An extension of the linear Robin BCs can be considered as nonlinear BCs. For example,

$$
D\frac{\partial u(z=z_l,t)}{\partial z} - f_{rl}(u(z-z_l,t)) = 0
$$

$$
D\frac{\partial u(z=z_u,t)}{\partial z} + f_{ru}(u(z-z_u,t)) = 0
$$

and  $f_{rl}$ ,  $f_{ru}$  are functions to be specified. The FD approximations of the nonlinear Robin BCs are

$$
D \frac{u(z_l + \Delta z, t) - u(z_l - \Delta z, t)}{2\Delta z} - f_{rl}(u(z - z_l, t)) = 0
$$
  

$$
D \frac{u(z_u + \Delta z, t) - u(z_u - \Delta z, t)}{2\Delta z} + f_{ru}(u(z - z_u, t)) = 0
$$

or

$$
u(z_l - \Delta z, t) = u(z_l + \Delta z, t) - (2\Delta z) f_{rl}(u(z = z_l, t))
$$
 (A.9-8)

$$
u(z_u + \Delta z, t) = u(z_u - \Delta z, t) - (2\Delta z) f_{ru}(u(z = z_u, t))
$$
 (A.9-9)

Equations (A.9-8,9) can be programmed in the ODE/MOL routine (pde1c) since  $u(z = z_l, t)$ ,  $u(z = z_u, t)$  are available in the input argument vector for  $u(z,t)$ .

• The counter for the calls to pde1c is incremented and returned to the main program of Listing A.8 by <<-.

```
#
# Increment calls to pde1c
  ncall <<- ncall+1;
```
• The vector ut is returned as a list as required by lsodes. c is the R vector utility. The final  $\}$  concludes pde1c.

```
#
# Return derivative vector
  return(list(c(ut)));
  }
```
This completes the discussion of pde1c. The output from the main program of Listing A.8 and ODE/MOL routine pde1c of Listing A.9 is considered next, staring with ncase=1.

[1] 11

[1] 22  $ncase = 1$ t z u(z,t) uex(z,t) error 0.00 0.00 0.000e+00 0.000e+00 0.000e+00 0.00 0.25 7.071e-01 7.071e-01 0.000e+00 0.00 0.50 1.000e+00 1.000e+00 0.000e+00 0.00 0.75 7.071e-01 7.071e-01 0.000e+00 0.00 1.00 0.000e+00 1.225e-16 -1.225e-16 t z  $u(z,t)$   $u(x,t)$  error 0.20 0.00 0.000e+00 0.000e+00 0.000e+00 0.20 0.25 5.807e-01 5.804e-01 2.349e-04 0.20 0.50 8.212e-01 8.209e-01 3.323e-04 0.20 0.75 5.807e-01 5.804e-01 2.349e-04 0.20 1.00 0.000e+00 1.005e-16 -1.005e-16 t z u(z,t) uex(z,t) error 0.40 0.00 0.000e+00 0.000e+00 0.000e+00 0.40 0.25 4.769e-01 4.765e-01 3.873e-04 0.40 0.50 6.744e-01 6.738e-01 5.477e-04 0.40 0.75 4.769e-01 4.765e-01 3.873e-04 0.40 1.00 0.000e+00 8.252e-17 -8.252e-17 t z u(z,t) uex(z,t) error 0.60 0.00 0.000e+00 0.000e+00 0.000e+00 0.60 0.25 3.916e-01 3.911e-01 4.747e-04 0.60 0.50 5.538e-01 5.531e-01 6.714e-04 0.60 0.75 3.916e-01 3.911e-01 4.747e-04 0.60 1.00 0.000e+00 6.774e-17 -6.774e-17 t z u(z,t) uex(z,t) error 0.80 0.00 0.000e+00 0.000e+00 0.000e+00 0.80 0.25 3.216e-01 3.211e-01 5.196e-04 0.80 0.50 4.548e-01 4.540e-01 7.349e-04 0.80 0.75 3.216e-01 3.211e-01 5.196e-04 0.80 1.00 0.000e+00 5.560e-17 -5.560e-17 t z u(z,t) uex(z,t) error 1.00 0.00 0.000e+00 0.000e+00 0.000e+00 1.00 0.25 2.641e-01 2.635e-01 5.331e-04

```
1.00 0.50 3.735e-01 3.727e-01 7.540e-04
1.00 0.75 2.641e-01 2.635e-01 5.331e-04
1.00 1.00 0.000e+00 4.564e-17 -4.564e-17
```
 $ncall = 55$ 

Table A.5: Numerical output from Listings A.8, A.9, ncase=1

The following details about Table A.5 can be noted (with some repetition of the discussion of Tables A.1-4).

- 11 *t* output points as the first dimension of the solution matrix out from lsodes as programmed in the main program of Listing A.8 (with  $n$ <sup>out=11</sup>).
- The solution matrix out returned by 1 sodes has 22 elements as a second dimension. The first element is the value of *t*. Elements 2 to 22 are  $u(z,t)$ from eq. (A.4-1) (for each of the 21 output points).
- The solution is displayed for  $t=0,1/10=0.1,\ldots,1$  as programmed in Listing A.8 (every second value of *t* is displayed as explained previously).
- The solution is displayed for  $z=0,1/20=0.05,...,1$  as programmed in Listing A.8 (every fifth value of *z* is displayed as explained previously).
- IC (A.4-10) is confirmed  $(t = 0)$ .
- BCs (A.4-11,12) are confirmed ( $z = z_l = 0, z = z_u = 1$ ).
- The computational effort as indicated by ncall = 55 is modest so that lsodes computed the solution to eq. (A.4-1) efficiently.

The graphical output is in Figures A.3-1. Comparison of the numerical solution  $u(z,t)$  (plotted with *n*) and exact solution of eq. (A.4-18) (plotted with *x*) indicates good agreement between the numerical and exact solutions. In other words, Figure A.3-1 indicates the numerical integration of the parabolic (diffusion) PDE with Dirichlet BCs is straightforward in comparison with the first-order hyperbolic (advection) PDE.

The output for ncase=2 follows.

```
[1] 11
```

```
[1] 22
```
 $ncase = 2$ 



0.00 1.00 -1.000e+00 -1.000e+00 0.000e+00 t z u(z,t) uex(z,t) error 0.20 0.00 8.212e-01 8.209e-01 3.323e-04 0.20 0.25 5.807e-01 5.804e-01 2.350e-04 0.20 0.50 -2.565e-15 5.026e-17 -2.615e-15 0.20 0.75 -5.807e-01 -5.804e-01 -2.350e-04 0.20 1.00 -8.212e-01 -8.209e-01 -3.323e-04 t z u(z,t) uex(z,t) error 0.40 0.00 6.744e-01 6.738e-01 5.476e-04 0.40 0.25 4.769e-01 4.765e-01 3.872e-04 0.40 0.50 -7.886e-15 4.126e-17 -7.928e-15 0.40 0.75 -4.769e-01 -4.765e-01 -3.872e-04 0.40 1.00 -6.744e-01 -6.738e-01 -5.476e-04 t z u(z,t) uex(z,t) error 0.60 0.00 5.538e-01 5.531e-01 6.714e-04 0.60 0.25 3.916e-01 3.911e-01 4.748e-04 0.60 0.50 1.522e-14 3.387e-17 1.518e-14 0.60 0.75 -3.916e-01 -3.911e-01 -4.748e-04 0.60 1.00 -5.538e-01 -5.531e-01 -6.714e-04 t z u(z,t) uex(z,t) error 0.80 0.00 4.548e-01 4.540e-01 7.349e-04 0.80 0.25 3.216e-01 3.211e-01 5.197e-04 0.80 0.50 6.965e-14 2.780e-17 6.962e-14 0.80 0.75 -3.216e-01 -3.211e-01 -5.197e-04 0.80 1.00 -4.548e-01 -4.540e-01 -7.349e-04 t z  $u(z,t)$   $u(x,t)$  error 1.00 0.00 3.735e-01 3.727e-01 7.540e-04 1.00 0.25 2.641e-01 2.635e-01 5.332e-04 1.00 0.50 3.852e-14 2.282e-17 3.850e-14 1.00 0.75 -2.641e-01 -2.635e-01 -5.332e-04 1.00 1.00 -3.735e-01 -3.727e-01 -7.540e-04

 $ncall = 55$ 

Table A.6: Numerical output from Listings A.8, A.9, ncase=2

The following details about Table A.6 can be noted (with some repetition of the discussion of Tables A.5).

The dimensions of the array out from 1 sodes are again  $11 \times 22$  (as for ncase=1, Table A.5).



**Figure A.3-1**  $u(z,t)$  from eqs. (A.4), ncase=1, Dirichlet BCs

- The solution is displayed for  $t=0,1/10=0.1,\ldots,1$  as programmed in Listing A.8 (every second value of *t*) and  $z=0,1/20=0.05,...,1$  (every fifth value of  $z$ ).
- IC (A.4-13) is confirmed  $(t = 0)$ .
- BCs (A.4-14,15) are confirmed ( $z = z_l = 0, z = z_u = 1$ ).
- The computational effort as indicated by ncall = 55 is modest so that lsodes computed the solution to eq. (A.4-1) efficiently.

The graphical output is in Figures A.3-2. Comparison of the numerical solution  $u(z,t)$  (plotted with *n*) and exact solution of eq. (A.4-19) (plotted with *x*) indicates good agreement between the numerical and exact solutions. In other words,





**Figure A.3-2**  $u(z,t)$  from eqs. (A.4), ncase=2, Neumann BCs

Figure A.3-2 indicates the numerical integration of the parabolic (diffusion) PDE with Neumann BCs is straightforward.

The output for ncase=3 follows.

[1] 11

[1] 22

ncase = 3

$\mathbf t$	$\mathbf{Z}% _{0}=\mathbf{Z}_{0}=\math$	u(z,t)
0.00	0.00	1.000e+00
0.00	0.25	1.000e+00
0.00	0.50	1.000e+00
0.00	0.75	1.000e+00
0.00	1.00	1.000e+00
t	$\mathbf{z}$	u(z,t)
0.20	0.00	$3.355e-01$
0.20	0.25	8.925e-01
0.20	0.50	$9.892e - 01$
0.20	0.75	8.925e-01
0.20	1.00	$3.355e-01$
t	$\mathbf{z}$	u(z,t)
0.40	0.00	2.547e-01
0.40	0.25	7.560e-01
0.40	0.50	$9.148e - 01$
0.40	0.75	$7.560e-01$
0.40	1.00	$2.547e-01$
t	$\mathbf{z}$	u(z,t)
0.60	0.00	2.122e-01
0.60	0.25	6.518e-01
0.60	0.50	8.123e-01
0.60	0.75	$6.518e-01$
0.60	1.00	$2.122e-01$
t 0.80	$\mathbf{z}$ 0.00	u(z,t) 1.822e-01
0.80	0.25	$5.659e - 01$
0.80	0.50	7.118e-01
	$0.80 \quad 0.75$	$5.659e-01$
	$0.80$ 1.00	1.822e-01
t	$\mathbf{z}$	u(z,t)
	1.00 0.00	1.580e-01
1.00	0.25	$4.925e-01$
	1.00 0.50	$6.212e-01$
1.00	0.75	$4.925e-01$
	1.00 1.00	1.580e-01
	$ncall = 145$	

Table A.7: Numerical output from Listings A.8, A.9, ncase=3

The following details about Table A.7 can be noted (with some repetition of the discussion of Table A.5).

- The dimensions of the array out from 1 sodes are again  $11 \times 22$  (as for ncase=1,2, Tables A.5, A.6).
- The solution is displayed for  $t=0,1/10=0.1,\ldots,1$  as programmed in Listing A.8 (every second value of *t*) and  $z=0,1/20=0.05,...,1$  (every fifth value of *z*).
- The IC  $u(z,t=0) = 1$  (programmed in Listing A.8) is confirmed  $(t=0)$ and in Figure A.3-3 that follows.
- BCs (A.4-16,17) are confirmed ( $z = z_l = 0, z = z_u = 1$ ) and in Figure A.3-3 that follows.
- The computational effort as indicated by ncall = 145 is modest so that lsodes computed the solution to eq. (A.4-1) efficiently.

The graphical output is in Figures A.3-3. An exact solution to eq. (A.4-1), (A.4- 16,17) is available, but is relatively complicated so it is not included in Figure A.3-3. The numerical solution of eqs.  $(A.4-1) (A.4-16,17)$  is straightforward, which indicates a principal feature of the numerical MOL.

This concludes the discussion of a parabolic PDE with eq. (A.4-1) (diffusion equation) as an example. Consideration is next for a multitype PDE, including convection and diffusion.

## **A.5 MULTITYPE PDE**

Equation (A.6-1) has convection and diffusion terms ( $v_z \neq 0, D \neq 0$ ) and is termed a convection-diffusion or hyperbolic-parabolic PDE. The MOL numerical integration (solution) of this multitype PDE is straightforward. A main program follows.

```
#
# Convection-diffusion PDE
#
# Delete previous workspaces
 rm(list=ls(all=TRUE))
#
# Access ODE integrator
 library("deSolve");
#
# Access functions for numerical solution
  setwd("f:/Covid-19 neurological effects/appA");
  source("pde1d.R");
  source("vanl.R");
#
# Specify case
 ncase=1;
```

```
#
# Parameters
 vz=1;
 ue=1;
  if(ncase==1){
   D=1;nz=21;}
  if(ncase==2){
   D=0.001;
    nz=101;}
#
# Spatial grid in z
  z1=0; zu=1; dz=(zu-z1)/(nz-1); dzs=dz^2;z=seq(from=zl,to=zu,by=dz);
#
# Independent variable for ODE integration
 t0=0; tf=1; nout=11;tout=seq(from=t0,to=tf,by=(tf-t0)/(nout-1));
#
# Initial condition (t=0)
 u0=rep(0,nz);for(iz in 1:nz){
    u0[iz]=0}
 ncall=0;
#
# ODE integration
  out=lsodes(y=u0,times=tout,func=pde1d,
      sparsetype="sparseint",rtol=1e-6,
      atol=1e-6,maxord=5);
  nrow(out)
 ncol(out)
#
# Array for plotting numerical solution
  u=matrix(0,nrow=nz,ncol=nout);
  for(it in 1:nout){
    for(iz in 1:nz){
       u[iz,it]=out[it,iz+1];
    }
    u[1, it] = ue;}
#
# Display numerical solution
  Pe=vz*(zu-zl)/D;
  iv=seq(from=1,to=nout,by=5);
```

```
cat(sprint(f' \n) ncase = %2d Pe = %7.3e\n",
               ncase,Pe));
  for(it in iv){
      cat(sprint(f''\n t z u(z,t)\n^n));iv=seq(from=1,to=nz,by=10);
      for(iz in iv){
         cat(sprintf("%6.2f%6.2f%12.3e\n",
           \text{tout}[\text{it}],\text{z}[\text{iz}],\text{u}[\text{iz},\text{it}]),\}}
#
# Calls to ODE routine
  cat(sprintf("\n\n ncall = \delta5d\n\n",ncall));
#
# Plot PDE solution
#
# u
  par(mfrow=c(1,1));matplot(x=z[2:nz],y=u[2:nz,],type="l",xlab="z",ylab="u(z,t)",
           xlim=c(z1,zu), lty=1, main="1", lwd=2, col="black");
  matpoints(x=z[2:nz],y=u[2:nz],pch="n" ,lty=1,lwd=2,col="black" );
```
Listing A.10: Main program for eqs. (A.6-1,2,3,5), hyperbolic-parabolic

The following details about Listing A.10 can be noted.

• Previous workspaces are deleted.

```
#
# Convection-diffusion PDE
#
# Delete previous workspaces
 rm(list=ls(all=TRUE))
```
• The R ODE integrator library deSolve is accessed [6].

```
#
# Access ODE integrator
 library("deSolve");
#
# Access functions for numerical solution
  setwd("f:/Covid-19 neurological effects/appA");
  source("pde1d.R");
  source("vanl.R");
```
Then the directory with the files for the solution of eqs.  $(A.6-1,2,3,5)$  is designated. Note that setwd (set working directory) uses / rather than the usual  $\backslash$ .



**Figure A.3-3**  $u(z,t)$  from eqs. (A.4), ncase=3, Robin BCs

The ODE/MOL routine pde1d is discussed subsequently. The van Leer flux ∂*u* limiter is used for the convection term,  $v_z \frac{\partial u}{\partial z}$ , in eq. (A.6-1).

An index for a case, with  $n \text{case}=1, 2$ , is specified.

```
#
# Specify case
  ncase=1;
```
- The parameters of eqs.  $(A.6-1,2,3,5)$  are specified
	- # # Parameters

```
vz=1;
ue=1;
if(ncase==1){
  D=1;
  nz=21;}
if(ncase==2){
  D=0.001;
  nz=101;}
```
The number of grid points in *z*, nz varies with ncase to provide adequate resolution of the graphical solution (in Figures A.4 discussed subsequently).

• A spatial grid for eq.  $(A.6-1)$  is defined with nz points.

```
#
# Spatial grid in z
  zl=0;zu=1;dz=(zu-zl)/(nz-1);dzs=dz^2;
  z=seq(from=zl,to=zu,by=dz);
```
The grid spacing is  $dz = \Delta z$ .

• The interval in *t* is defined with nout=11 output points.

```
#
# Independent variable for ODE integration
 t0=0; tf=1; nout=11;tout=seq(from=t0,to=tf,by=(tf-t0)/(nout-1));
```
• IC (A.6-2) is implemented, with  $u(z,t=0) = f(z) = 0$ .

```
#
# Initial condition (t=0)
 u0=rep(0,nz);for(iz in 1:nz){
    u0[iz]=0;ncall=0;
```
Also, the counter for the calls to pde1d is initialized.

• The system of nz ODEs is integrated by the library integrator 1 sodes (available in deSolve, [6]). As expected, the inputs to lsodes are the ODE function, pde1d, the IC vector u0, and the vector of output values of *t*, tout. The length of u0 (nz) informs lsodes how many ODEs are to be integrated. func,y,times are reserved names.

# # ODE integration

```
out=lsodes(y=u0,times=tout,func=pde1d,
    sparsetype="sparseint",rtol=1e-6,
    atol=1e-6,maxord=5);
nrow(out)
ncol(out)
```
nrow,ncol confirm the dimensions of out.

• The numerical values of  $u(z,t)$  returned by 1 sodes are placed in matrix u. The BC  $u(z = z_l, t) = u[1, it] = ue$  is specified since it is not returned from lsodes (only solutions to ODEs are returned from lsodes).

```
#
# Array for plotting numerical solution
  u=matrix(0,nrow=nz,ncol=nout);
  for(it in 1:nout){
    for(iz in 1:nz){
       u[iz,it]=out[it,iz+1];
    }
    u[1, it] = ue;}
```
• The numerical values of  $u(z,t)$  returned by 1 sodes are displayed. Every fifth value in *t* and every tenth value in *z* appear from by=5,10. The axial *v* Peclet number,  $P_e = \frac{v_z(z_u - z_l)}{R}$  $P_e = \frac{P_e(\leq a \leq 1)}{D}$  is computed and displayed as explained subsequently.

```
#
# Display numerical solution
  Pe=vz*(zu-zl)/D;
  iv=seq(from=1,to=nout,by=5);
  cat(sprintf("\n ncase = \frac{2}{d} Pe = \frac{2}{3}.3e\n",
              ncase,Pe));
  for(it in iv){
      cat(sprintf("\n \ t \ z \ u(z,t)\n^n));iv=seq(from=1,to=nz,by=10);
      for(iz in iv){
        cat(sprintf("%6.2f%6.2f%12.3e\n",
          tout[it],z[iz],u[iz,it]));}
   }
```
• The number of calls to pde1d is displayed at the end of the solution.

```
#
# Calls to ODE routine
  cat(sprintf("\n\n ncall = \delta5d\n\n",ncall));
```
• The numerical solution is plotted as lines and superimposed points with the letter n.

```
#
# Plot PDE solution
#
# u
 par(mfrow=c(1,1));matplot(x=z[2:nz],y=u[2:nz],type="1",xlab="z",ylab="u(z,t)",xlim=c(zl,zu),lty=1,main="",lwd=2,
          col="black");
 matpoints(x=z[2:nz],y=u[2:nz],pch="n",lty=1,lwd=2,col="black");
```
The solution at  $z = z_l$  is not plotted ([2:nz,]) to avoid the discontiniuty in the IC and BC,  $u(z,t=0) = 0$ ,  $u(z = z_l = 0,t) = u_e = 1$ .

This completes the discussion of the main program of Listing A.10. The ODE/MOL routine, pde1d, called by lsodes in the main program is considered next.

```
pde1d=function(t,u,parm){
#
# Function pde1d computes the t derivative
# of u(z,t)#
# BC, z=zl
  u[1]=ue;
#
# PDE
  uz=vanl(zl,zu,nz,u,vz);
  ut=rep(0,nz);for(iz in 1:(nz-1)){
    if(iz==1){ut[iz]=0;}
    if(iz>1){
      ut[iz] = -vz*uz[iz] +D*(u[iz+1]-2*u[iz]+u[iz-1])/dzs;}
  }
#
# BC, z=zu
   ut[nz] = -vz * uz[nz];
#
# Increment calls to pde1d
 ncall <<- ncall+1;
#
# Return derivative vector
  return(list(c(ut)));
  }
```
Listing A.11: ODE/MOL routine pde1d for eqs. (A.6-1,2,3,5)

The function is defined.

```
pde1d=function(t,u,parm){
#
# Function pde1d computes the t derivative
# of u(z,t)
```
t is the current value of *t* in eq. (A.6-1). u is the nz-vector of ODE/PDEdependent variables. parm is an argument to pass parameters to pde1d (unused, but required in the argument list). The arguments must be listed in the order stated to properly interface with lsodes called in the main program of Listing A.10. The derivative vector of the LHS of eq. (A.6-1) is calculated and returned to lsodes as explained subsequently.

• BC  $(A.6-3)$  is programmed.

```
#
# BC, z=zl
  u[1] = ue;
```
• Equation  $(A.6-1)$  is programmed.

```
#
# PDE
 uz=vanl(zl,zu,nz,u,vz);
 ut=rep(0,nz);for(iz in 1:(nz-1)){
    if(iz==1){ut[iz]=0;}
    if(iz>1){
      ut[iz] = -vz*uz[iz] +D*(u[iz+1]-2*u[iz]+u[iz-1])/dzs;}
```
Note that the hyperbolic term  $-vz*uz[iz]$  and parabolic term  $D*(u[iz+1]-2*u[iz]+u[iz-1])/dzs$  are included.

• The dynamic BC (A.6-5) is programmed.

```
#
# BC, z=zu
   ut[nz] = -vz * uz[nz];
```
• The counter for the calls to pde1d is incremented and returned to the main program of Listing A.10 by <<-.

```
#
# Increment calls to pde1d
 ncall <<- ncall+1;
```
• The vector ut is returned as a list as required by lsodes. c is the R vector utility. The final } concludes pde1d.

```
#
# Return derivative vector
  return(list(c(ut)));
  }
```
The numerical and graphical output from the main program and ODE/MOL routine pde1d in Listings A.10, A.11 is considered next.

For ncase=1, the numerical output is in Table A.8.

[1] 11 [1] 22  $ncase = 1$   $Pe = 1.000e+00$ t z  $u(z,t)$ 0.00 0.00 1.000e+00 0.00 0.50 0.000e+00 0.00 1.00 0.000e+00 t z  $u(z,t)$ 0.50 0.00 1.000e+00 0.50 0.50 7.066e-01 0.50 1.00 3.360e-01  $t \t z \t u(z,t)$ 1.00 0.00 1.000e+00 1.00 0.50 8.376e-01 1.00 1.00 6.300e-01  $ncall = 247$ 

Table A.8: Numerical output from Listings A.10, A.11, ncase=1

The following details about Table A.8 can be noted.

- The dimensions of the array out from 1 sodes are  $11 \times 22$ .
- The solution is displayed for  $t=0,1/10=0.1,\ldots,1$  as programmed in Listing A.10 (every fifth value of *t*) and  $z=0,1/20=0.05,...,1$  (every tenth value of *z*).



**Figure A.4-1**  $u(z,t)$  from eq. (A.6-1), ncase=1

- The IC  $u(z,t=0) = 0$  (programmed in Listing A.10) is confirmed  $(t=0)$ and in Figure A.4-1 that follows.
- BC (A.6-3) is confirmed ( $z = z_l = 0, z = z_u = 1$ ) and in Figure A.4-1 that follows.
- The computational effort as indicated by ncall = 247 is modest so that lsodes computed the solution to eq. (A.4-1) efficiently.

The graphical output is in Figures A.4-1. The solution for the strongly parabolic  $a_1 \cdot a_2 = 1$ ,  $P_e = \frac{v_z(z - z_l)}{D} = \frac{(1)(1)}{1} = 1$  (with  $v_z = 1, D = 1$ ) is confirmed<sup>5</sup> (a smoothing of the discontinuity at  $z = z_l = 0$ ).

For ncase=2, the numerical output is given in Table A.9.

```
[1] 11
```
[1] 102

 $ncase = 2$  Pe = 1.000e+03

t	$\mathbf{z}$	u(z,t)
0.00	0.00	1.000e+00
0.00	0.10	$0.000e + 00$
0.00	0.20	$0.000e + 00$
0.00	0.30	$0.000e + 00$
0.00	0.40	$0.000e + 00$
0.00	0.50	$0.000e + 00$
0.00	0.60	$0.000e + 00$
0.00	0.70	$0.000e + 00$
0.00	0.80	$0.000e + 00$
0.00	0.90	$0.000e + 00$
0.00	1.00	$0.000e + 00$
t	$\mathbf{z}$	u(z,t)
0.50	0.00	$1.000e + 00$
0.50	0.10	1.000e+00
0.50	0.20	1.000e+00
0.50	0.30	1.000e+00
0.50	0.40	$9.969e - 01$
0.50	0.50	$5.362e-01$
0.50	0.60	$6.452e-07$
0.50	0.70	3.982e-08
0.50	0.80	$9.385e-10$
0.50	0.90	7.827e-12
0.50	1.00	$2.390e-14$
t	$\mathbf{z}$	u(z,t)
1.00	0.00	$1.000e + 00$
1.00	0.10	1.000e+00

<sup>&</sup>lt;sup>5</sup>The Peclet number,  $P_e = \frac{v_z(z_u - z_l)}{D}$ , can be considered as the ratio of the relative hyperbolic to parabolic contributions. For  $P_e = 1$  (ncase=1), eq. (A.6-1) is strongly parabolic (diffusive). For  $P_e = 1000$ (ncase=2), eq. (A.6-1) is strongly hyperbolic (convective).



ncall = 5885

Table A.9: Numerical output from Listings A.10, A.11, ncase=2

The following details about Table A.9 can be noted.

- The dimensions of the array out from 1 sodes are  $11 \times 102$ .
- The solution is displayed for  $t=0,1/10=0.1,\ldots,1$  as programmed in Listing A.10 (every fifth value of *t*) and  $z=0,1/100=0.01,\ldots,1$  (every tenth value of *z*).
- The IC  $u(z,t=0) = 0$  (programmed in Listing A.10) is confirmed  $(t=0)$ and in Figure A.4-2 that follows.
- BC (A.6-3) is confirmed  $(z = z_l = 0, z = z_u = 1)$  and in Figure A.4-2 that follows.
- The computational effort indicated by ncall = 5885 reflects the computational requirement of the van Leer limiter.

The graphical output is in Figure A.4-2.

*z* The solution for the strongly hyperbolic case, ncase=2,  $P_e = \frac{v_z(z - z_l)}{R}$  $P_e = \frac{P_e(\mathbf{x} - \mathbf{x}_i)}{D}$  =  $(1)(1)$  $\frac{(1)(1)}{0.001}$  = 1000 (with  $v_z = 1, D = 0.001$ ) is confirmed, that is, propagation (movement left to right) of the discontinuity originating at  $z = z_l = 0$ . The solution has no numerical oscillation. The small axial diffusion from the van Leer flux limiter is physical (from eq.  $(A.6-1)$  with  $D = 0.001$ ), not numerical. The right BC, eq.  $(A.6-5)$ , gives a smooth exit of the moving front at  $z = z_u = 1$ .

This concludes the discussion of a hyperbolic-parabolic PDE with eq. (A.6-1) (convection-diffusion equation) as an example. Consideration is next for a  $2 \times 2$  (two equations in two unknowns) system of simultaneous PDEs.

## **A.6 SIMULTANEOUS PDEs**

The concluding PDE example is based on the application of eqs. (A.6-1,2,3,5), to a  $2 \times 2$  PDE system. The equations are listed next.

$$
\frac{\partial u_1}{\partial t} = -v_{z1}\frac{\partial u_1}{\partial z} + D_1 \frac{\partial^2 u_1}{\partial z^2} + k_m(u_2 - u_1)
$$
 (A.10-1)



**Figure A.4-2**  $u(z,t)$  from eq. (A.6-1), ncase=2

$$
\frac{\partial u_2}{\partial t} = -v_{z2}\frac{\partial u_2}{\partial z} + D_2 \frac{\partial^2 u_2}{\partial z^2} - k_m(u_2 - u_1)
$$
 (A.10-2)

Equations (A.10-1,2) are first order in *t* and each requires an IC.

$$
u_1(z, t = 0) = f_1(z); u_2(z, t = 0) = f_2(z)
$$
 (A.10-3,4)

where  $f_1(z)$ ,  $f_2(z)$  are functions to be specified.

Equations  $(A.10-1,2)$  are second order in *z* and each requires two BCs. For a countercurrent system with  $v_{z1} > 0$ ,  $v_{z2} < 0$ ,

$$
u_1(z = z_l, t) = g_1(t) \tag{A.10-5}
$$

$$
\frac{\partial u_1(z=z_u,t)}{\partial t} + v_{z1} \frac{\partial u_1(z=z_u,t)}{\partial z} - k_m(u_2(z=z_u,t) - u_1(z=z_u,t)) = 0 \quad (A.10-6)
$$

$$
u_2(z = z_u, t) = g_2(t) \tag{A.10-7}
$$

$$
\frac{\partial u_2(z=z_l,t)}{\partial t} + v_{z2} \frac{\partial u_2(z=z_l,t)}{\partial z} + k_m(u_2(z=z_l,t) - u_1(z=z_l,t)) = 0 \quad (A.10-8)
$$

where  $g_1(t)$ ,  $g_2(t)$  are functions to be specified.

A main program for eqs. (A.10) follows.

```
#
# Two convection-diffusion PDEs
#
# Delete previous workspaces
  rm(list=ls(all=TRUE))
#
# Access ODE integrator
  library("deSolve");
#
# Access functions for numerical solution
  setwd("f:/Covid-19 neurological effects/appA");
  source("pde1e.R");
  source("vanl.R");
#
# Parameters
 vz1 = 1;
 vz2=-1;
 u1e=1;
 u2e=0;
  D1=0.001;
 D2=0.001
 km=1;nz=41;
#
# Spatial grid in z
  z1=0; zu=1; dz=(zu-z1)/(nz-1); dzs=dz^2;z=seq(from=zl,to=zu,by=dz);
#
# Independent variable for ODE integration
  t0=0; tf=1; nout=11;tout=seq(from=t0,to=tf,by=(tf-t0)/(nout-1));
```

```
#
# Initial condition (t=0)
 u0 = rep(0, 2*nz);for(iz in 1:nz){
    u0[iz]=0;u0[iz+nz]=0;}
 ncall=0;
#
# ODE integration
  out=lsodes(y=u0,times=tout,func=pde1e,
      sparsetype="sparseint",rtol=1e-6,
      atol=1e-6,maxord=5);
 nrow(out)
  ncol(out)
#
# Arrays for plotting numerical solution
  u1=matrix(0,nrow=nz,ncol=nout);
  u2=matrix(0,nrow=nz,ncol=nout);
  for(it in 1:nout){
    for(iz in 1:nz){
       u1[iz,it]=out[it,iz+1];
       u2[iz, it] = out[it, iz+1+nz];}
    u1[1, it] = u1e;u2[nz,it]=u2e;
  }
#
# Display numerical solution
 Pe1 = abs(vz1)*(zu-z1)/D1;Pe2 = abs(vz2)*(zu-z1)/D2;iv=seq(from=1,to=nout,by=5);
  cat(sprintf("\n Pe1 = %7.3e Pe2 = %7.3e\n",Pe1,Pe2));
  for(it in iv){
      cat(sprint(f' \n t z u1(z,t) u2(z,t)\n^n));iv=seq(from=1,to=nz,by=10);
      for(iz in iv){
        cat(sprintf("%6.2f%6.2f%12.3e%12.3e\n",
          tout[it],z[iz],u1[iz,it],u2[iz,it]));}
   }
#
# Calls to ODE routine
  cat(sprintf("\n\n ncall = \delta5d\n\n",ncall));
#
```

```
# Plot PDE solution
#
# u1
 par(mfrow=c(1,1));matplot(x=z[2:nz],y=u1[2:nz,],type="l",xlab="z",
          ylab="u1(z,t)",xlim=c(zl,zu),lty=1,main="",lwd=2,
          col="black");
 matpoints(x=z[2:nz], y=u1[2:nz], pch="n", lty=1, lwd=2,col="black");
#
# u2
 par(mfrow=c(1,1));matplot(x=z[1:(nz-1)],y=u2[1:(nz-1),],type="l",xlab="z",
          ylab="u2(z,t)",xlim=c(zl,zu),lty=1,main="",lwd=2,
          col="black");
 matpoints(x=z[1:(nz-1)], y=u2[1:(nz-1),], pch="n", lty=1, lwd=2,col="black");
```

```
Listing A.12: Main program for eqs. (A.10), 2 \times 2 hyperbolic-parabolic
```
The following details about Listing A.10 can be noted.

• Previous workspaces are deleted.

```
#
# Two convection-diffusion PDEs
#
# Delete previous workspaces
  rm(list=ls(all=TRUE))
```
• The R ODE integrator library deSolve is accessed [6].

```
#
# Access ODE integrator
  library("deSolve");
#
# Access functions for numerical solution
  setwd("f:/Covid-19 neurological effects/appA");
  source("pde1e.R");
  source("vanl.R");
```
Then the directory with the files for the solution of eqs. (A.10) is designated. Note that setwd (set working directory) uses / rather than the usual  $\mathcal{L}$ .

The ODE/MOL routine pde1e is discussed subsequently. The van Leer flux limiter is used for the convection terms,  $v_{z1} \frac{\partial u_1}{\partial z_1}$ ,  $v_{z2} \frac{\partial u_2}{\partial z_2}$  $\frac{\partial u_1}{\partial z}$ ,  $v_{z2} \frac{\partial u_2}{\partial z}$  in eqs. (A.10-1,2).

The parameters of eqs.  $(A.10)$  are specified

```
#
# Parameters
  vz1 = 1;
  vz2=-1;
  u1e=1;
  u2e=0;
  D1=0.001;
  D2=0.001
  km=1;nz=41;
```
The following details about these parameters can be noted.

- − Countercurrent convection is specified with velocities of opposite sign,  $vz1=1$ ,  $vz2=-1$ .
- $-$  The boundary value  $u_1(z = z_l, t) = u_{e_1} = 1$  moves the PDE system away from the ICs.
- − The PDE is strongly convective with D1=D2=0.001 so that *Pe*<sup>1</sup> =  $P_{e2} = 1000.$
- − The transfer coefficient in eqs. (A.10-1,2) is specified, *k<sup>m</sup>* = 1.
- − The number of grid points in *z*, nz=41, provides adequate spatial resolution of the graphical solution (in Figures A.5 discussed subsequently).
- A spatial grid for eqs.  $(A.10-1,2)$  is defined with nz=41 points.

```
#
# Spatial grid in z
  z1=0; zu=1; dz=(zu-z1)/(nz-1); dzs=dz^2;z=seq(from=zl,to=zu,by=dz);
```
The grid spacing is  $dz = \Delta z$ .

• The interval in *t* is defined with  $nout = 11$  output points.

```
#
```
- # Independent variable for ODE integration  $t0=0; t f=1; nout=11;$ tout=seq(from=t0,to=tf,by=(tf-t0)/(nout-1));
- ICs (A.10-3,4) are implemented, with  $u_1(z, t = 0) = f_1(z) = 0$ .  $u_2(z, t = 0)$  $0) = f_2(z) = 0.$

```
#
# Initial condition (t=0)
 u0=rep(0,2*nz);
  for(iz in 1:nz){
```
```
u0[iz]=0;u0[iz+nz]=0;}
 ncall=0;
```
Also, the counter for the calls to pde1e is initialized.

• The system of 2\*nz=82 ODEs is integrated by the library integrator lsodes (available in deSolve, [6]). As expected, the inputs to lsodes are the ODE function, pde1e, the IC vector u0, and the vector of output values of  $t$ , tout. The length of u0 ( $2*nz=82$ ) informs 1 sodes how many ODEs are to be integrated. func,y,times are reserved names.

```
# ODE integration
  out=lsodes(y=u0,times=tout,func=pde1e,
      sparsetype="sparseint",rtol=1e-6,
      atol=1e-6,maxord=5);
  nrow(out)
  ncol(out)
```
nrow,ncol confirm the dimensions of out.

• The numerical values of  $u_1(z,t), u_2(z,t)$  returned by 1sodes are placed in matrix u1, u2. The BCs  $u_1(z = z_l, t) = u_1[1, \text{it}] = u_1e$ ,  $u_1(z = z_l, t) = u_1e$  $z<sub>u</sub>$ ,*t*)=u2[nz,it]=u2e are specified since they are not returned from lsodes (only solutions to ODEs are returned from lsodes).

```
#
# Arrays for plotting numerical solution
  u1=matrix(0,nrow=nz,ncol=nout);
  u2=matrix(0,nrow=nz,ncol=nout);
  for(it in 1:nout){
    for(iz in 1:nz){
       u1[iz, it] = out[it, iz+1];u2[iz,it]=out[it,iz+1+nz];
    }
    u1[1,it] = u1e;u2[nz,it]=u2e;
  }
```
• The numerical values of  $u_1(z,t)$ ,  $u_2(z,t)$  returned by 1 sodes are displayed. Every fifth value in *t* and every tenth value in *z* appear from by=5,10. The axial Peclet numbers,  $P_{e1} = P_{e2} = 1000$  are computed and displayed as explained subsequently.

# # Display numerical solution  $Pe1 = abs(vz1)*(zu-z1)/D1;$ 

```
Pe2 = abs(vz2)*(zu-z1)/D2;iv=seq(from=1,to=nout,by=5);
cat(sprintf("\n Pe1 = %7.3e Pe2 = %7.3e\n",Pe1,Pe2));
for(it in iv){
   cat(sprint(f''\n t z u1(z,t) u2(z,t)\n^n));iv=seq(from=1,to=nz,by=10);
   for(iz in iv){
     cat(sprintf("%6.2f%6.2f%12.3e%12.3e\n",
       tout[it],z[iz],u1[iz,it],u2[iz,it]));}
 }
```
• The number of calls to pde1e is displayed at the end of the solution.

```
#
# Calls to ODE routine
  cat(sprintf("\n\n ncall = %5d\n\n",ncall));
```
• The numerical solution  $u_1(z,t)$  is plotted as lines and superimposed points with the letter n.

```
#
# Plot PDE solution
#
# 11par(mfrow=c(1,1));matplot(x=z[2:nz],y=u1[2:nz,],type="l",xlab="z",
          ylab="u1(z,t)",xlim=c(zl,zu),lty=1,main="",lwd=2,
          col="black");
 matpoints(x=z[2:nz], y=u1[2:nz], pch="n", lty=1, lwd=2,col="black");
```
The solution at  $z = z_l$  is not plotted ([2:nz,]) to avoid the discontiniuty in the IC and BC,  $u_1(z,t=0) = 0$ ,  $u_1(z = z_l = 0,t) = u_{\ell 1} = 1$ .

• The numerical solution  $u_2(z,t)$  is plotted as lines and superimposed points with the letter n.

```
#
# u2
 par(mfrow=c(1,1));matplot(x=z[1:(nz-1)],y=u2[1:(nz-1),],type="l",xlab="z",
          vlab="u2(z,t)",xlim=c(zl,zu),lty=1,main="",lwd=2,
          col="black");
 matpoints(x=z[1:(nz-1)],y=u2[1:(nz-1),],pch="n",lty=1,
            lwd=2,col="black");
```
The solution at  $z = z_u$  is not plotted ([1:(nz-1)]) to avoid a possible discontinuity in the IC and BC,  $u_2(z,t=0)$ ,  $u_2(z=z_u,t)$ .

This completes the discussion of the main program of Listing A.12. The ODE/MOL routine, pde1e, called by lsodes in the main program, is considered next.

```
pde1e=function(t,u,parm){
#
# Function pde1e computes the t derivative
# of u1(z,t), u2(z,t)#
# One vector to two vectors
  u1=rep(0,nz);u2=rep(0,nz);for(iz in 1:nz){
    u1[iz]=u[iz];u2[iz]=u[iz+nz];}
#
# BCs, z=zl, z=zu
 u1[1] = u1e;u2[nz] = u2e;#
# PDEs
#
# u1t
 u1z=vanl(zl,zu,nz,u1,vz1);
  ut=rep(0,nz);for(iz in 1:(nz-1)){
    if(iz==1){u1t[1]=0;}
    if(iz>1){
      u1t[iz] = -vz1*u1z[iz] +D1*(u1[iz+1]-2*u1[iz]+u1[iz-1])/dzs+
              km*(u2[iz]-u1[iz]);}
#
# u2t
  u2z=vanl(z1,zu,nz,u2,vz2);u2t=rep(0,nz);for(iz in 2:nz){
    if(iz==nz){u2t[nz]=0;}
    if(iz<nz){
      u2t[iz] = -vz2*u2z[iz] +D2*(u2[iz+1]-2*u2[iz]+u2[iz-1])/dzs-
              km*(u2[iz]-u1[iz]);}
#
```

```
# BC, z=zl, zu
  u1t[nz] = -vz1*u1z[nz]+km*(u2[nz]-u1[nz]);
  u2t[1] = -vz2*u2z[1] -km*(u2[1]-u1[1]);#
# Two vectors to one vector
 ut=rep(0,2*nz);for(iz in 1:nz){
    ut[iz] = ut[iz];ut[iz+nz]=u2t[iz];}
#
# Increment calls to pde1e
 ncall <<- ncall+1;
#
# Return derivative vector
 return(list(c(ut)));
  }
```
Listing A.13: ODE/MOL routine pde1e for eqs.  $(A.10)$ ,  $2 \times 2$  hyperbolic-parabolic

The following details about Listing A.11 can be noted.

The function is defined.

```
pde1e=function(t,u,parm){
#
# Function pde1e computes the t derivative
# of u1(z,t), u2(z,t)
```
t is the current value of *t* in eqs.  $(A.10-1,2)$ . u is the  $2*nz=82$ -vector of ODE/PDE dependent variables. parm is an argument to pass parameters to pde1e (unused, but required in the argument list). The arguments must be listed in the order stated to properly interface with lsodes called in the main program of Listing A.12. The derivative vector of the LHS of eqs. (A.10-1,2) is calculated and returned to lsodes as explained subsequently.

• u is placed in two vectors, u1, u2, to facilitate the programming of eqs.  $(A.10-1,2)$ 

```
#
# One vector to two vectors
 u1=rep(0,nz);u2=rep(0,nz);for(iz in 1:nz){
   u1[iz]=u[iz];u2[iz]=u[iz+nz];}
```

```
• BCs (A.10-5,7) are programmed.
```

```
#
# BCs, z=zl, z=zu
  u1[1] = u1e;u2[nz]=u2e;
```
iz=1,nz specify points  $z = z_l, z_u$ , respectively (programmed in Listing A.12). u1e=1 moves the PDE solutions away from tne homogeneous ICs, eqs. (A.10-3,4) with  $f_1(z) = f_2(z) = 0$  programmed in Listing A.12.

```
• Equation (A.10-1) is programmed.
```

```
#
# PDEs
#
# u1t
  u1z=vanl(z1,zu,nz,u1,vz1);ut=rep(0,nz);for(iz in 1:(nz-1)){
    if(iz==1){u1t[1]=0;}
    if(iz>1){
      u1t[iz] = -vz1*u1z[iz] +D1*(u1[iz+1]-2*u1[iz]+u1[iz-1])/dzs+
              km*(u2[iz]-u1[iz]);}
  }
```
Note that the hyperbolic term  $-vz1*u1z[iz]$  and parabolic term  $D1*(u1[iz+1]-2*u1[iz]+u1[iz-1])/dzs$  are included.

```
• Equation (A.10-2) is programmed.
```

```
#
# u2t
 u2z=vanl(z1,zu,nz,u2,vz2);u2t=rep(0,nz);for(iz in 2:nz){
    if(iz==nz){u2t[nz]=0;}
    if(iz<nz){
      u2t[iz] = -vz2*u2z[iz] +D2*(u2[iz+1]-2*u2[iz]+u2[iz-1])/dzs-
              km*(u2[iz]-u1[iz]);}
```
The hyperbolic term  $-vz2*u2z[iz]$  and parabolic term  $D2*(u2[iz+1]-2*u2[iz]+u2[iz-1])/dzs$  are included.

• The dynamic BCs  $(A.10-6.8)$  are programmed. iz=1,nz specify points  $z = z_l, z_u$ , respectively (programmed in Listing A.12).

```
#
# BC, z=zl, zu
   u1t[nz] = -vz1*u1z[nz]+km*(u2[nz]-u1[nz]);
   u2t[1] = -vz2*u2z[1] -km*(u2[1]-u1[1]);
```
• The counter for the calls to pde1e is incremented and returned to the main program of Listing A.13 by <<-.

```
#
# Increment calls to pde1e
  ncall <<- ncall+1;
```
- The vector ut is returned as a list as required by lsodes. c is the R vector utility. The final } concludes pde1e.
- The derivative vectors u1t, u2t are placed in a single vector ut to return to lsodes for the next step along the solution.

```
#
# Two vectors to one vector
 ut=rep(0,2*nz);for(iz in 1:nz){
    ut[iz] =u1t[iz];
    ut[iz+nz]=u2t[iz];
  }
```
• The vector ut is returned as a list as required by lsodes. c is the R vector utility. The final } concludes pde1e.

```
#
# Return derivative vector
  return(list(c(ut)));
  }
```
The numerical and graphical output from the main program and ODE/MOL routine pde1e in Listings A.12, A.13 is considered next. The numerical output is in Table A.10.

[1] 11 [1] 83 Pe1 = 1.000e+03 Pe2 = 1.000e+03 t z  $u1(z,t)$   $u2(z,t)$ 0.00 0.00 1.000e+00 0.000e+00 0.00 0.25 0.000e+00 0.000e+00



```
ncall = 3969
```
Table A.10: Numerical output from Listings A.12, A.13

The following details about Table A.10 can be noted.

- The dimensions of the array out from 1 sodes are  $11 \times 83$  corresponding to nout=11, 2(nz)+1=2(41)+1=83.
- The solution is displayed for  $t=0,1/10=0.1,\ldots,1$  as programmed in Listing A.12 (every fifth value of *t*) and  $z=0,1/40=0.025,...,1$  (every tenth value of *z*).
- The ICs  $u(z,t=0) = u_2(z,t=0) = 0$  (programmed in Listing A.12) are confirmed  $(t = 0)$  and in Figures A.5-1,2 that follow.
- BCs (A.10-5,7) are confirmed,  $(u_1(z = z_l = 0,t) = 1, u_2(z = z_u = 1,t) = 0,$ and in Figures A.5-1,2 that follow. The numerical solutions  $u_1(z,t)$ ,  $u_2(z,t)$ are the response to BC (A.10-5) starting from homogeneous ICs (A.10-3,4).
- The computational effort indicated by ncall = 3969 reflects the computational requirement of the van Leer limiter.

The graphical output is in Figures A.5-1,2.

 $u_1(z,t)$  is the response to BC (A.10-5) starting from homogeneous IC (A.10-3), and includes the effect of the transfer term  $k_m(u_2(z,t) - u_1(z,t))$ .  $u_2(z,t)$  is the response to the transfer term  $k_m(u_2(z,t) - u_1(z,t))$  starting from homogeneous IC  $(A.10-4),$ 



**Figure A.5-1**  $u_1(z,t)$  from eq. (A.10-1)

## **A.7 SUMMARY AND CONCLUSIONS**

This appendix is intended as a basic introduction to PDE analysis, with emphasis on evolutionary (time dependent) PDEs. PDE terminology and geometric classification are presented, followed by computer implementation of PDE systems by the method



**Figure A.5-2**  $u_2(z,t)$  from eq. (A.10-2)

of lines. Source routines in R with detailed documentation provide a starting point for the development of new PDE models.

## **REFERENCES**

- 1. https://en.wikipedia.org/wiki/Cartesian˙coordinate˙system.
- 2. https://en.wikipedia.org/wiki/Cylindrical˙coordinate˙system.
- 3. https://en.wikipedia.org/wiki/Spherical˙coordinate˙system.
- 4. https://en.wikipedia.org/wiki/Curvilinear˙coordinates.
- 5. Griffiths, G.W., and W.E. Schiesser (2012), *Traveling Wave Analysis of Partial Differential Equations*, Academic Press-Elsevier, Oxford, UK.
- 6. Soetaert, K., J. Cash, and F. Mazzia (2012), *Solving Differential Equations in R*, Springer-Verlag, Heidelberg, Germany.



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